

Superconducting rotating-gantry and other developments at HIMAC



Yoshiyuki Iwata

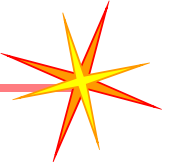
National Institute of Radiological Sciences (NIRS)



2013/10/4

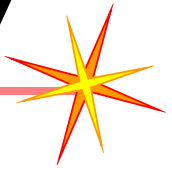


- **Introduction**
- **Recent developments**
 - Scanning irradiation
 - Multiple-flatop operation
 - Superconducting rotating-gantry
- **Summary**

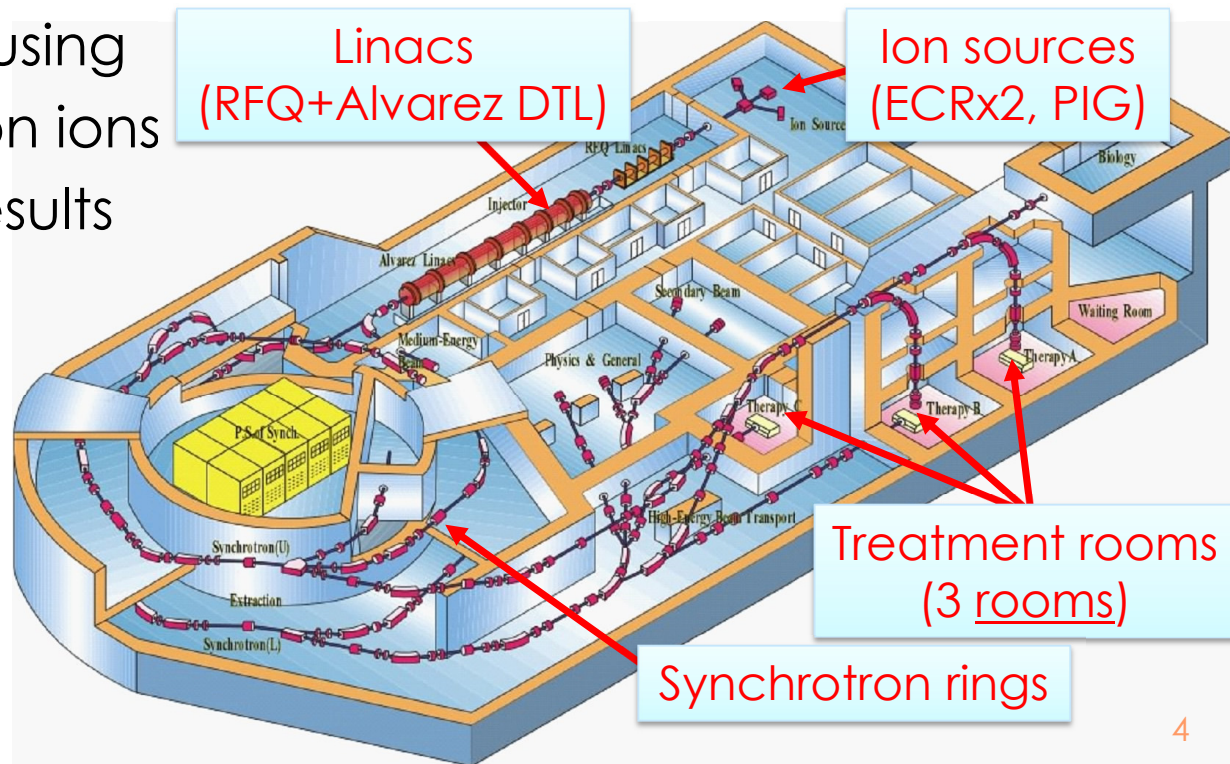


Introduction

Carbon radiotherapy



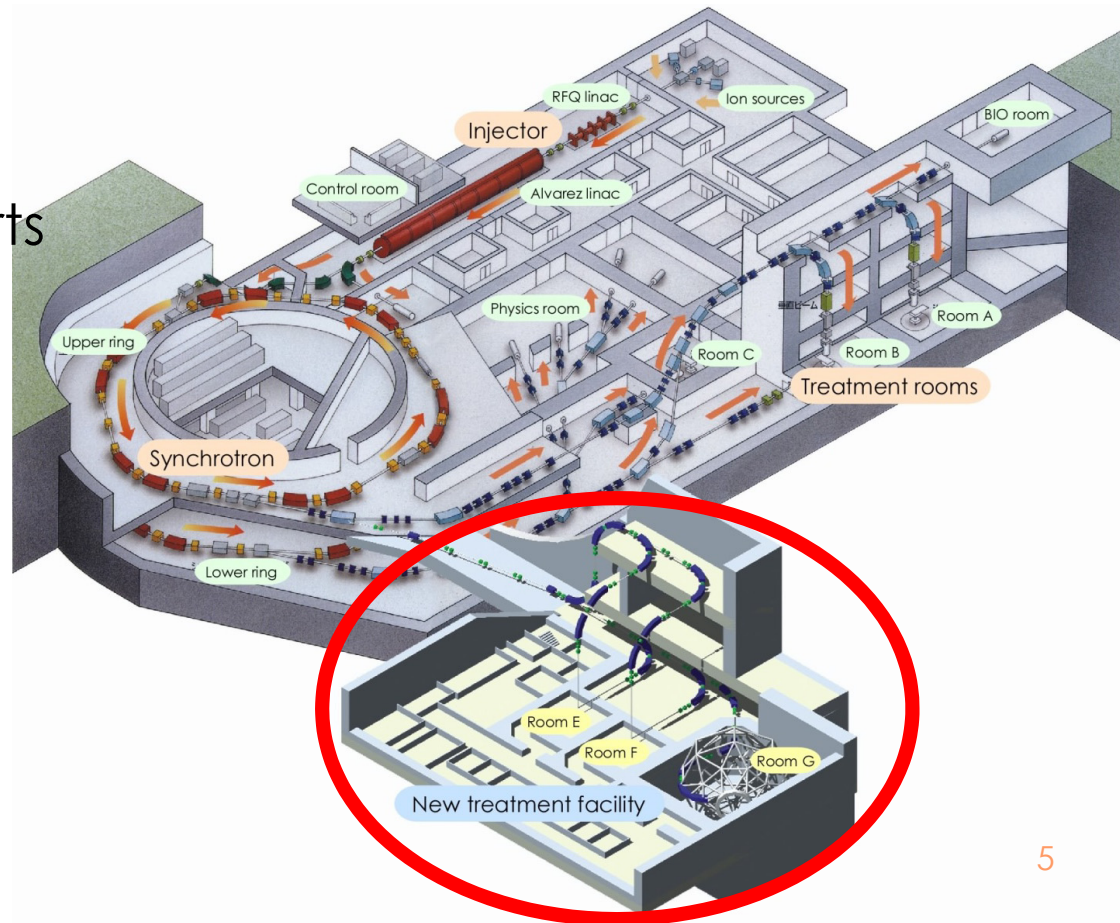
