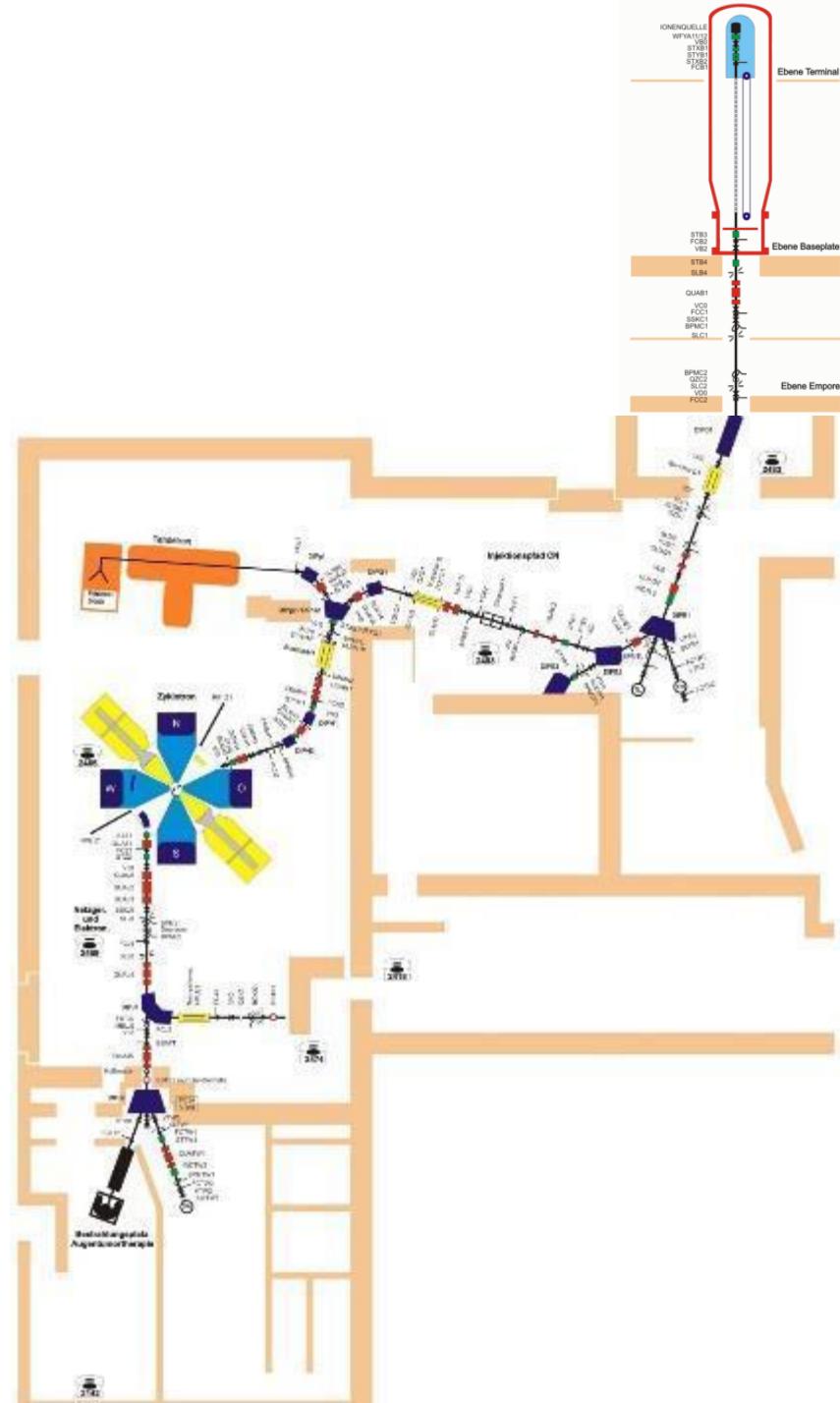


A. Denker, J. Bundesmann, T. Damerow, A. Dittwald, T. Fanselow, D. Hildebrand, U. Hiller, Y. Jlassi,  
I. Kailouh, G. Kourkafas, S. Ozierenski, R. Pena Freitas Mendes, J. Röhrich, C. Zimmer  
D. Cordini, J. Heufelder, S. Seidel, R. Stark, A. Weber  
A. Kwamou, Z. Önal, D. Rössink

# STATUS OF THE HZB CYCLOTRON

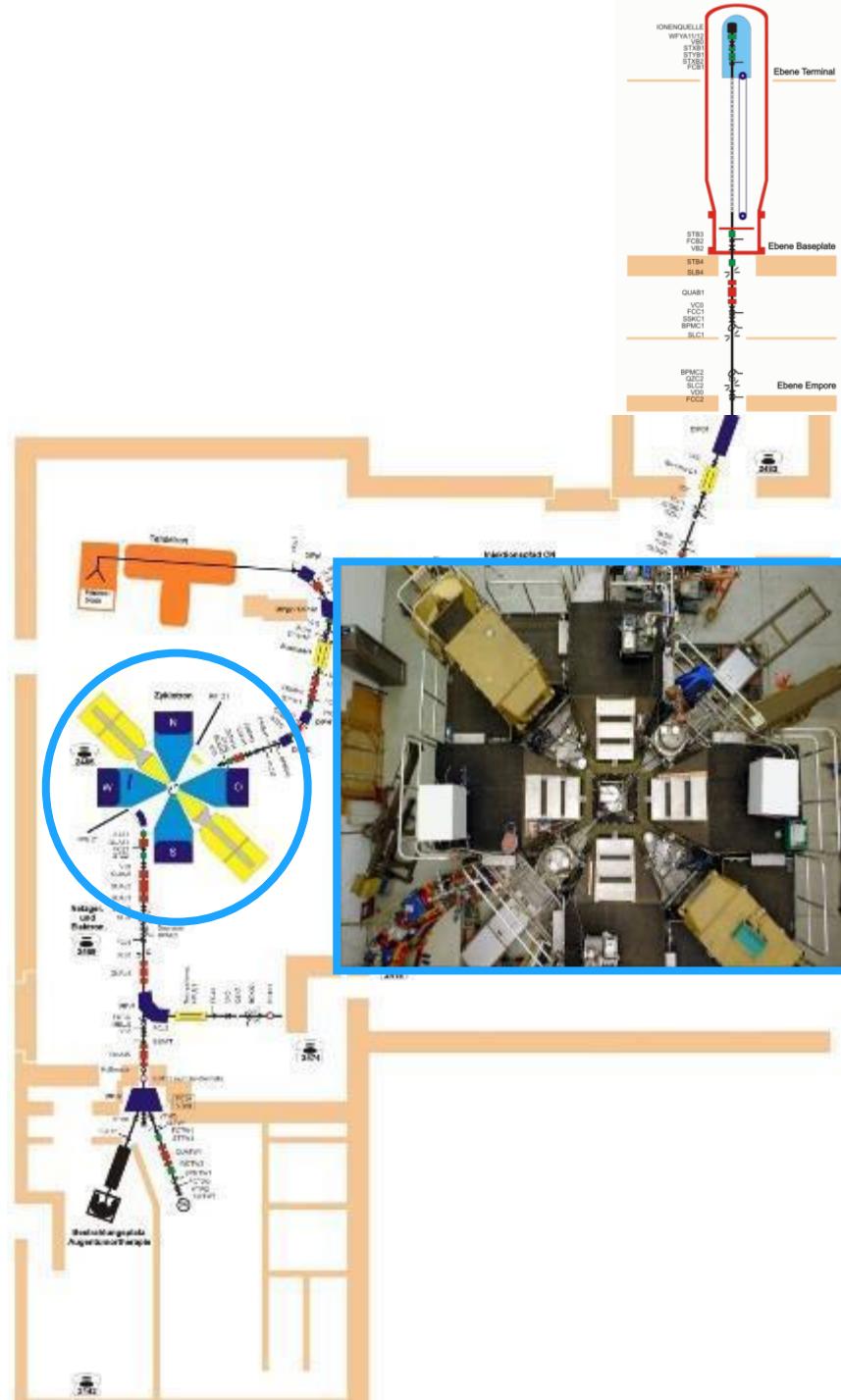
23rd International Conference on  
Cyclotrons and their Application