- Heavy Ion Medical Accelerator in Chiba (HIMAC)
- Ion species: p ~ Xe
- $E/A=800$ MeV for $q/m=1/2$
- Cancer treatments using energetic carbon ions
- Successful clinical results
 - ✓ **~7000 patients**



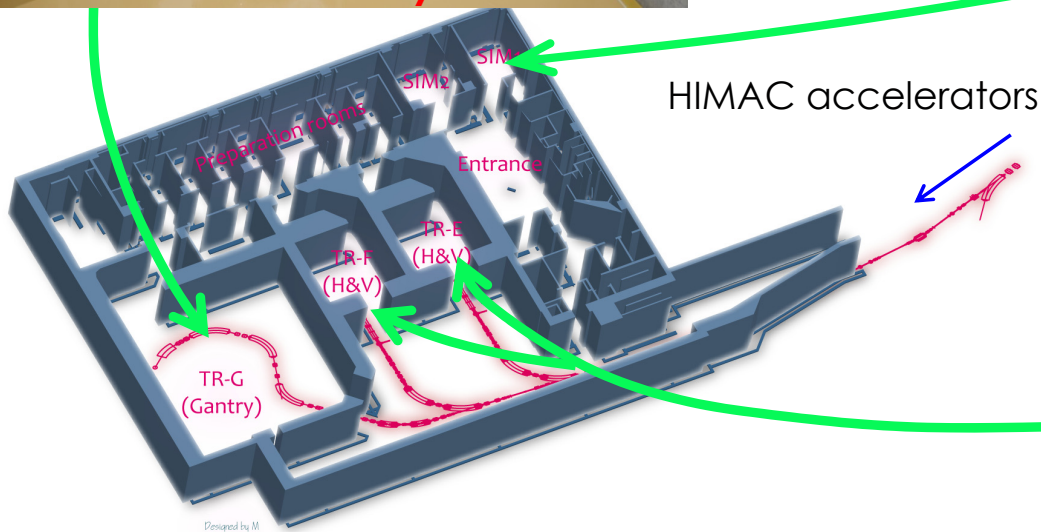
New treatment facility

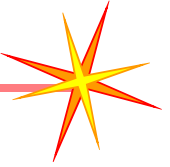


- Construction completed in FY2010
- 3 treatment rooms
 - Room E & F
Fixed H&C scanning ports
(in treatment operation)
 - **Room G**
Rotating gantry port
(Under construction)