# Layout of the accelerator complex



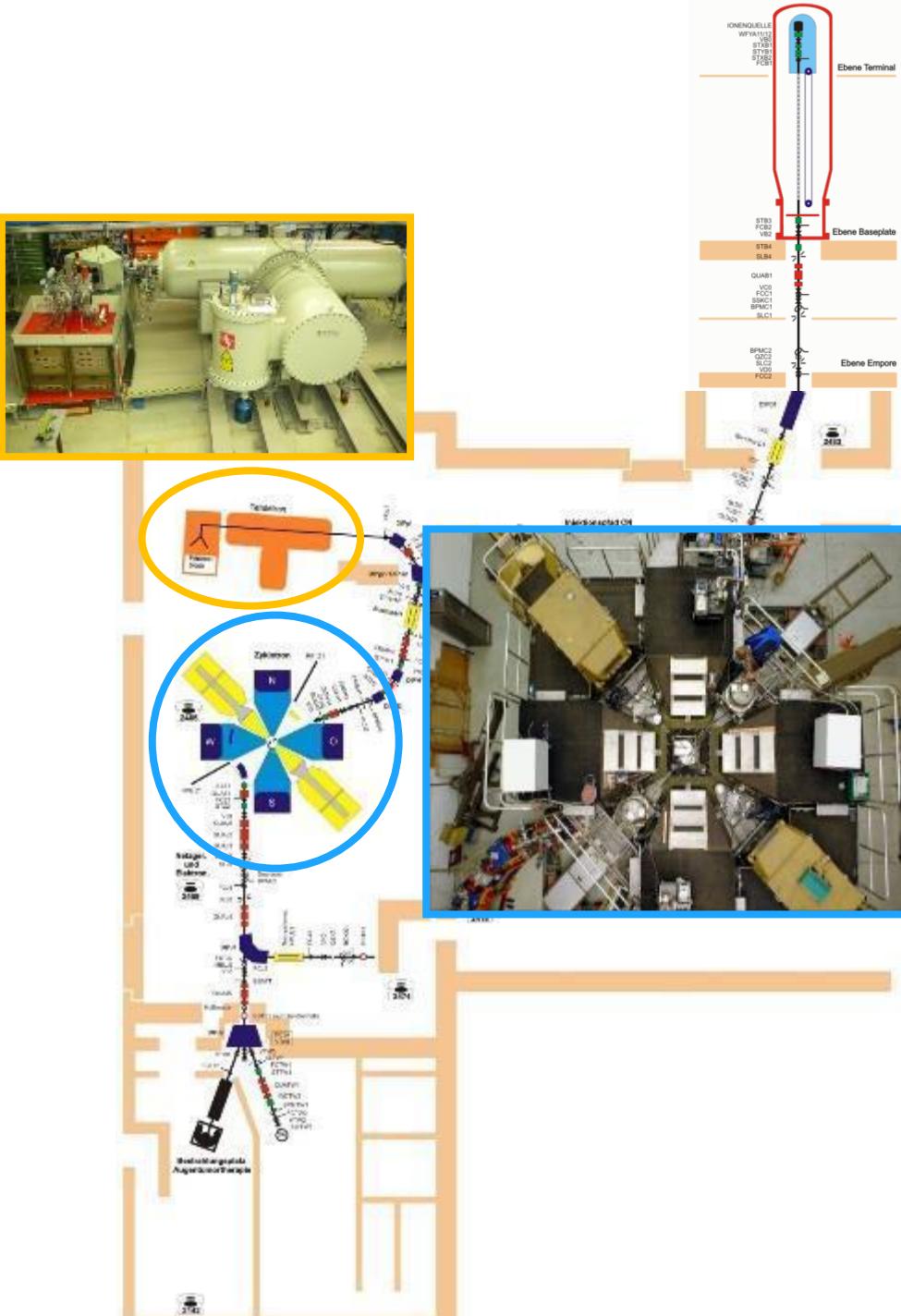
## Layout of the accelerator complex

- **k = 130 isochronous sector cyclotron**  
**10 – 20 MHz**



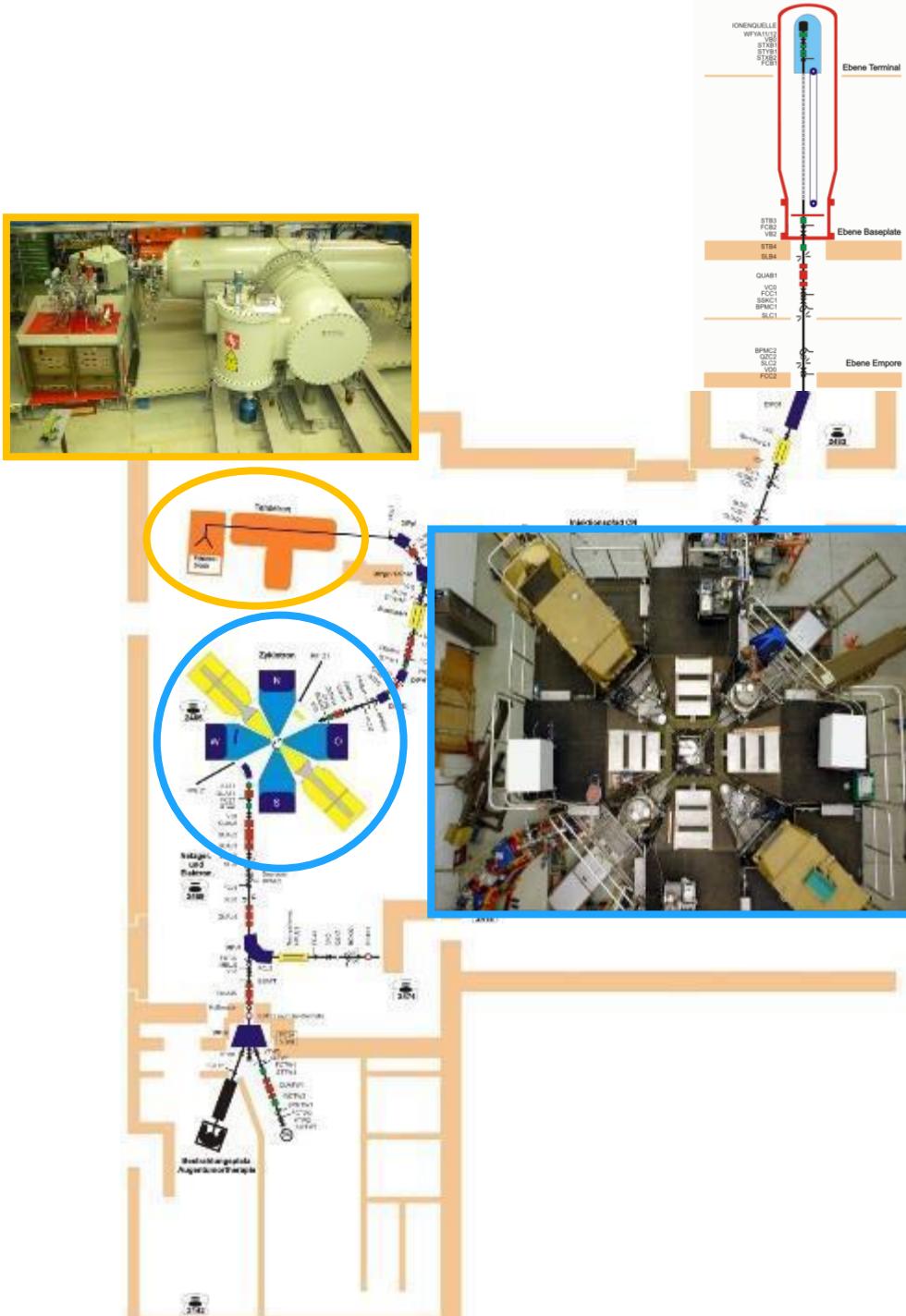
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- **two injectors:**
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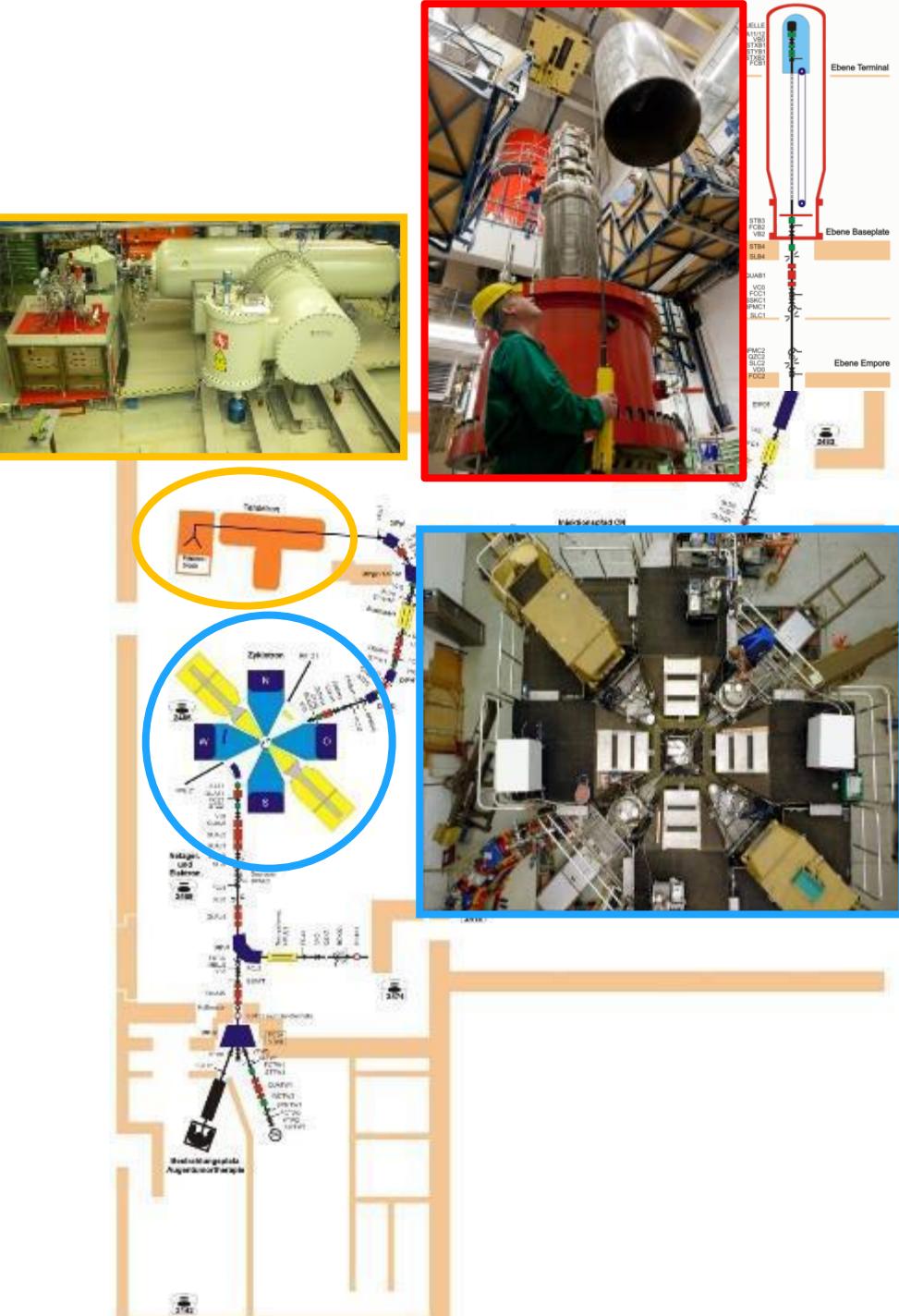
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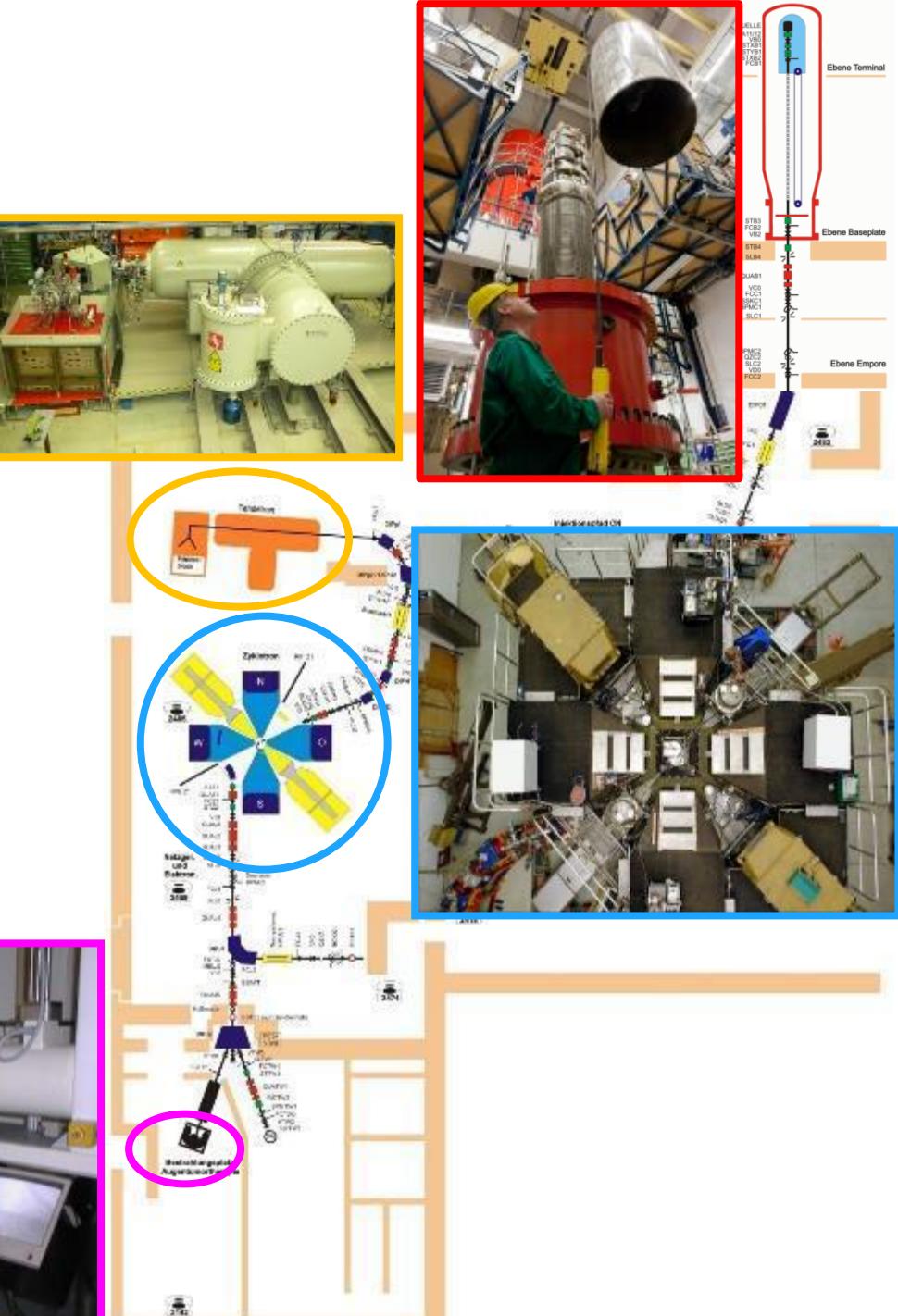
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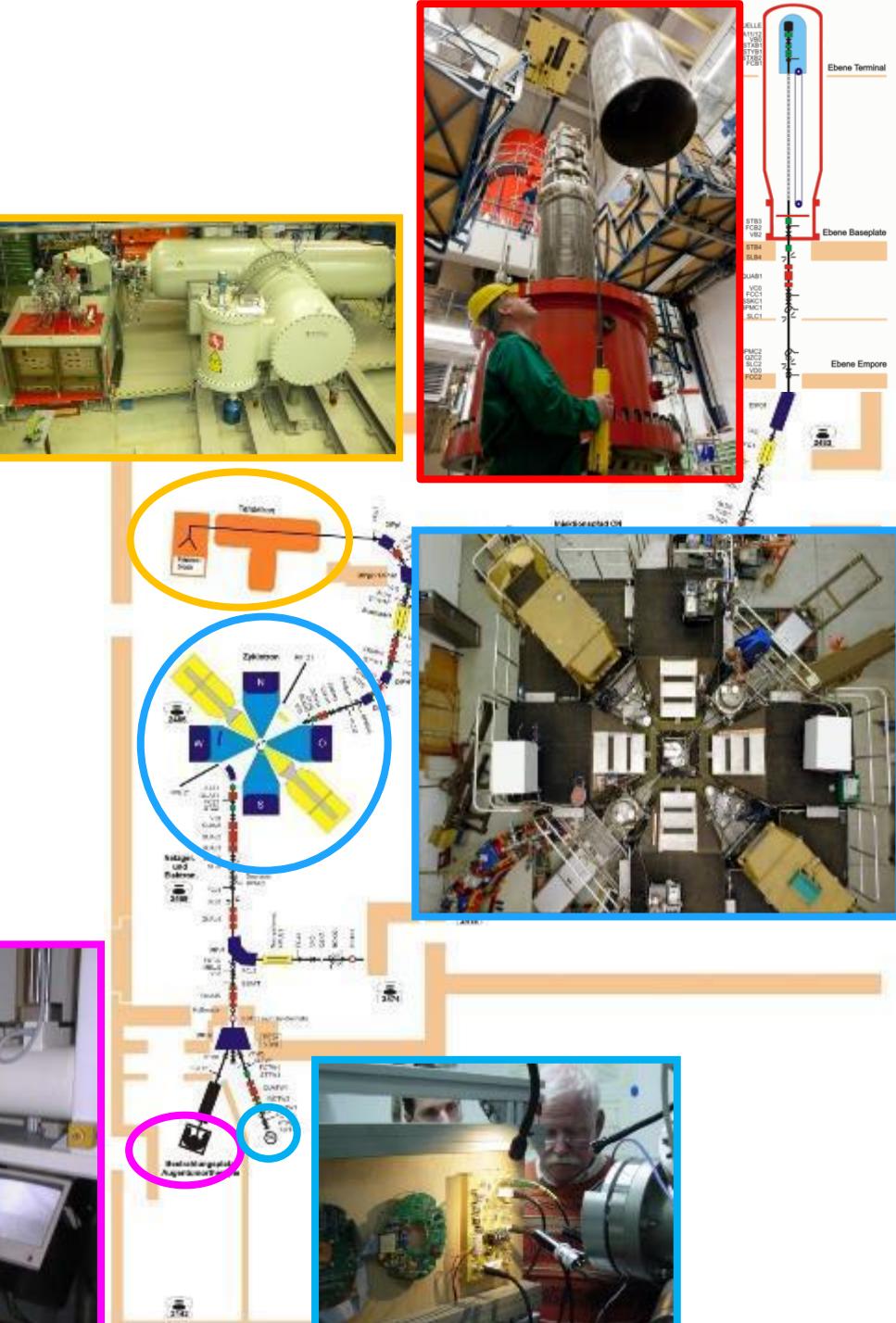
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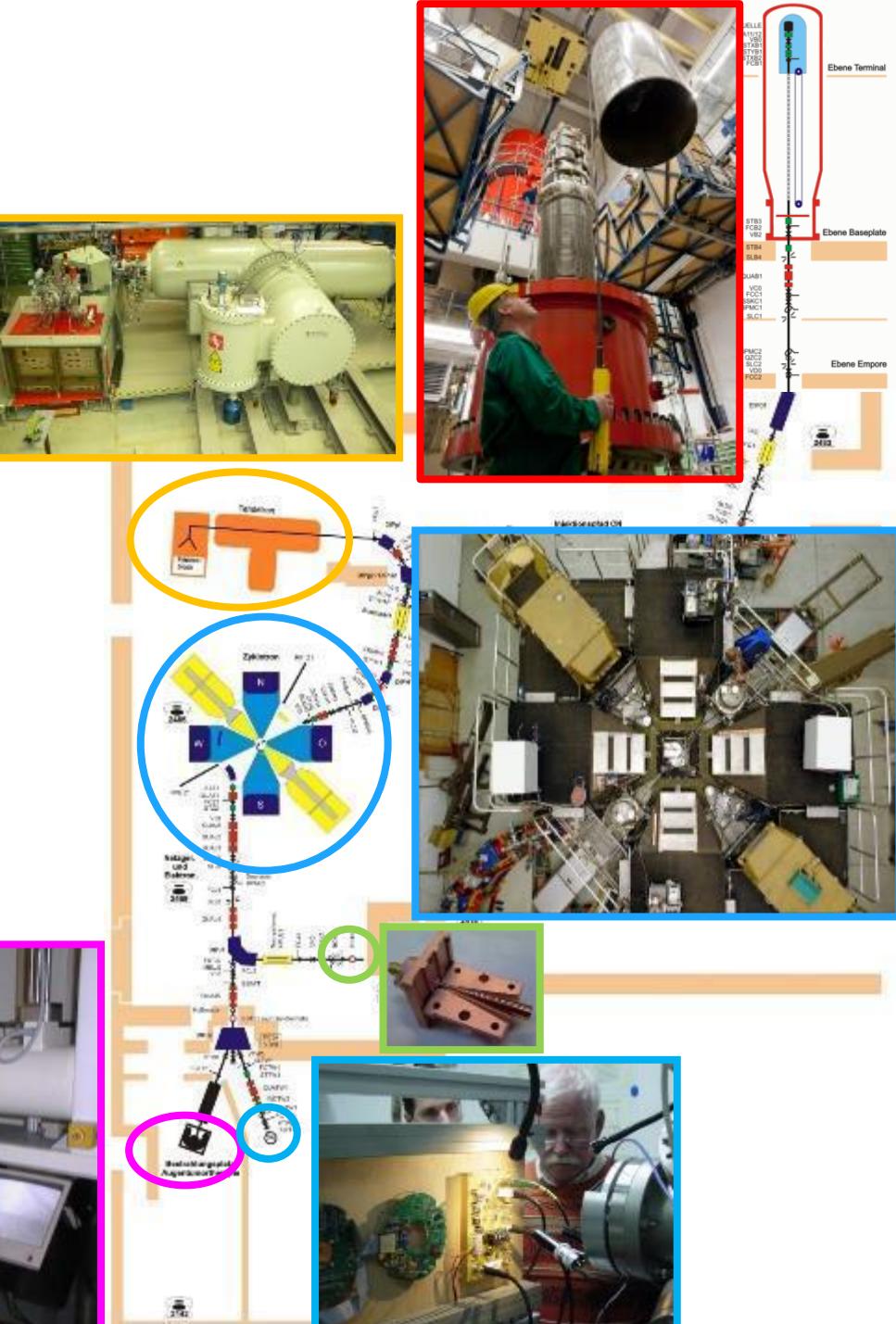
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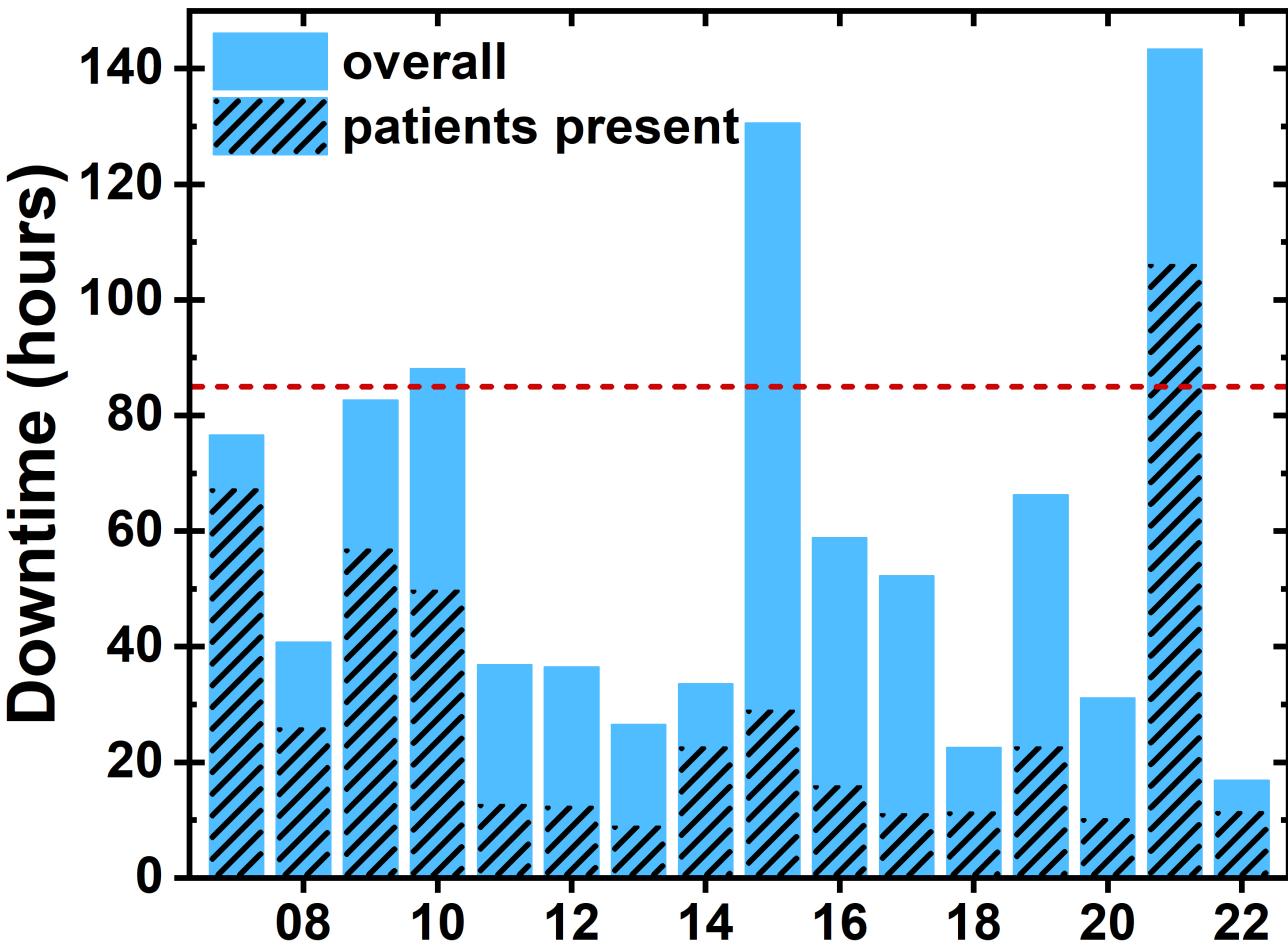
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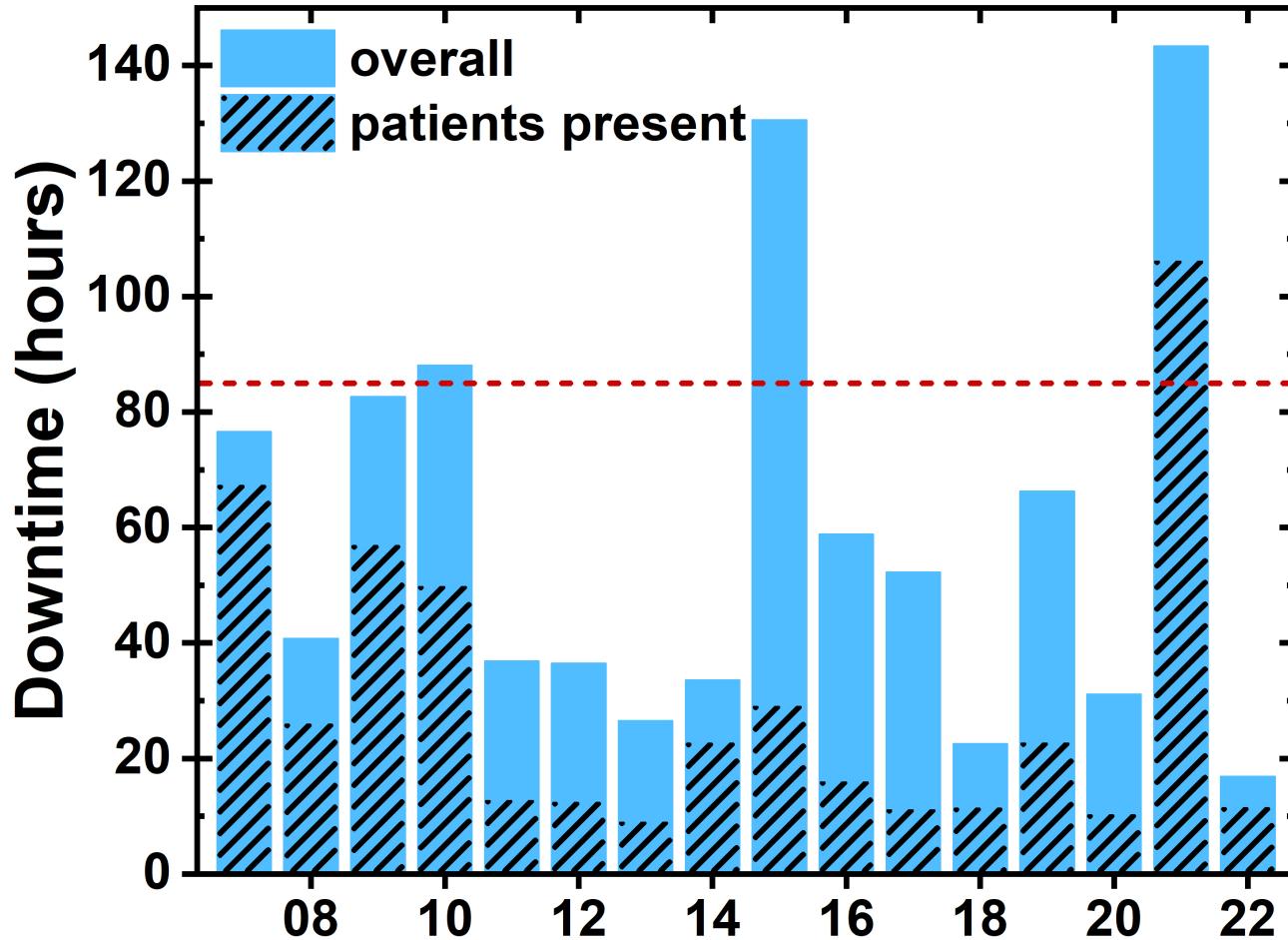
## Accelerator Performance

- only 1700 hours of scheduled beam time:  
major events → huge impact on statistics



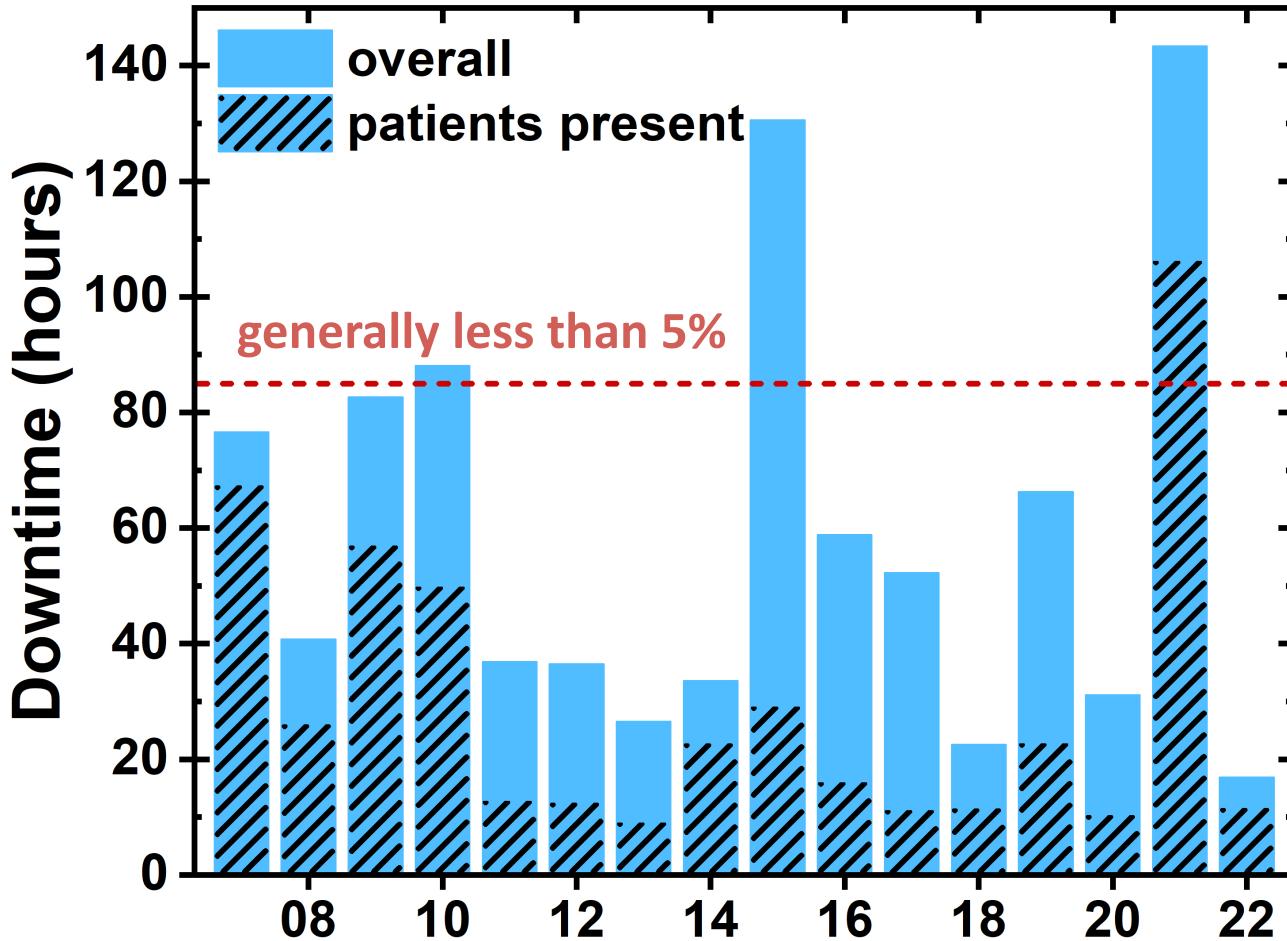
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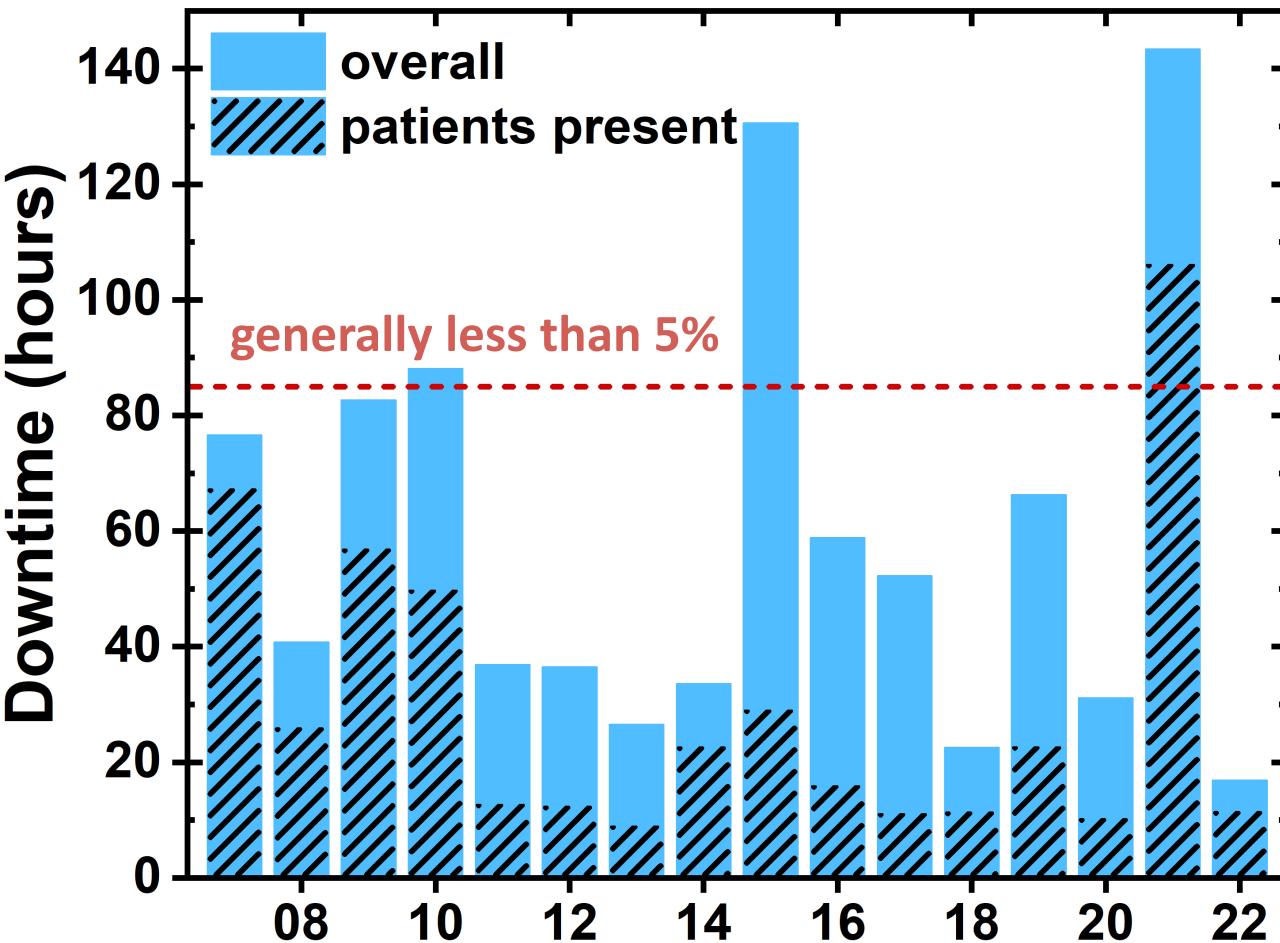
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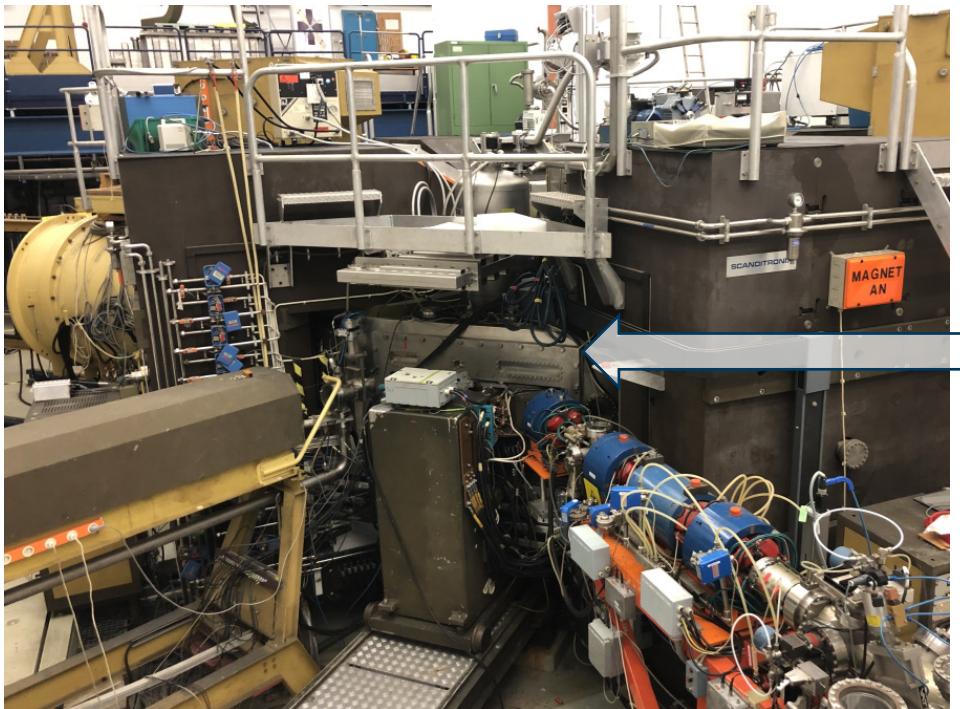
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- with few exceptions: downtime < 5%  
(Jan. – Nov. 2022: < 1%)
- good performance in spite of:
  - problems with suppliers  
(main issue: ultra long delivery times)
  - new safety regulations,  
requiring exchanges of perfectly working parts
- good performance thanks to huge efforts of the staff

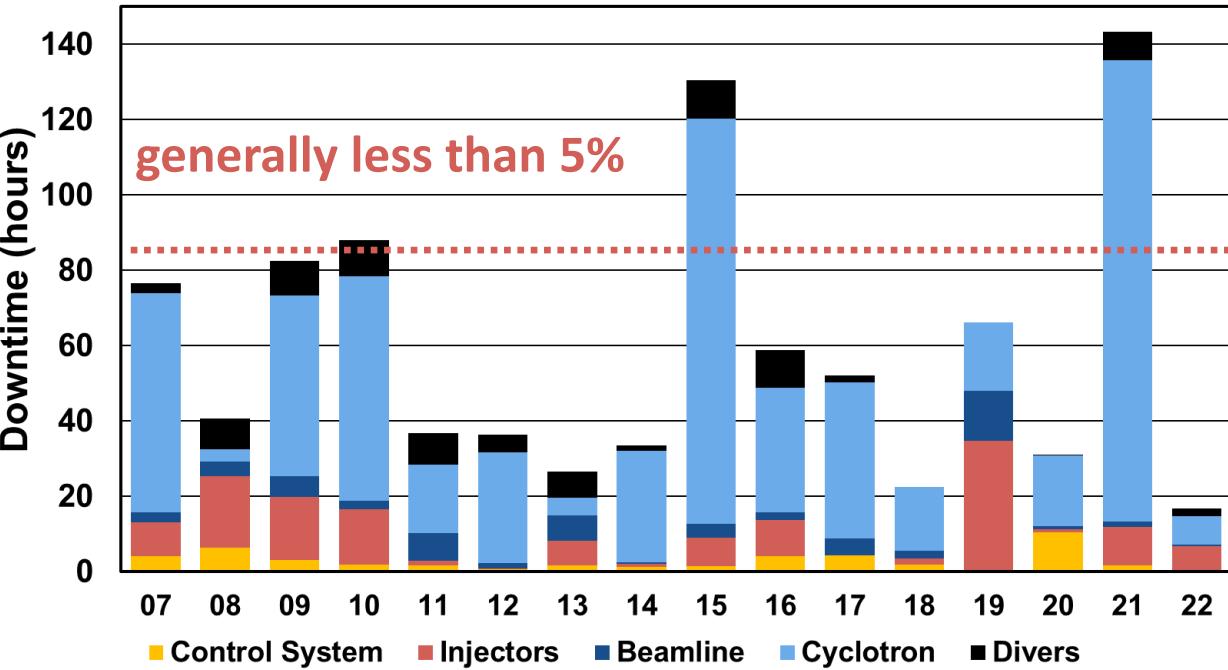


## Reasons for Down Time

- major events: cyclotron
- 2015: human error
  - increase of injector voltage too fast
- 2021: water leak in extraction coil
  - shifting of therapy week necessary  
(shifting counts as downtime)

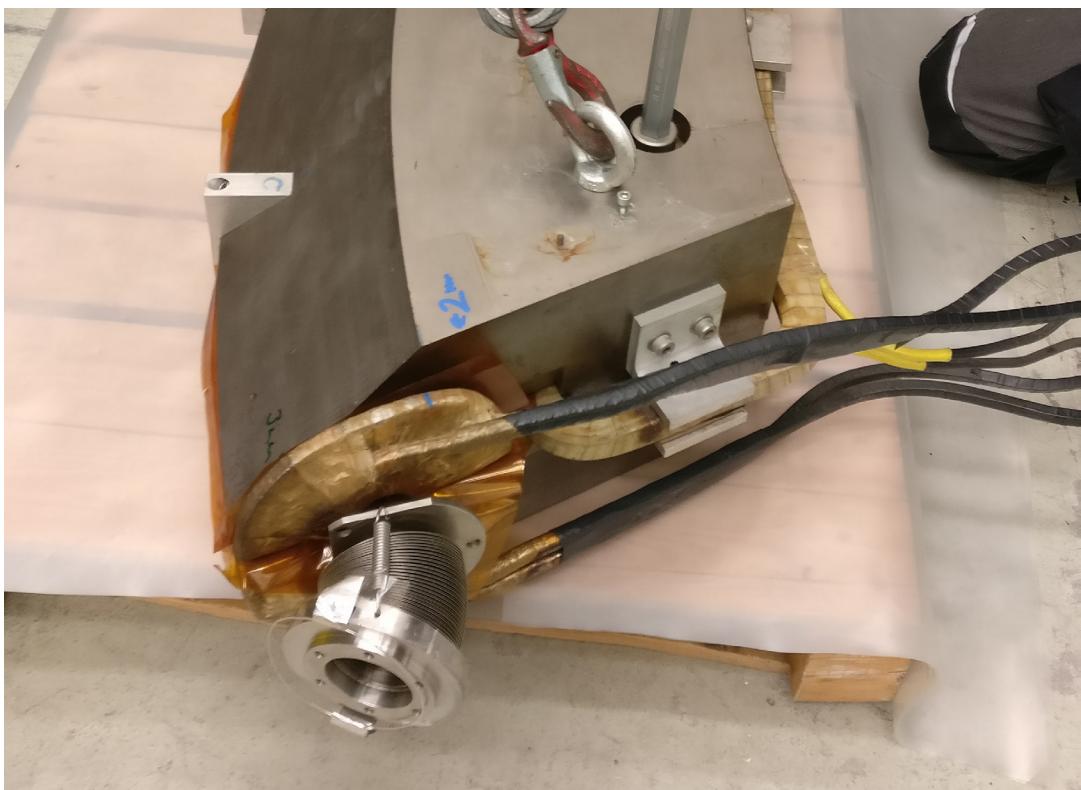


behind:  
extraction coil



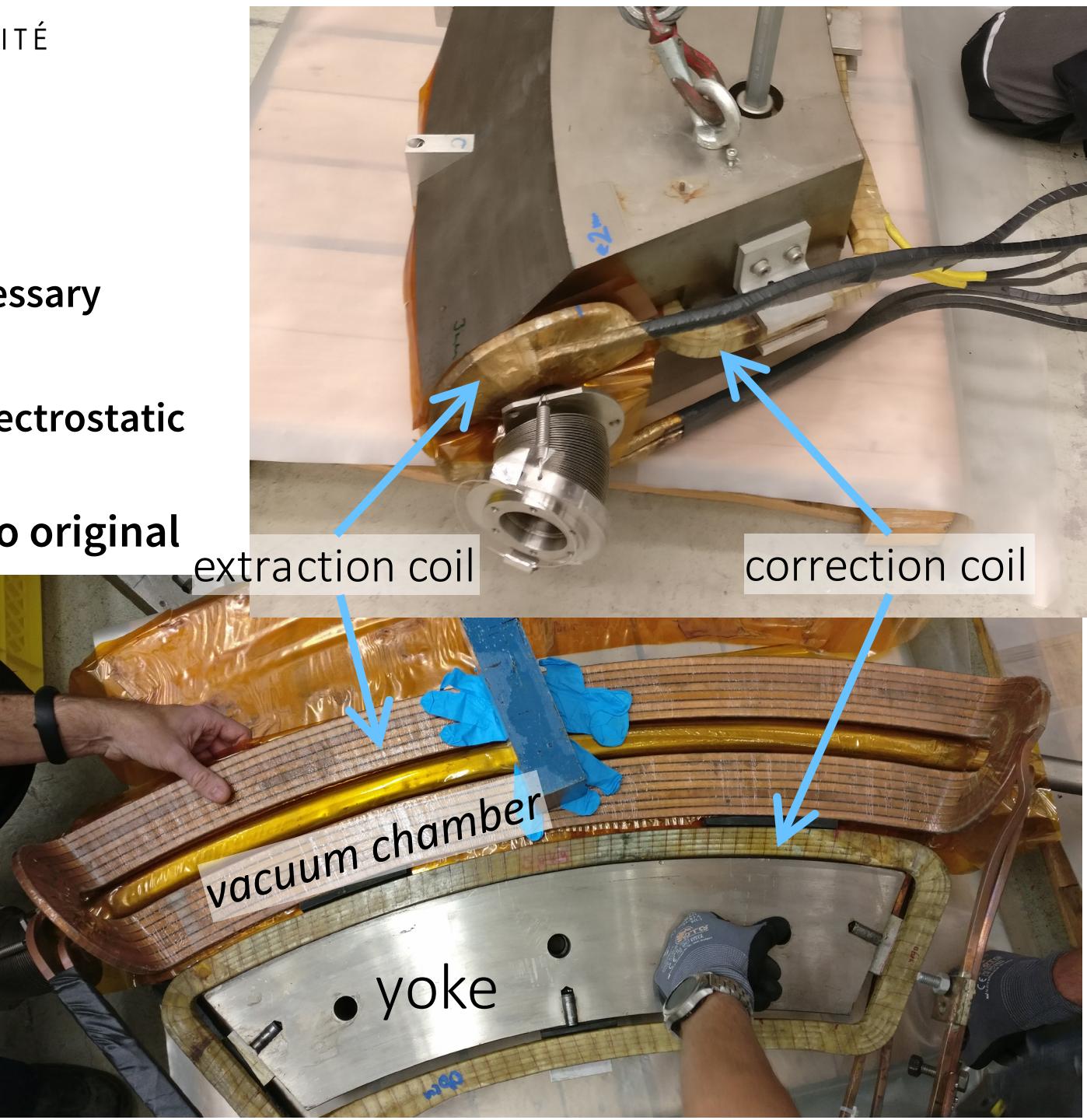
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- time consuming:
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  - after repair: pumping and conditioning of electrostatic elements