Treatment floor (B2F)





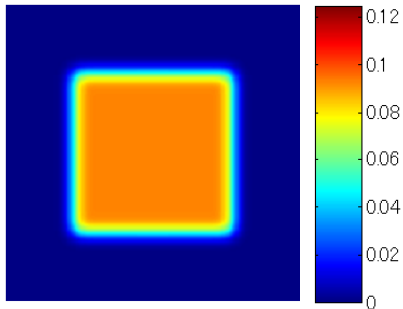
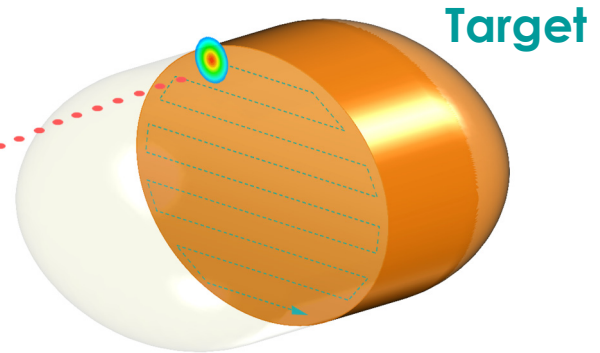
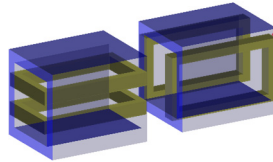
Recent developments #1 (Scanning irradiation)

3D raster-scanning irradiation



Development of 3D raster scanning-irradiation for moving targets

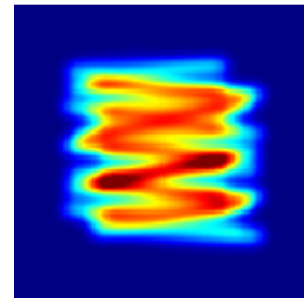
Scanning magnets



Dose distribution (designed)



For moving target....

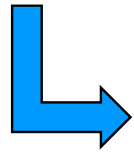


Interplay observed!

How can we fix it?