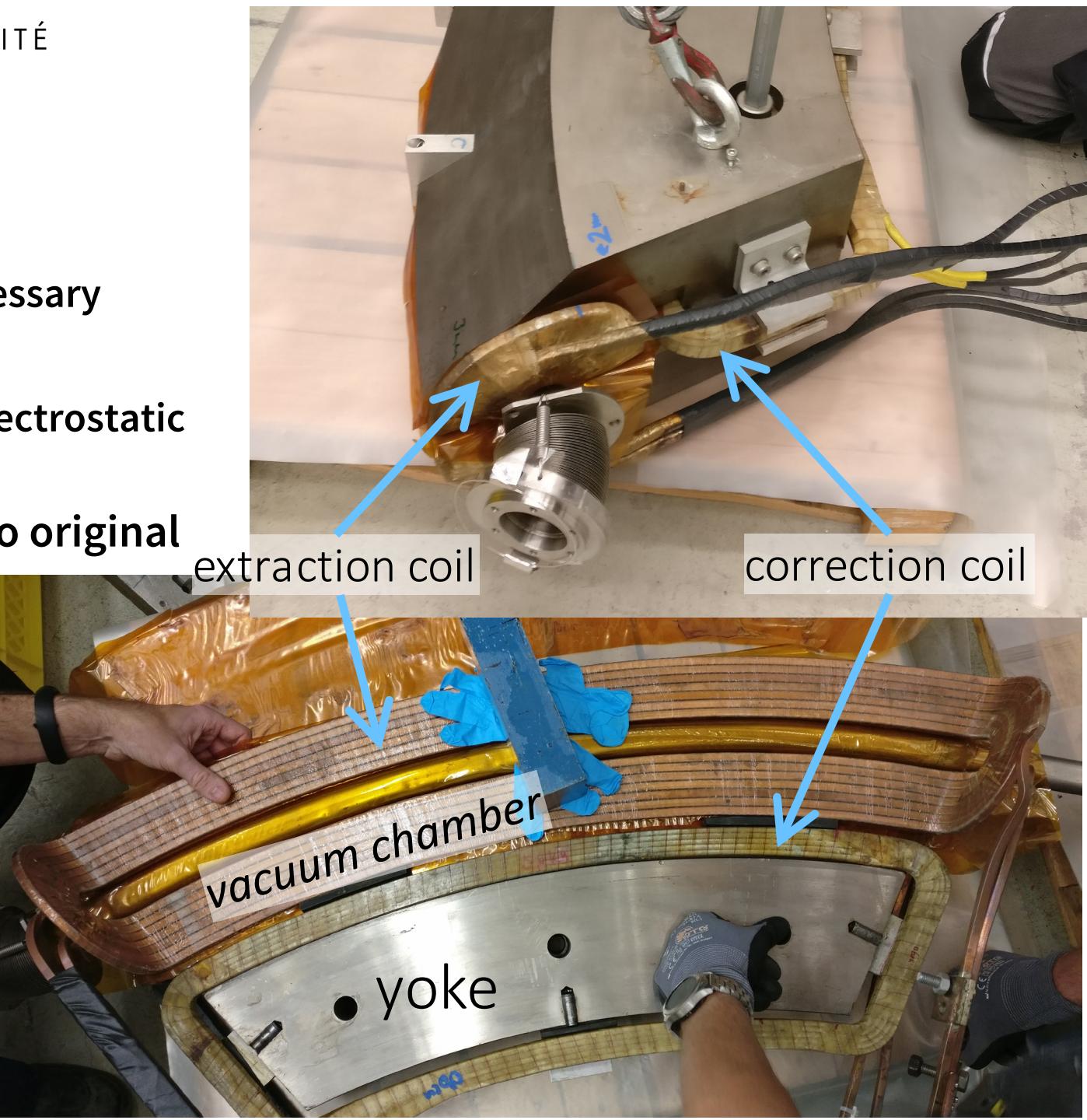
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- since several decades:  
correction coil never used,  
even not connected!



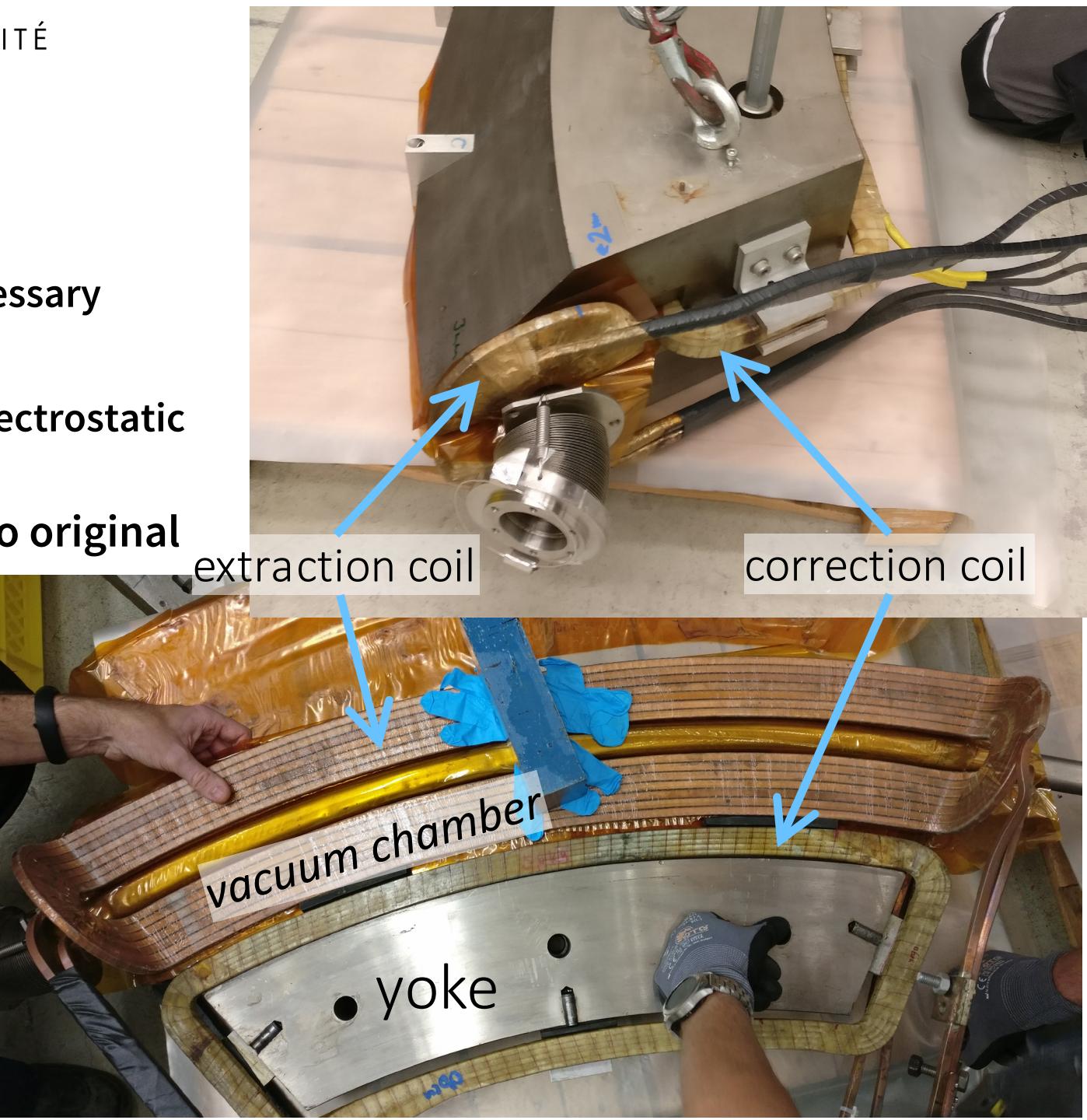
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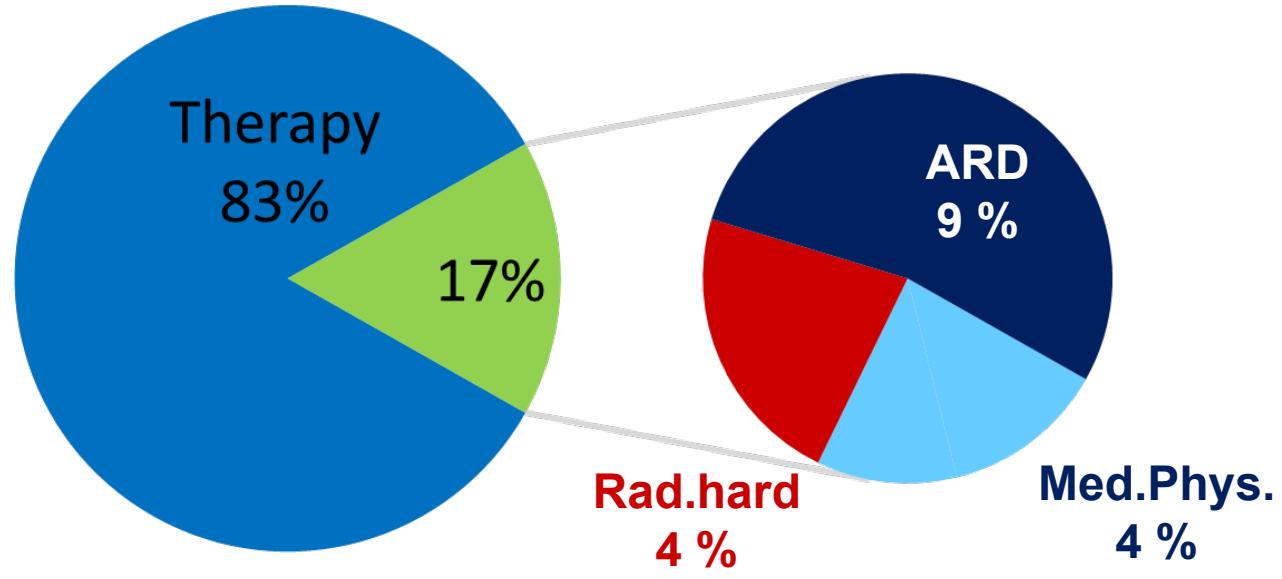
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otherwise no extraction possible!
- most likely: slightly different position  
of vacuum chamber



## Research & Development

- accelerator R & D (ARD):
  - beam delivery for Flash irradiations  
(extremely high doses in short times)  
see also poster MOP11 – Timo Fanselow
  - digitize beam profile monitors  
(poster WEP011 – Jürgen Bundesmann)
  - „Cocktail beams“: 90 MeV  ${}^4\text{He}^{2+}$  and 45 MeV  $\text{H}_2^+$



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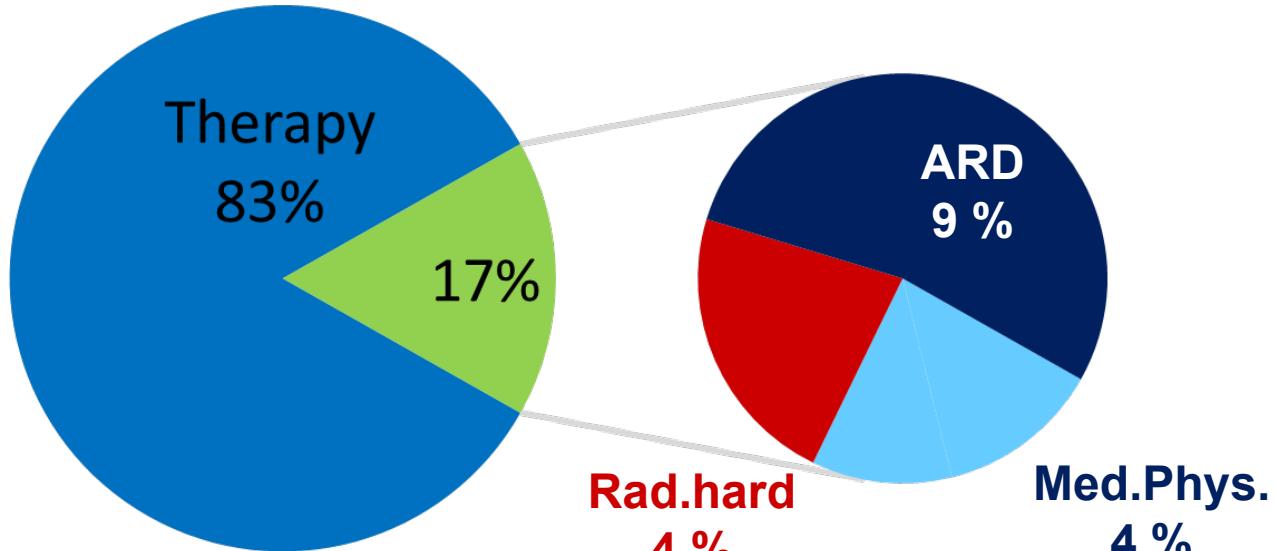
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- determination for appropriate material for artificial lenses in ocular proton therapy

- depth profile camera

(talk TUB02 – Alina Dittwald)



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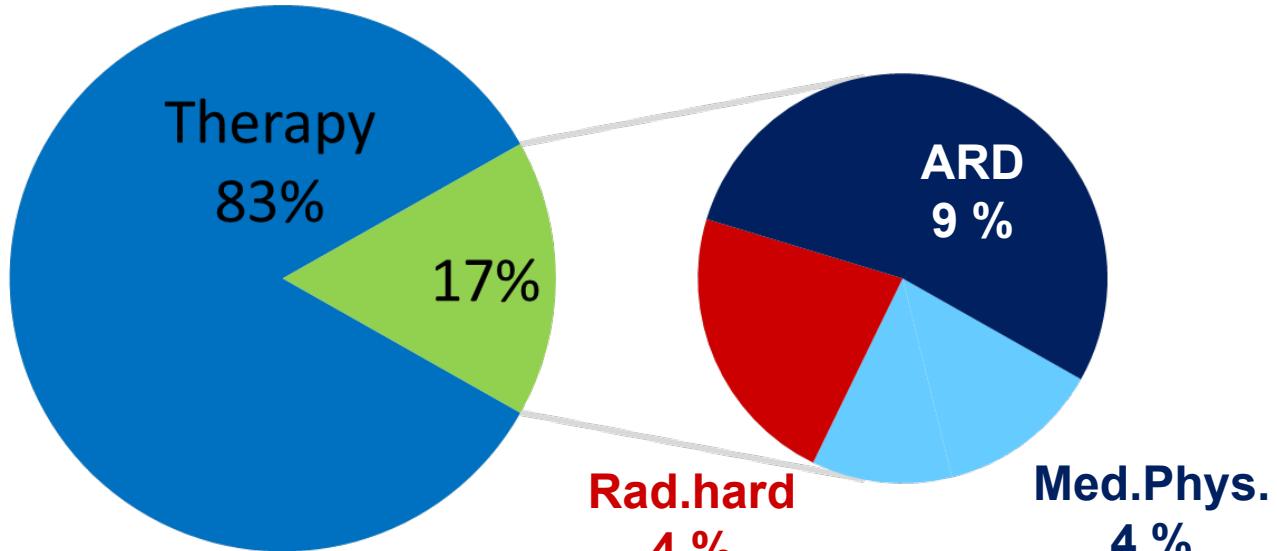
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- Radiation hardness tests:

external users, e.g. DLR, universities, industry



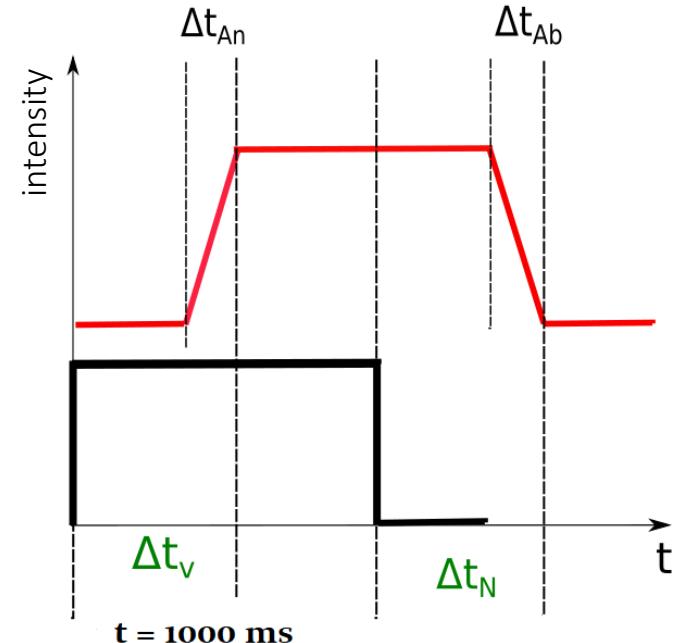
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intensity

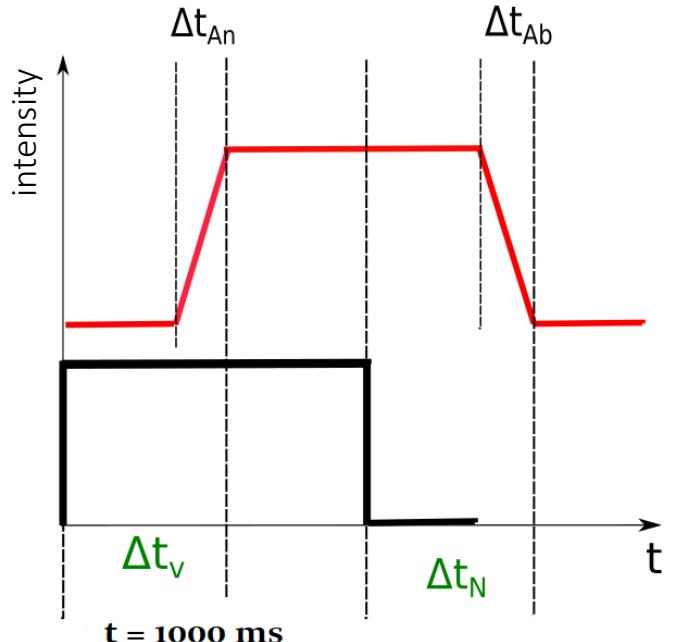
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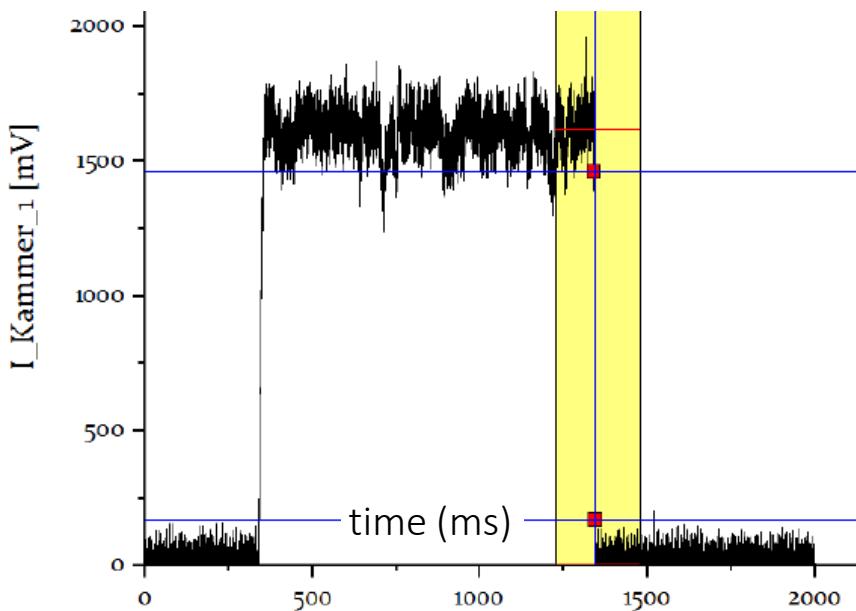
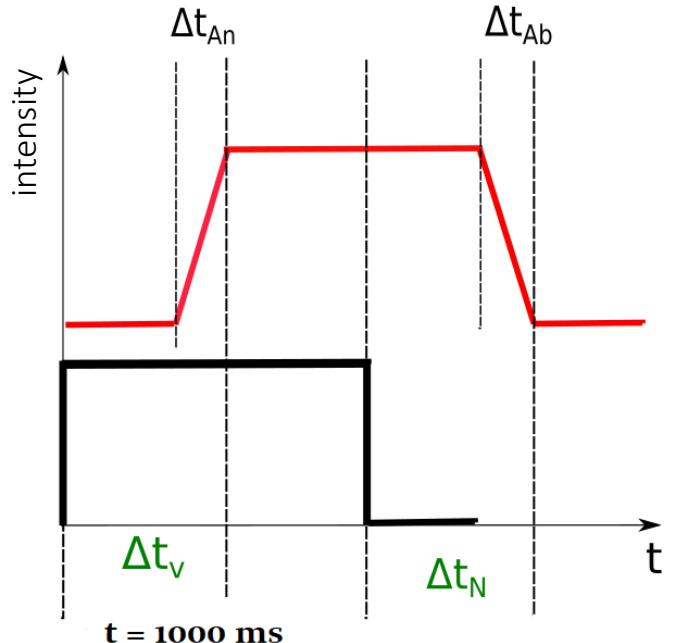
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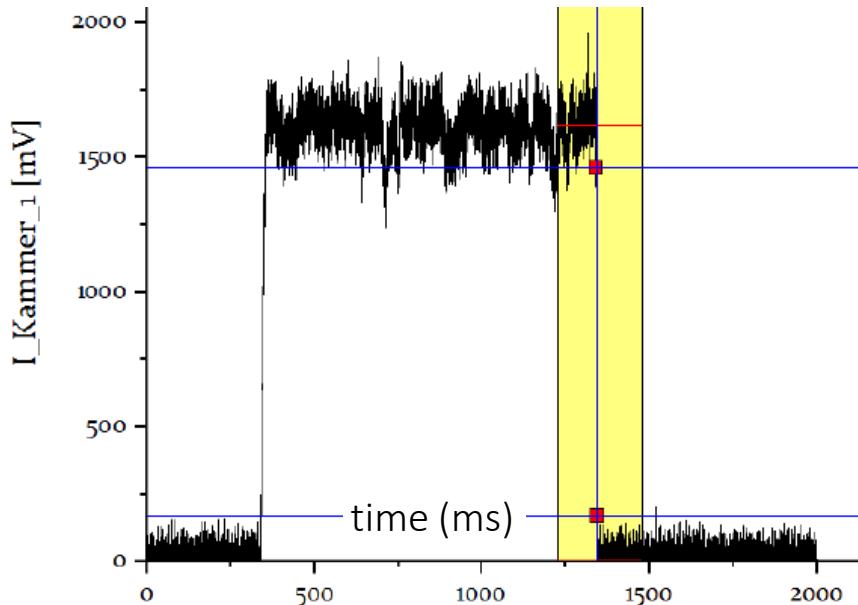
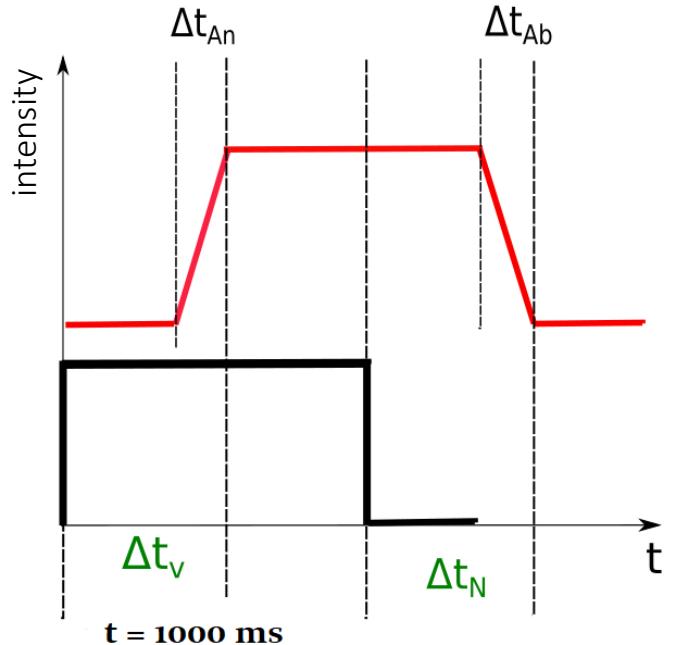
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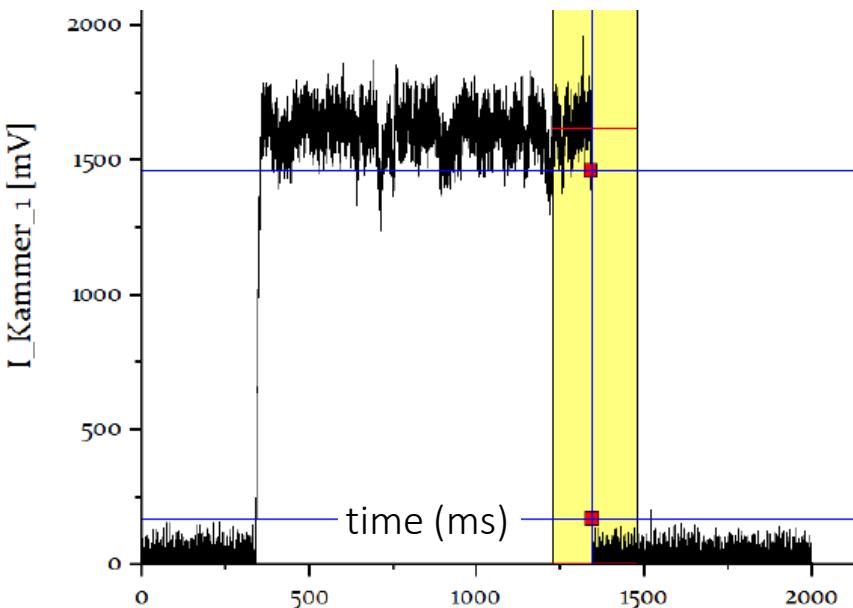
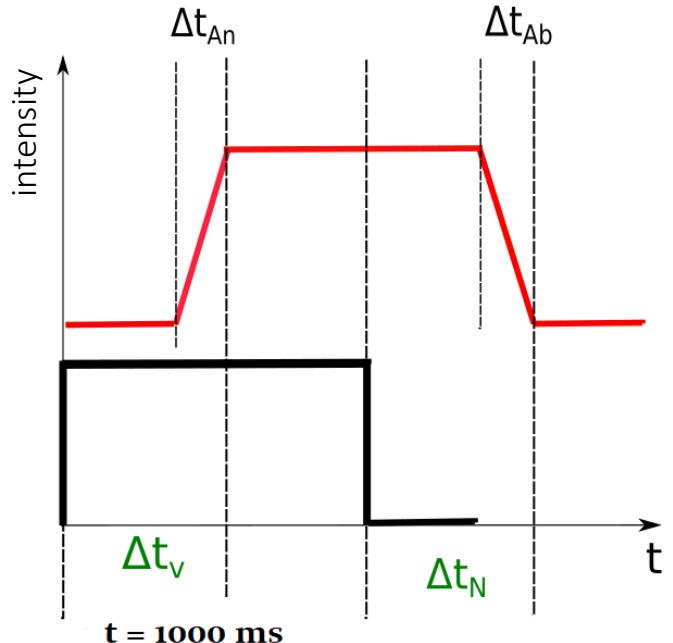
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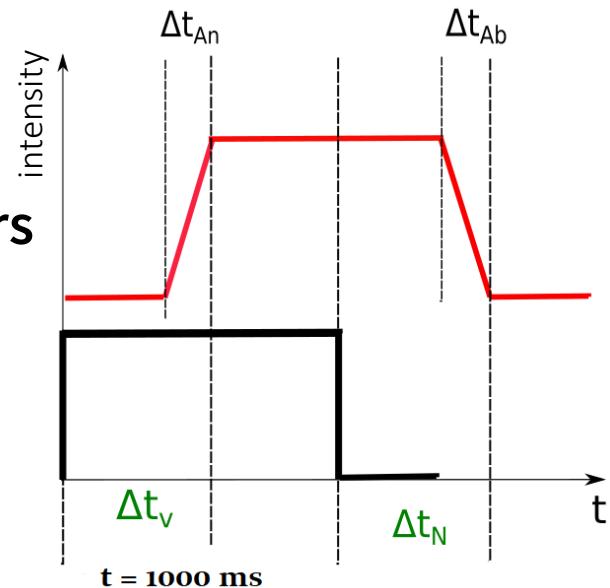
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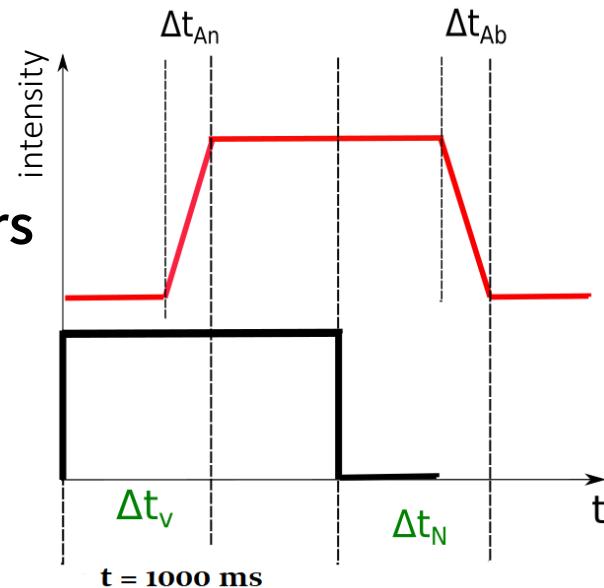
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- two ionization chambers for beam monitoring
- FPGA board processes signals of Faraday Cup (FC) and ionization chambers



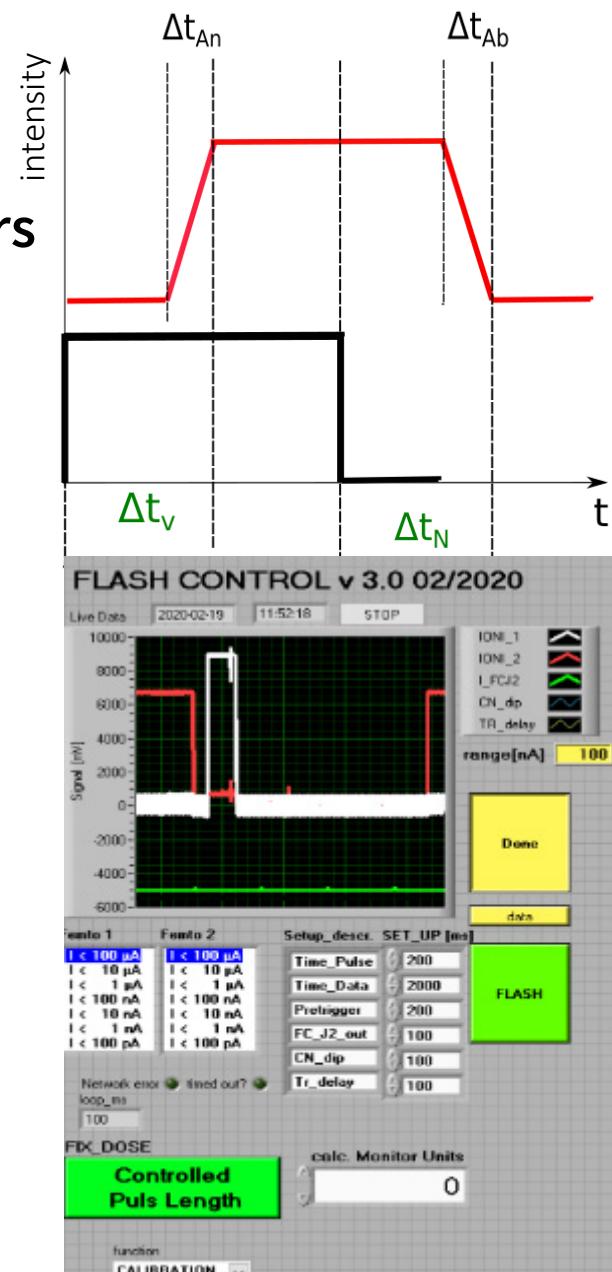
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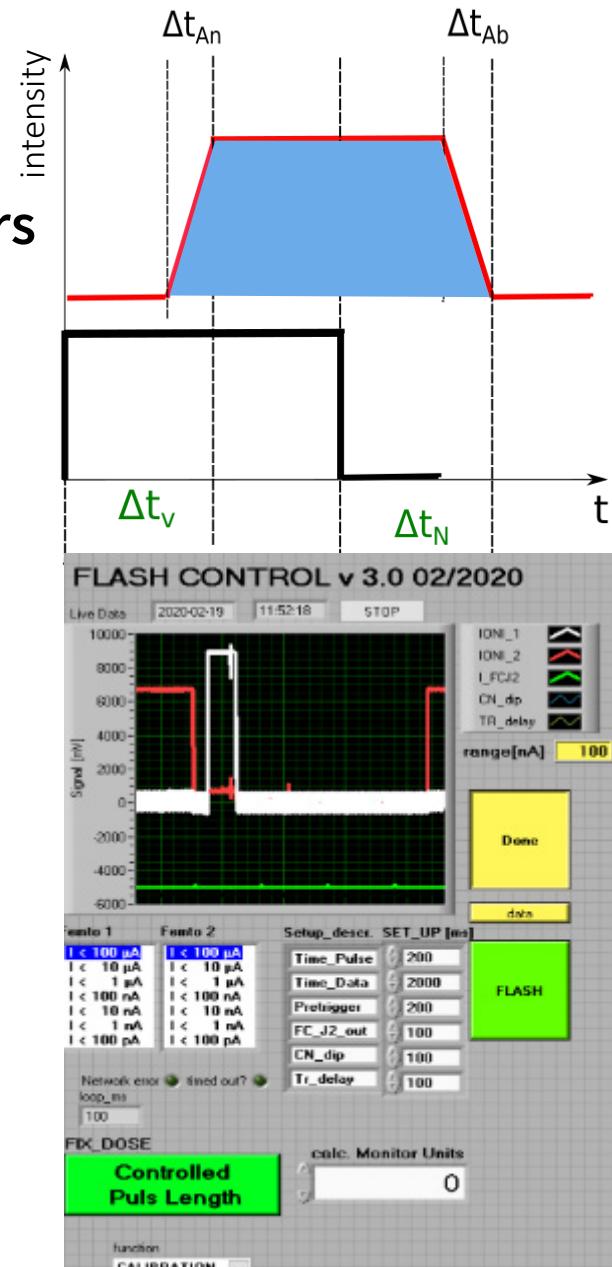
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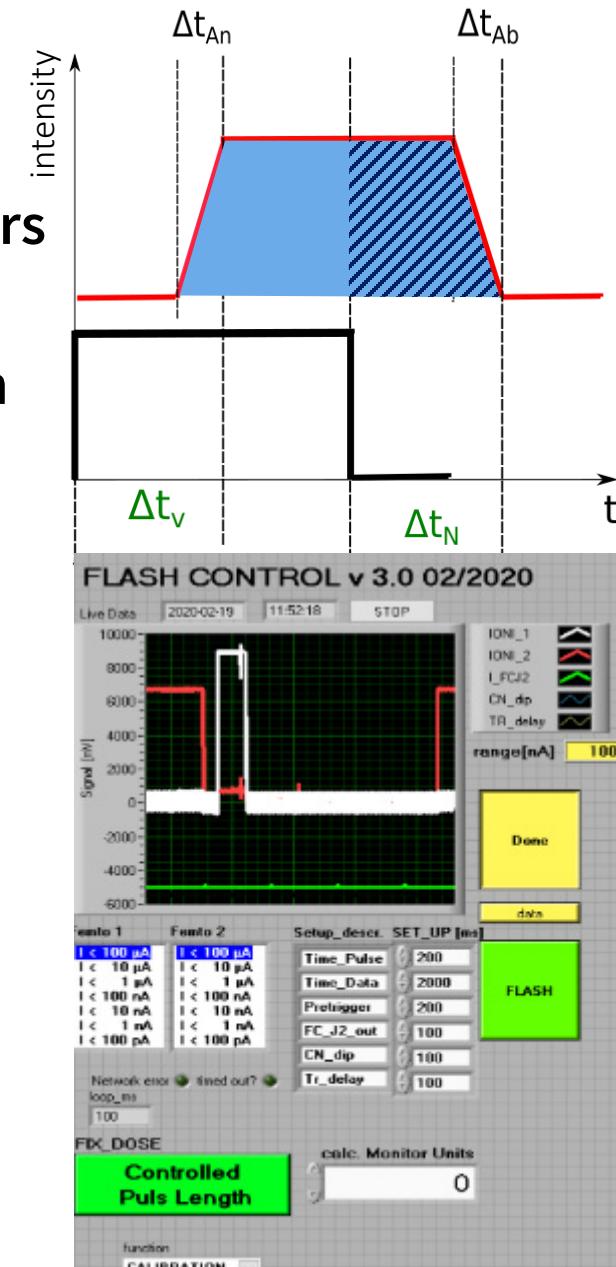
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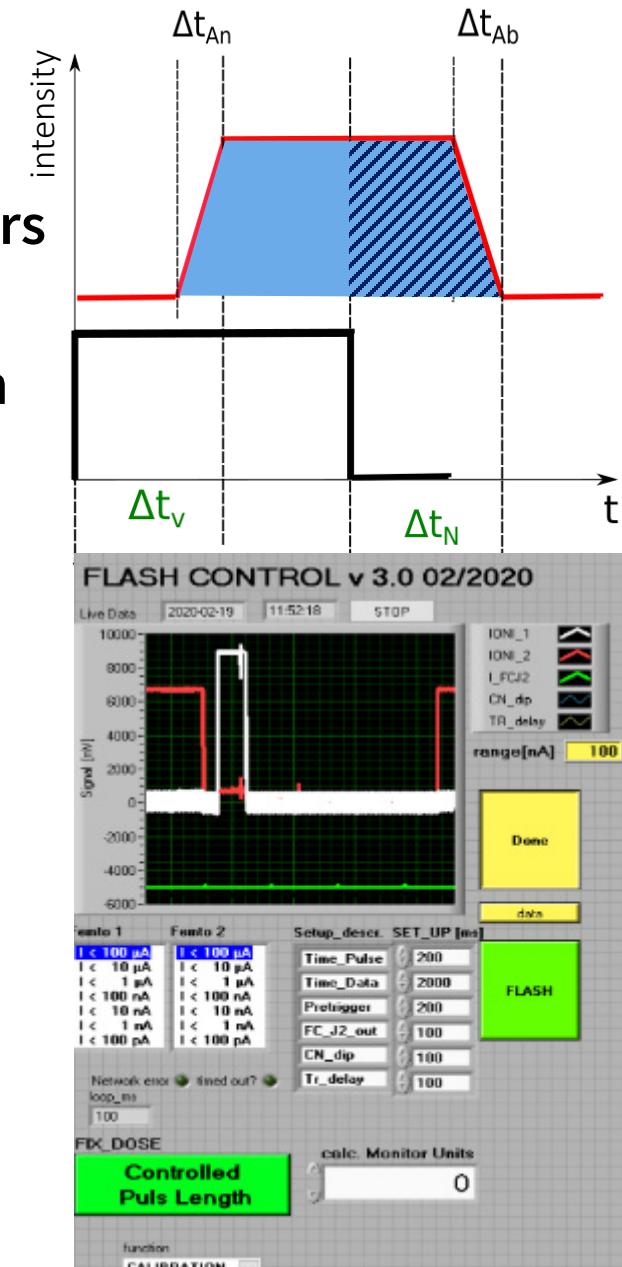
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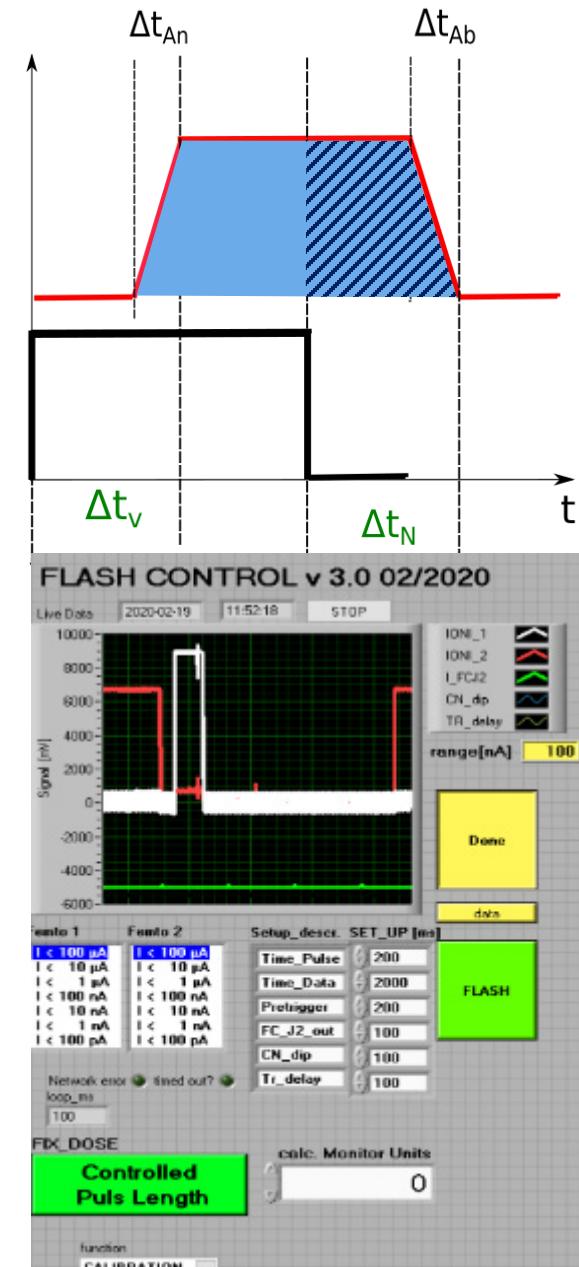
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- defines switch-off strategy: in “dose mode” the stop-signal is given for corresponding dose minus expected excess counts



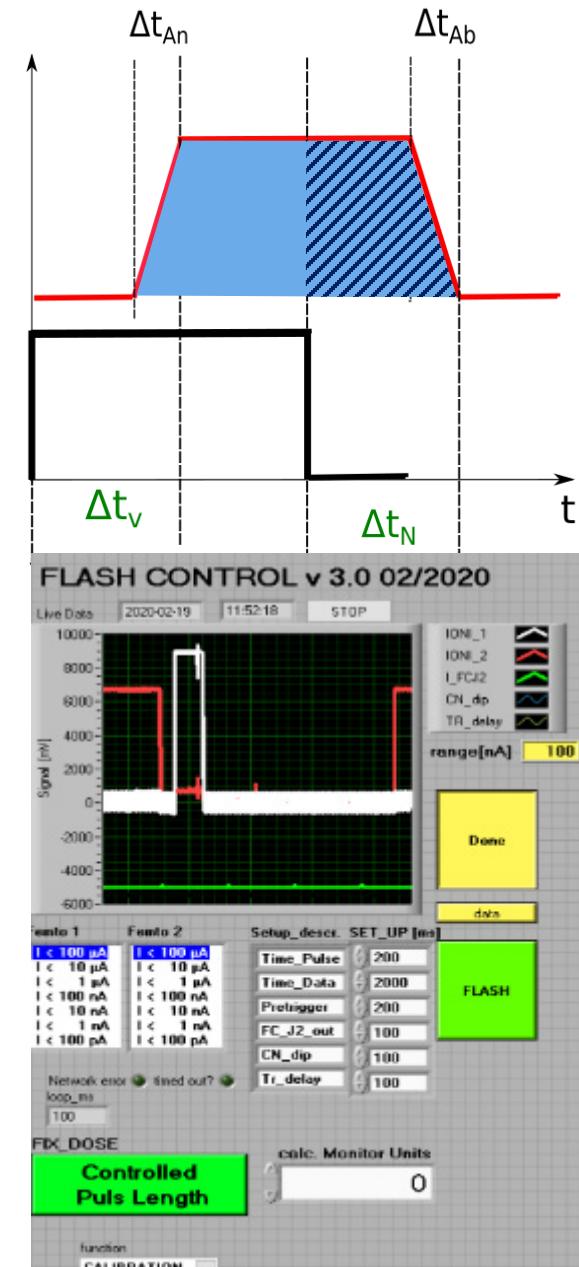
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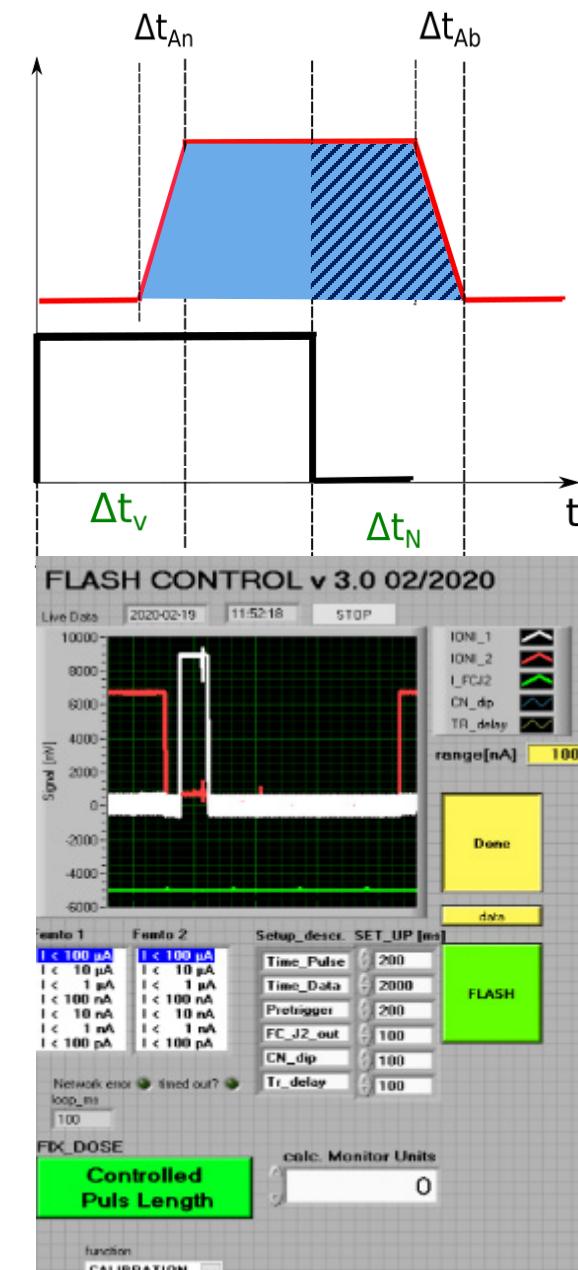
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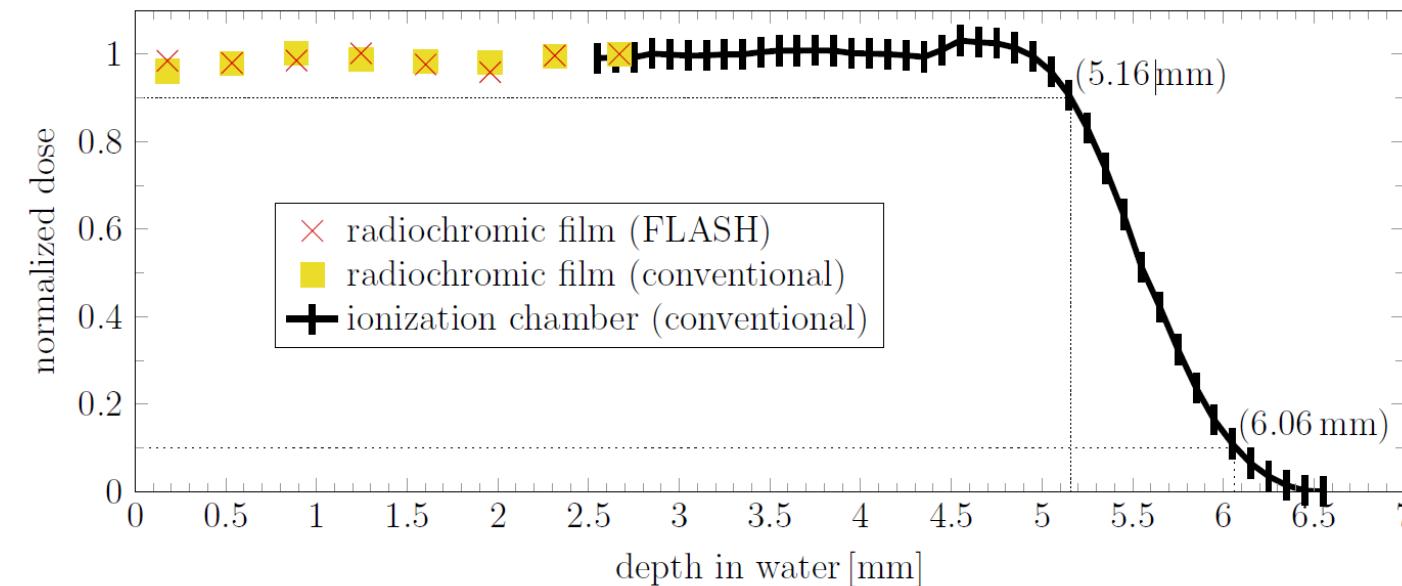
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- Flash ~ 50 nA , dose rate 75Gy/s - 30 trial runs to estimate error:  
**14.9 Gy with a standard deviation of 0.6%**



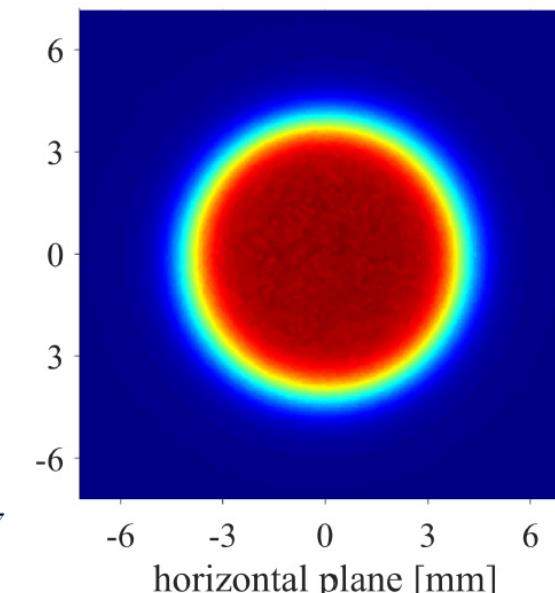
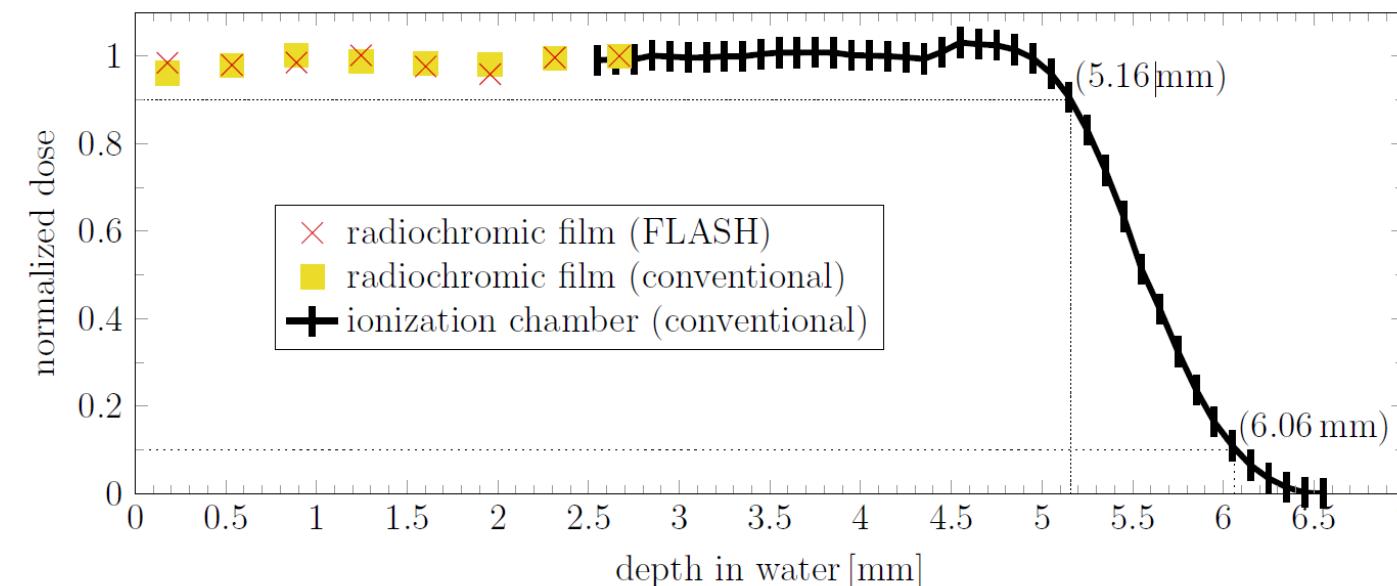
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- modulator wheel for Spread Out Bragg Peak (960 SOBP/s)



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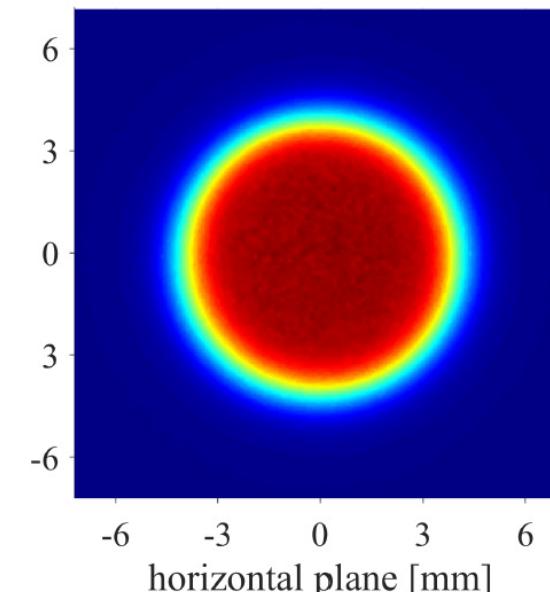
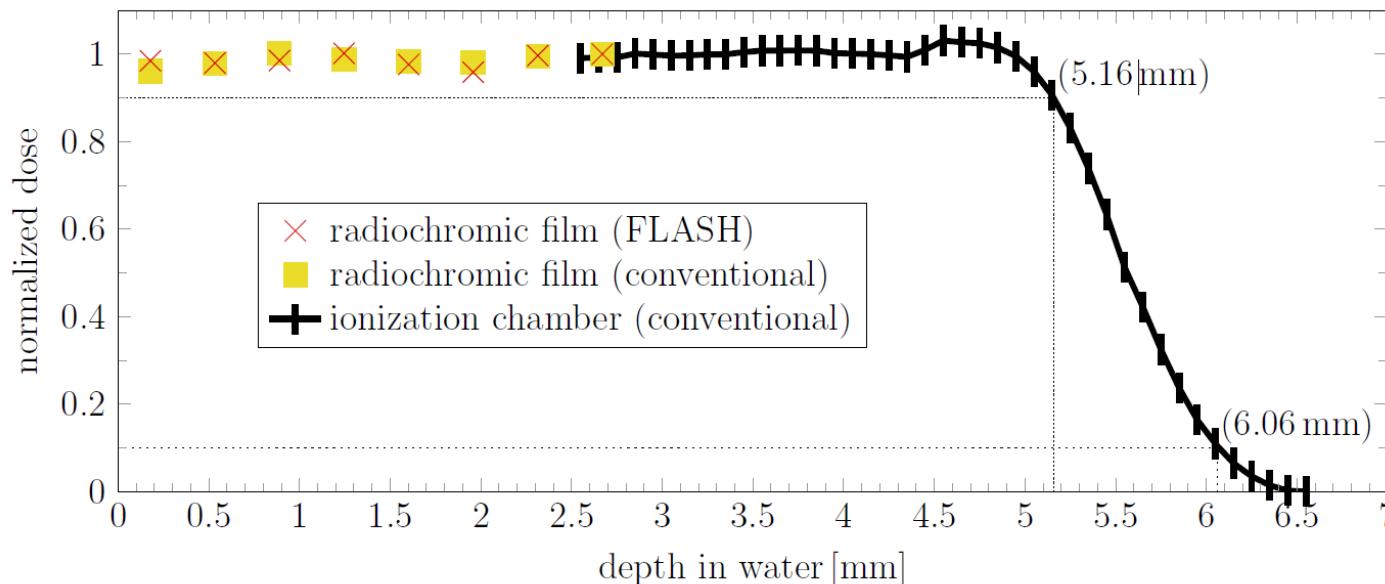
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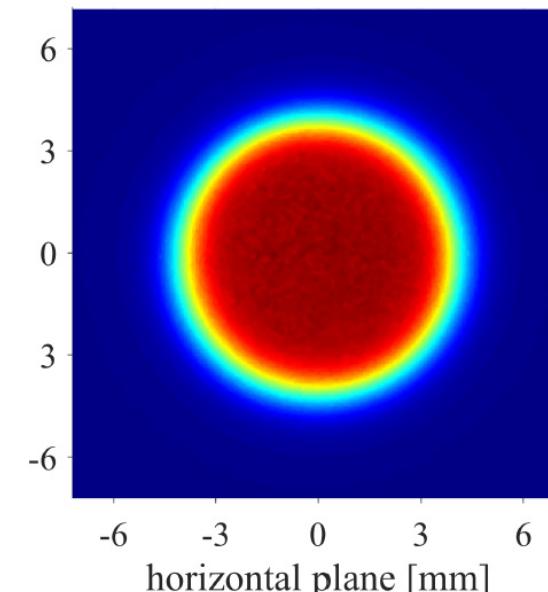
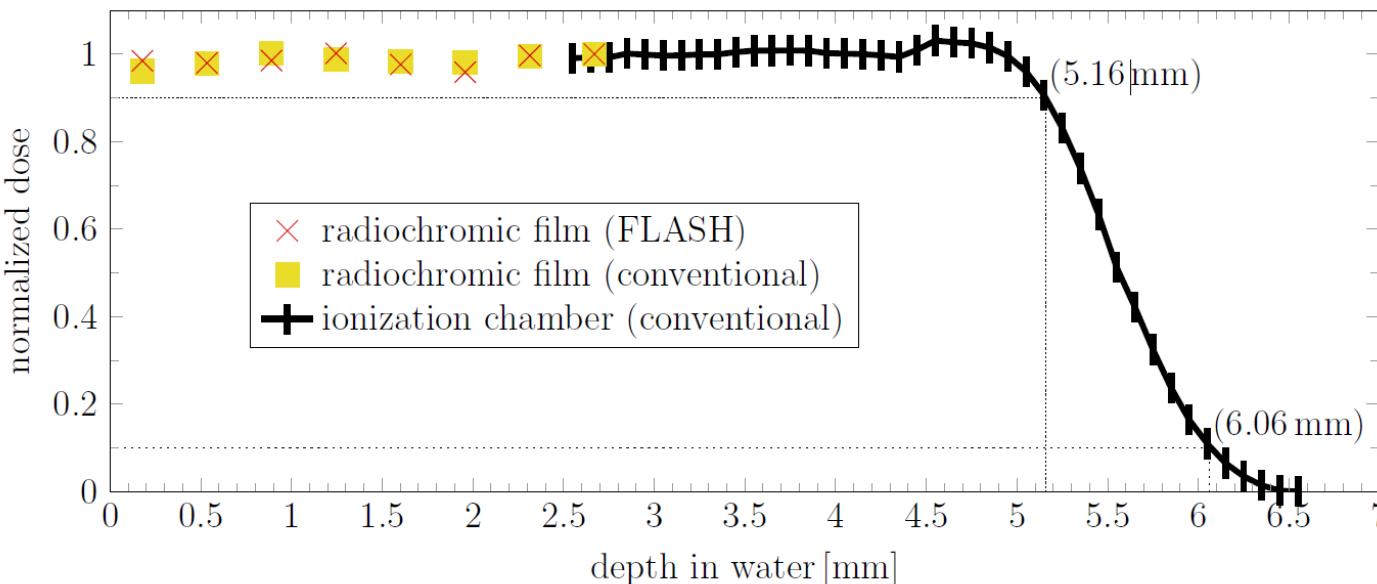
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confinement of proton field to **single** mouse eye  
G. Kourkafas et al.,  
Med. Phys. 2021



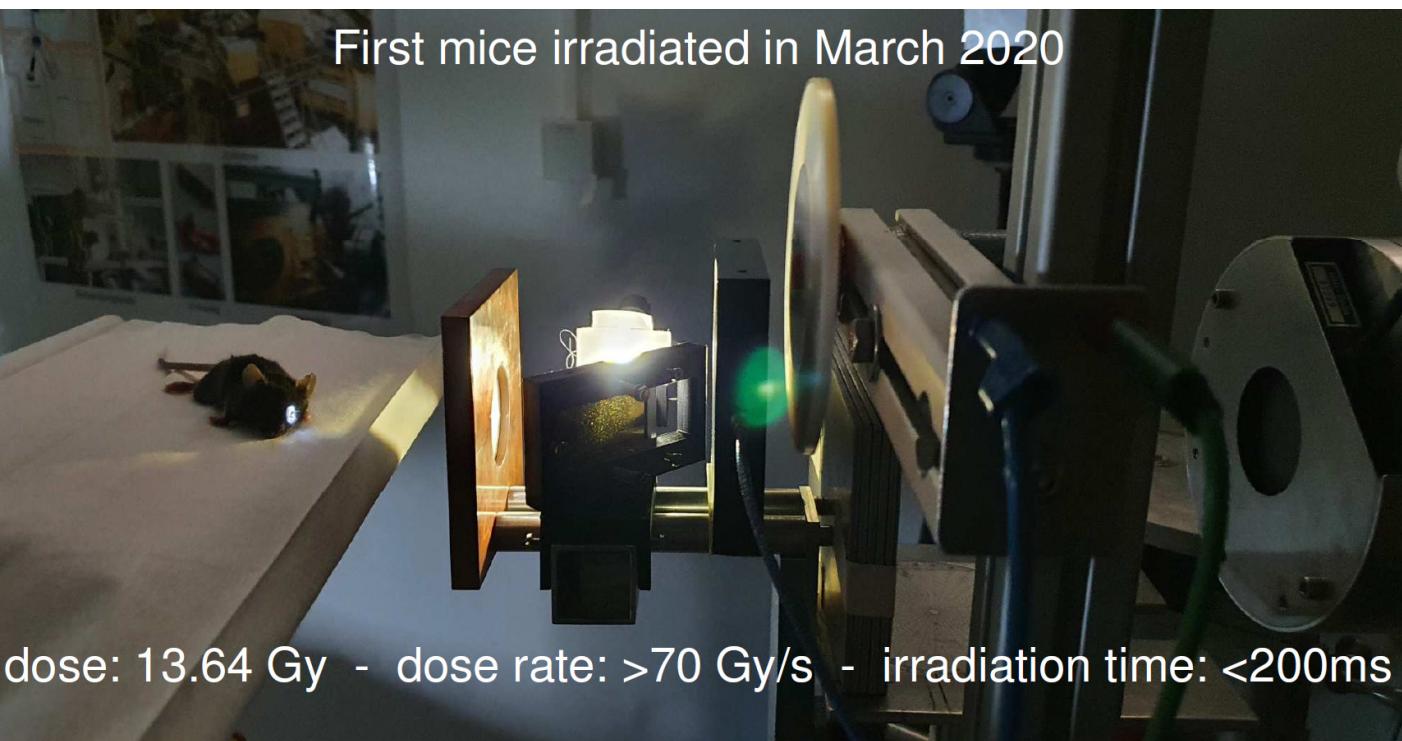
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  - modulator wheel for Spread Out Bragg Peak (960 SOBP/s)
  - collimator: 6.3 mm PTV , 1.7 mm lateral penumbra (90% to 10% isodose)
  - Early normal tissue reactions after FLASH proton beam exposure of mice eye: preliminary results from in-vivo investigation using optical coherence tomography
- Flash Radiotherapy & Particle Therapy, 30.11.22 – 2.12.22, Vienna
- confinement of proton field to **single** mouse eye  
G. Kourkafas et al., Med. Phys. 2021



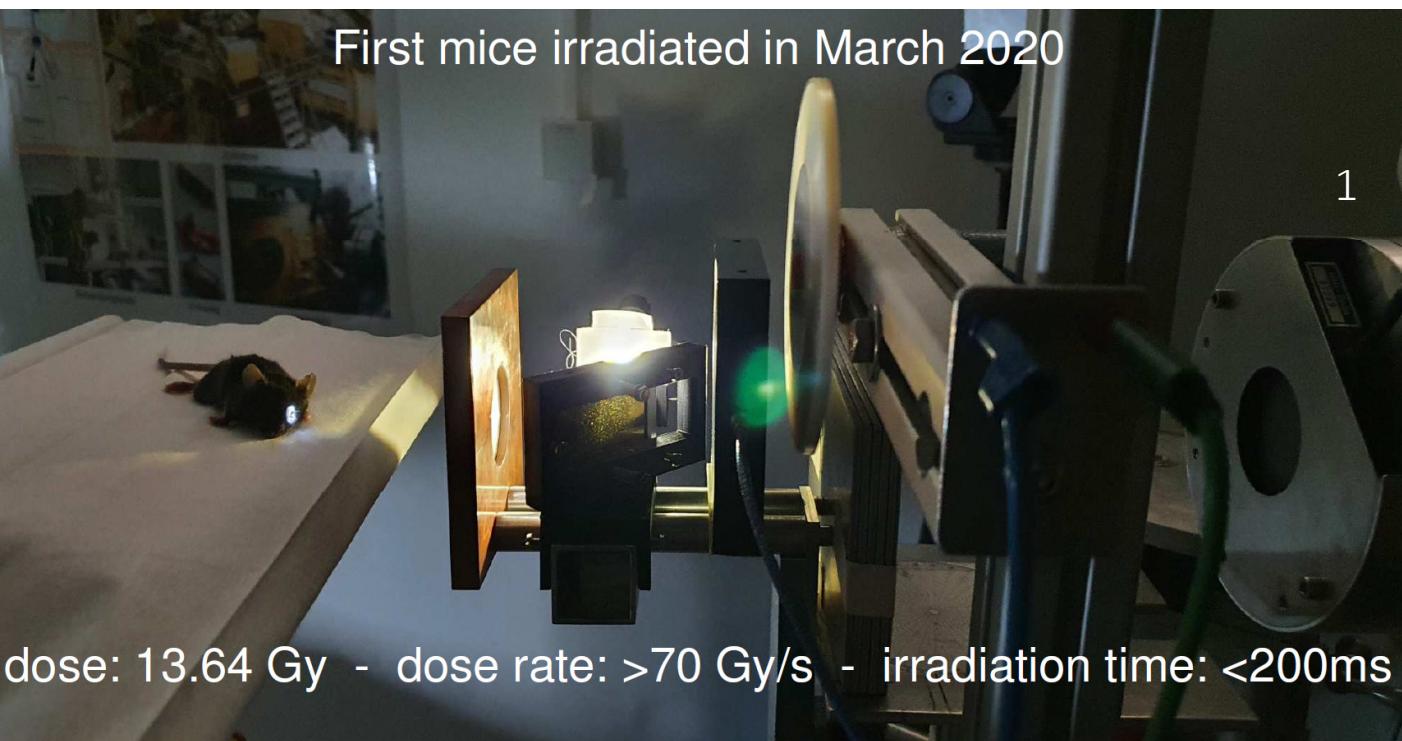
## beam delivery for FLASH irradiations – irradiation of mice eyes

- Flash not feasible in treatment room without changes
- new set-up at experimental station:
  - control group with conventional irradiation: 15 Gy in 60s (0.25 Gy/s)
  - flash irradiations: 15 Gy in 200 ms (75 Gy/s)
- in total: ~ 80 mice



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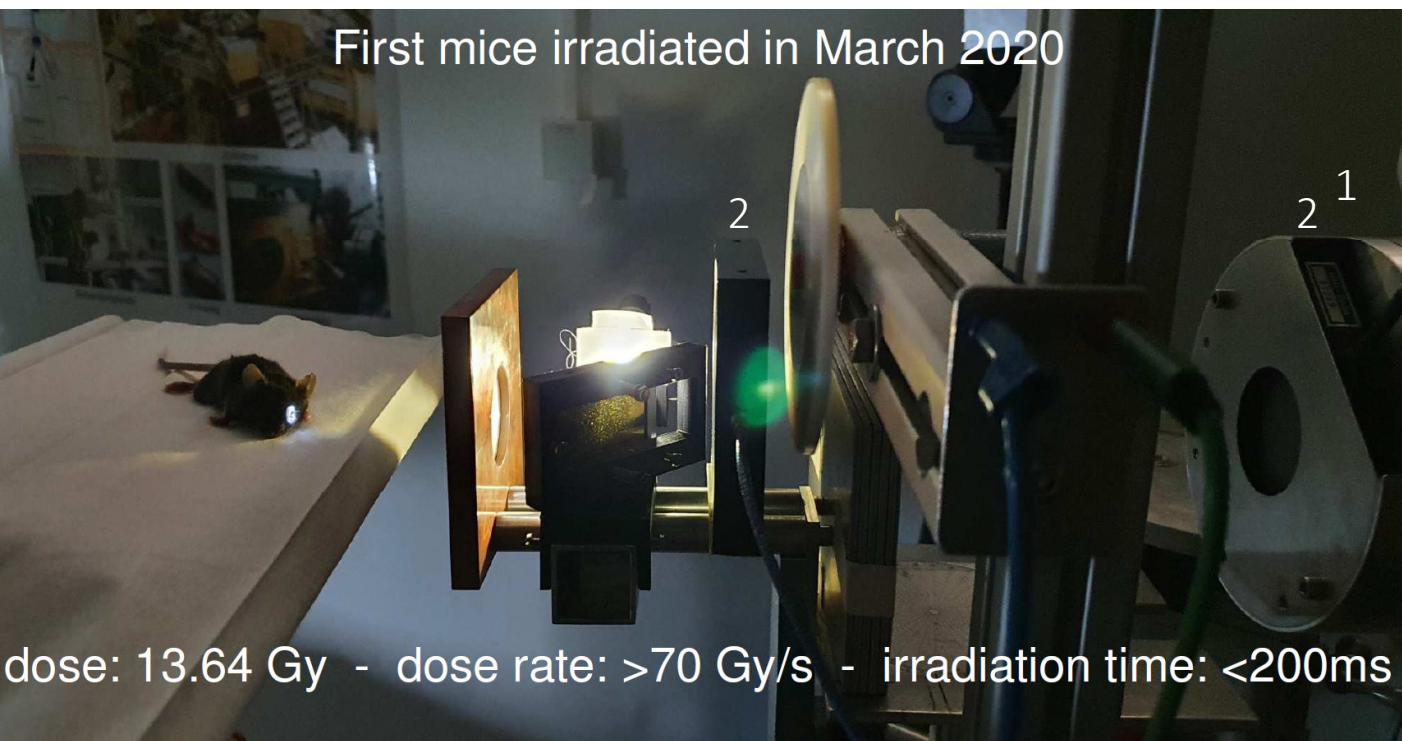


1. vacuum window

dose: 13.64 Gy - dose rate: >70 Gy/s - irradiation time: <200ms

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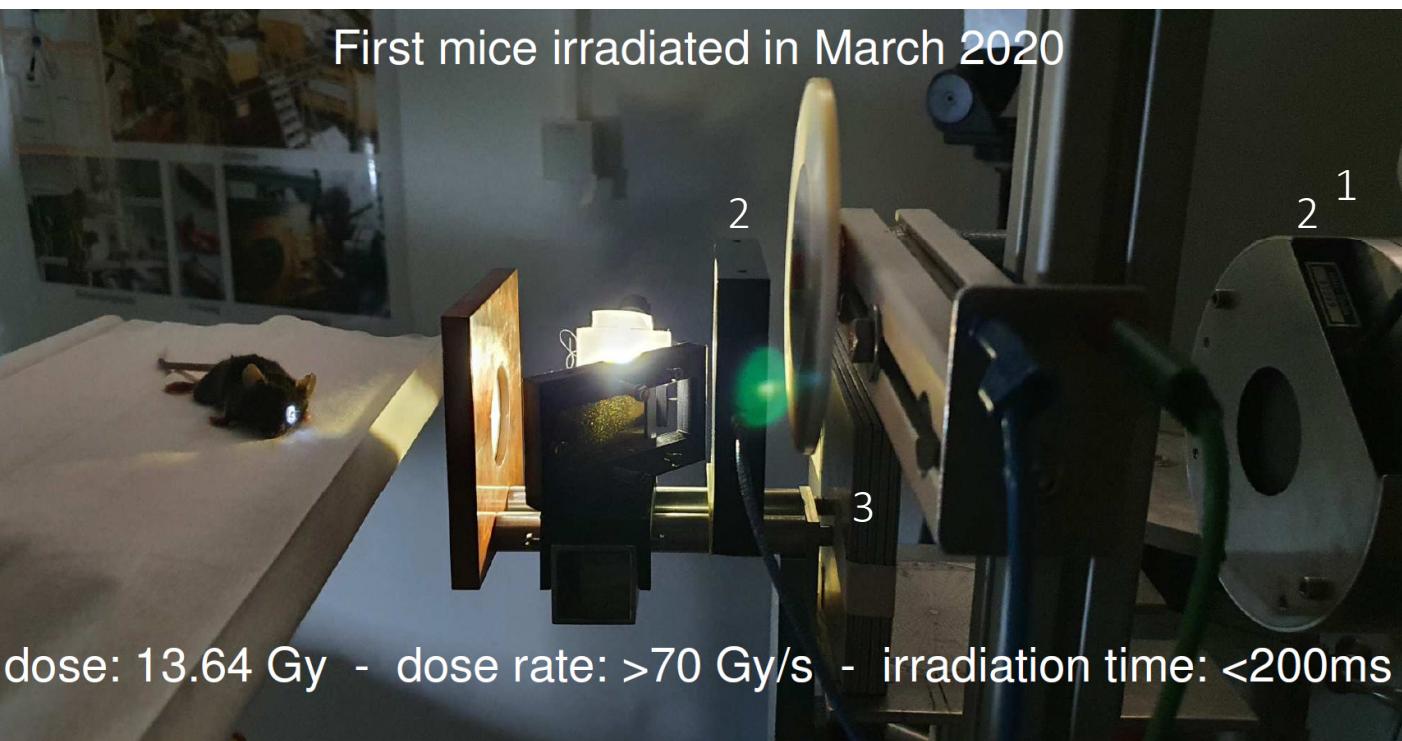
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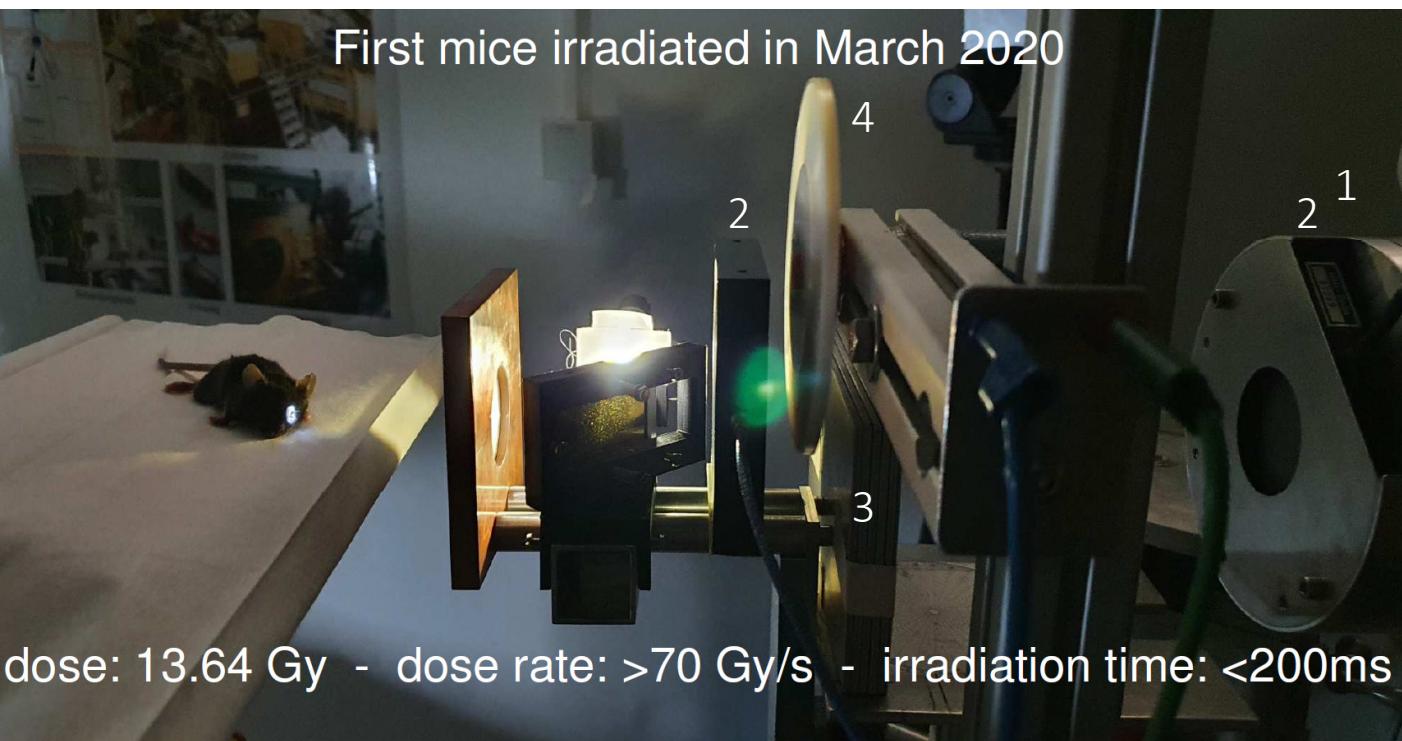
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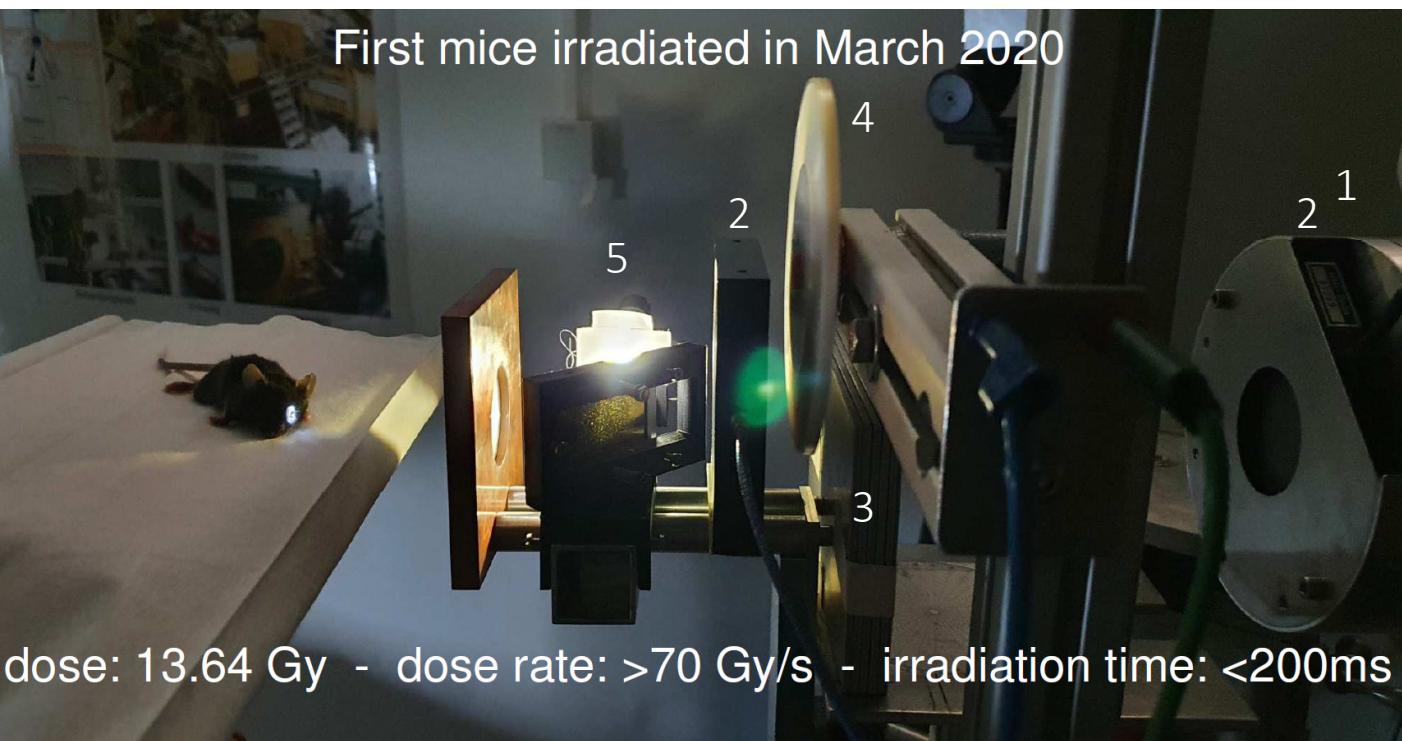
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(periods: 48; rotation speed: 20 Hz)

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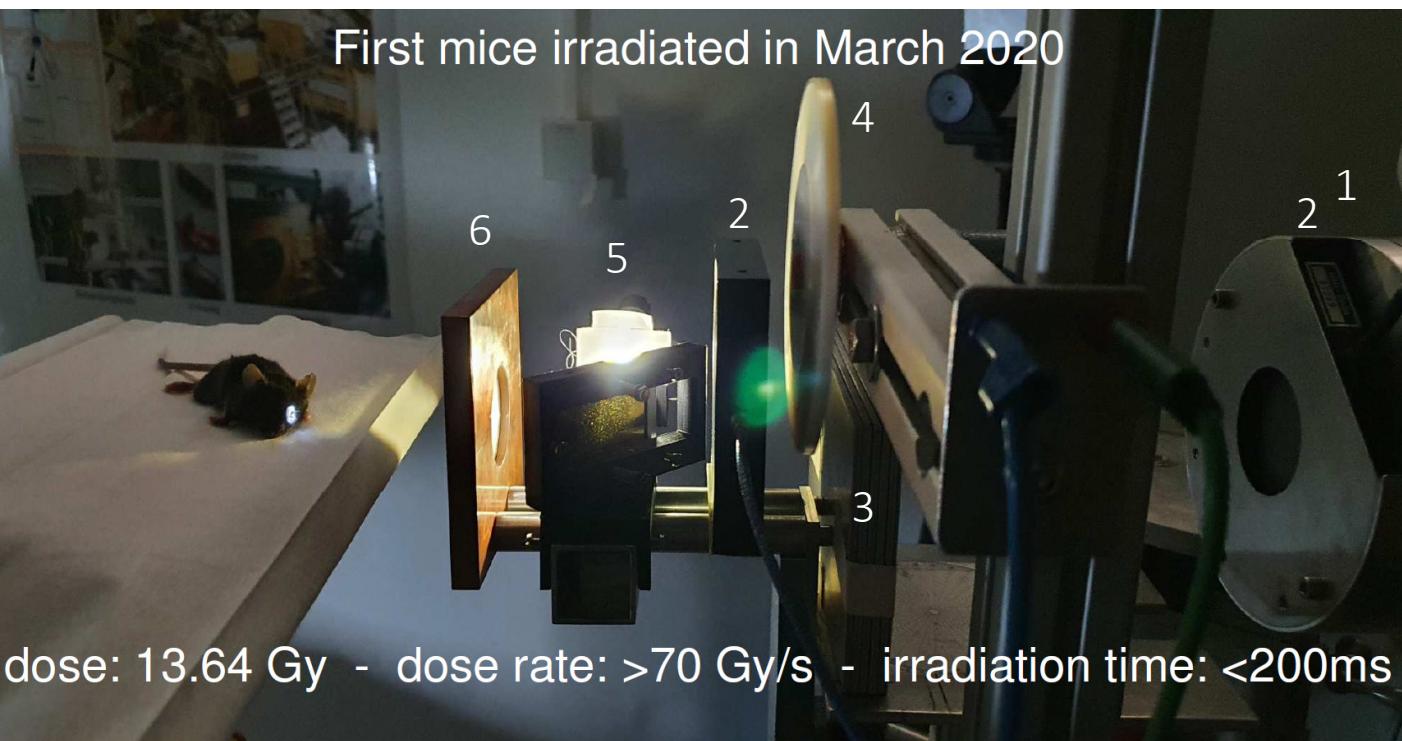
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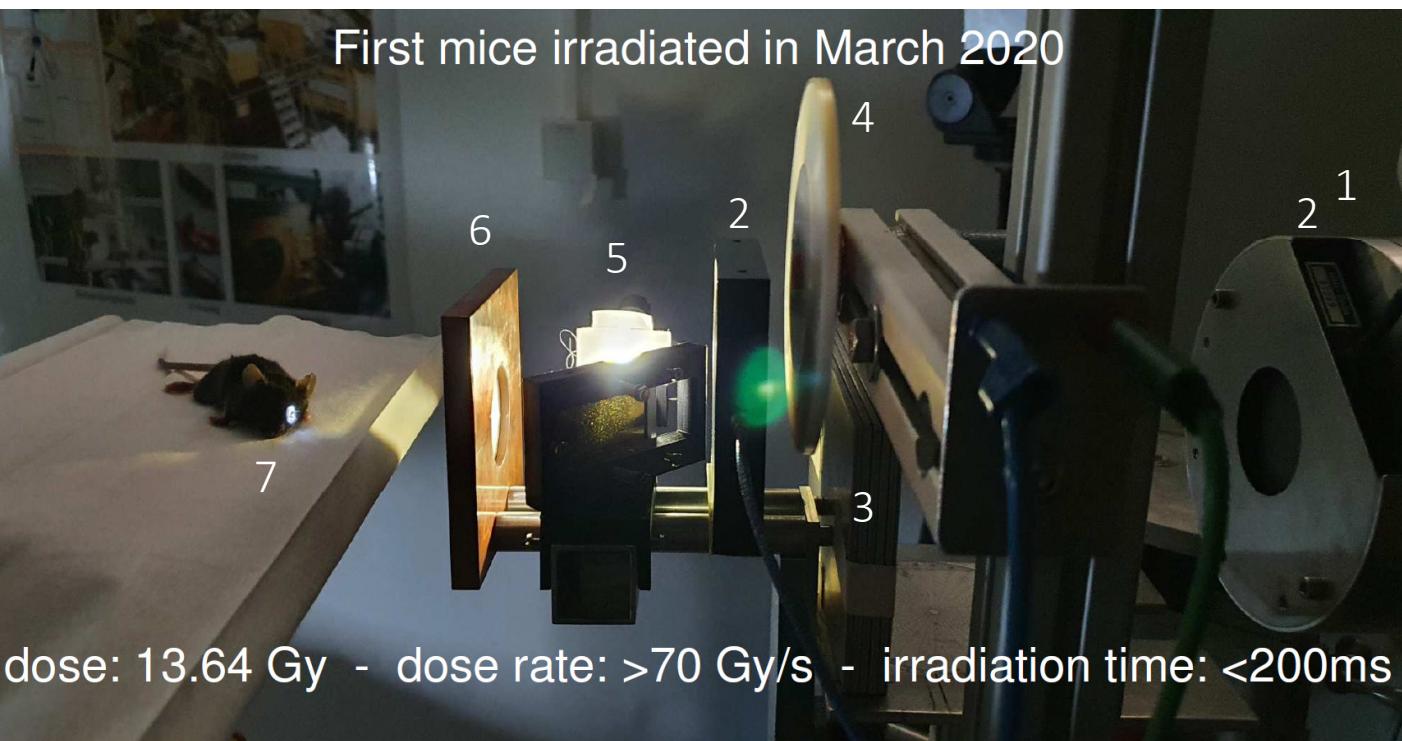
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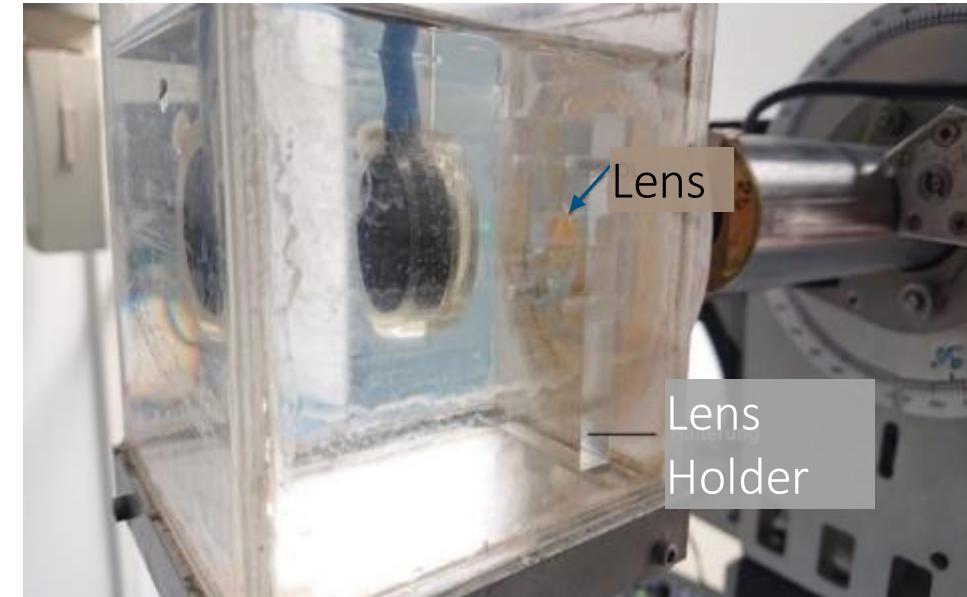
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7. anesthetized mouse with light field for positioning

## beam delivery for FLASH irradiations – further developments

- currently ideal irradiation time unknown (definition Flash: < 1 s)
- indications that irradiation times should be shorter than 100 ms
  - mechanical beam stop too slow
  - electrical beam deflector
- recently: electrical beam deflector only for the Van-de-Graaff injector available single pulses with 1ns pulse width and 2.4 MHz repetition rate feasible
- now: installation of a second chopper on the DC-beam from the Tandetron  
MOP11 – Timo Fanselow: Design and Operation of the new fast beam chopper between Tandetron and cyclotron
- replace modulator wheel with ridge filters
- near future: irradiations of sarcoma and uveal melanoma organoids

## determination for appropriate material for artificial lenses in ocular proton therapy

- artificial lenses from various manufacturers irradiated with protons under conventional and Flash mode
- lenses mounted in front of the water phantom with Markus chamber for absolute dosimetry
- identical irradiation field size for both modes
- conventional: 60 Gy, dose rate 0.2 Gy/s
- Flash: 60 Gy, dose rate 70 Gy/s



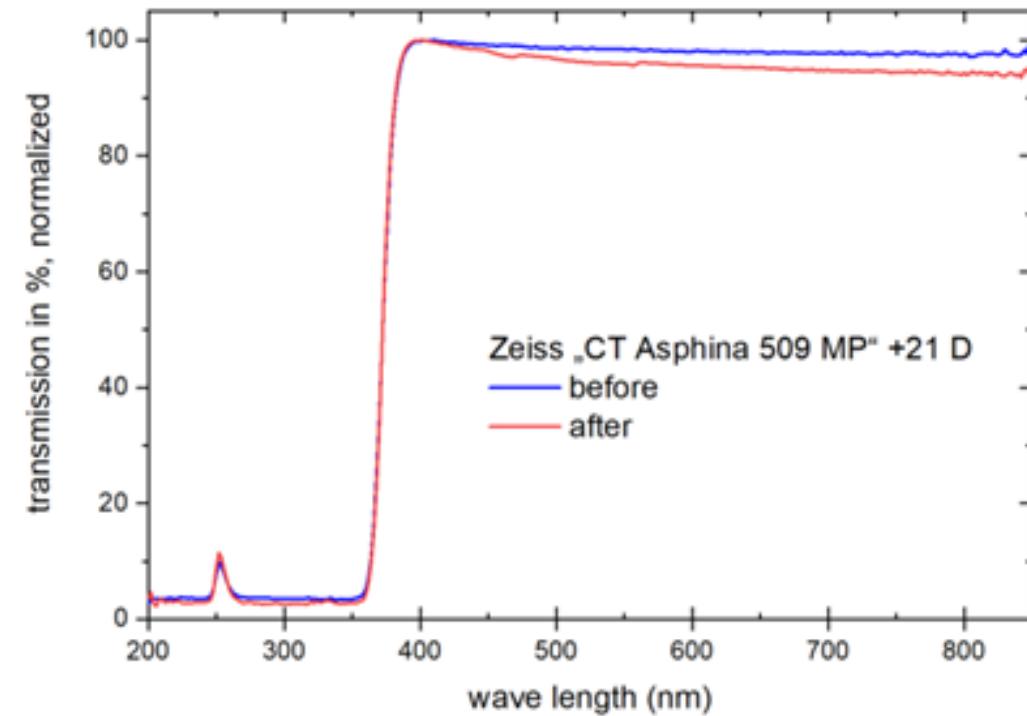
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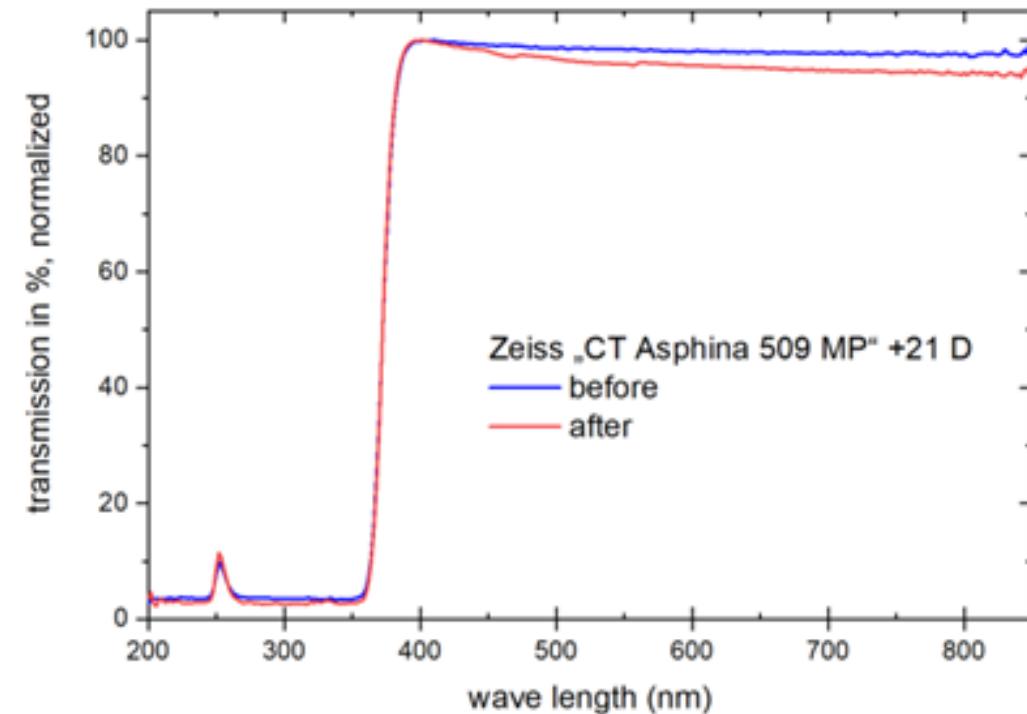
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- edges at the same wavelength



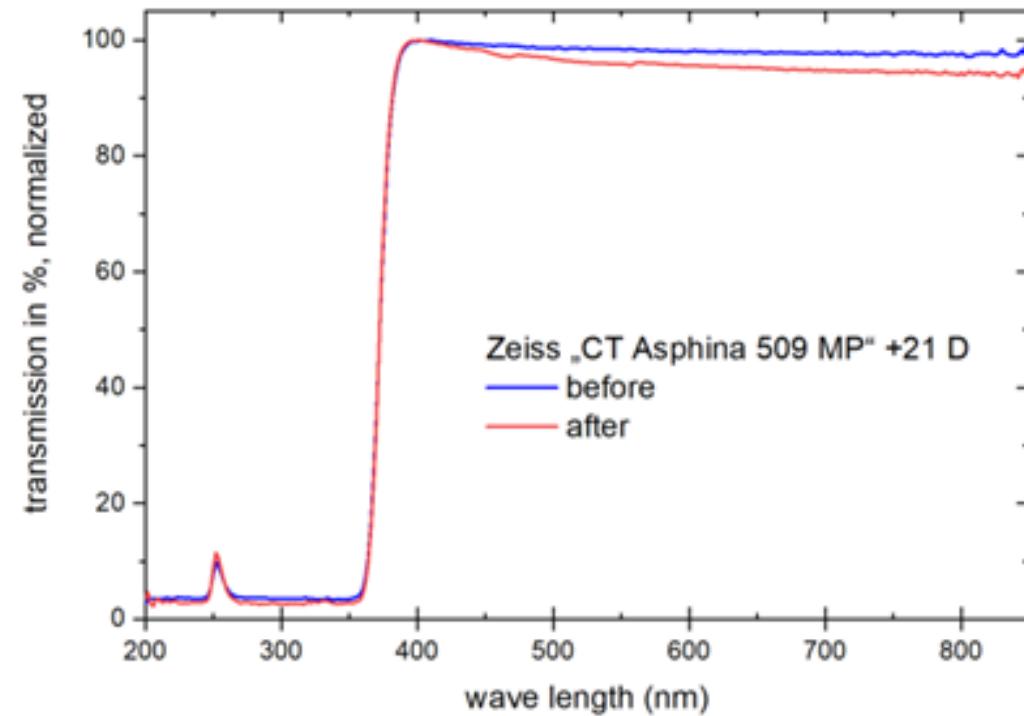
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- no significant changes in transmission before/after irradiation
- edges at the same wavelength  
→ dose rate is irrelevant
- only after irradiation with  $^{60}\text{Co}$ , 20000 Gy (typical sterilisation dose) changes in transmission observed



## Conclusion and Outlook

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- in spite of Covid-19: high patient numbers



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