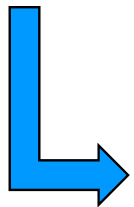
Respiration gating



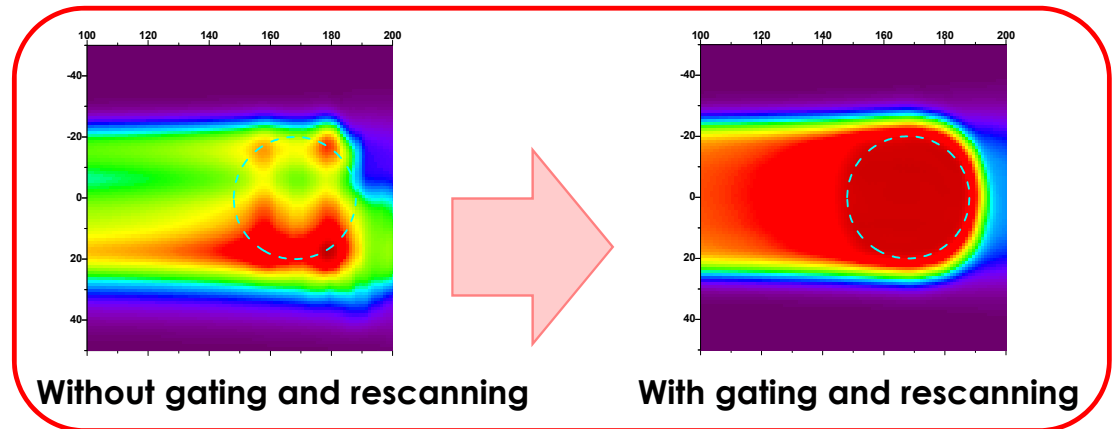
Suppress target movement within ~5mm

+

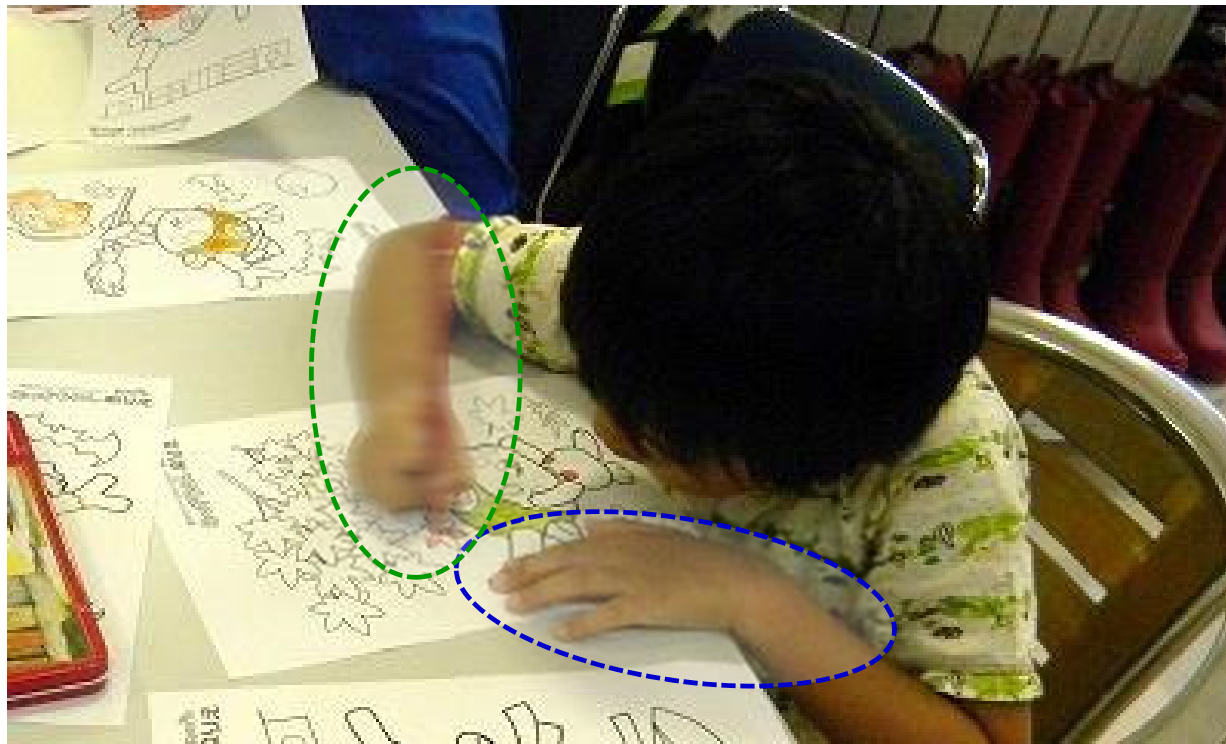
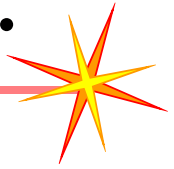
Rescanning



Fast rescanning
(scanning speed should be much faster
than target movement)

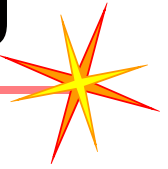


This is like...

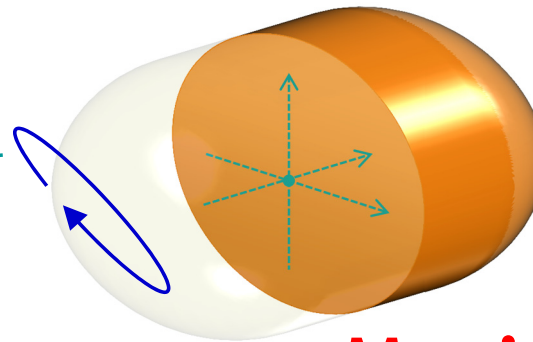
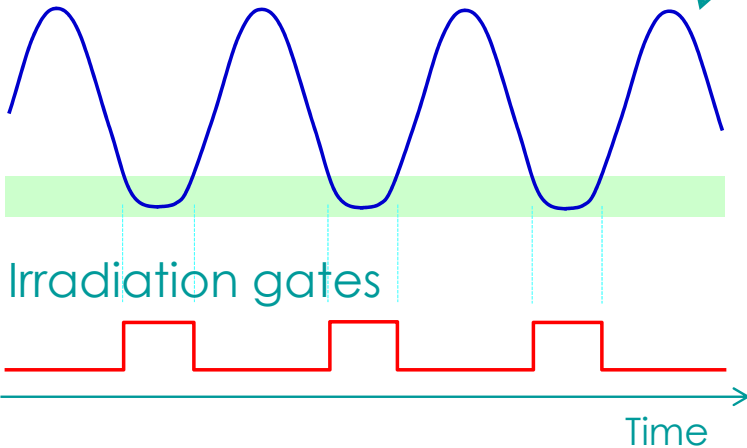


“Respiration gating” × “Fast rescanning”

Respiration gating



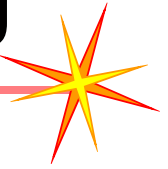
Respiration monitor



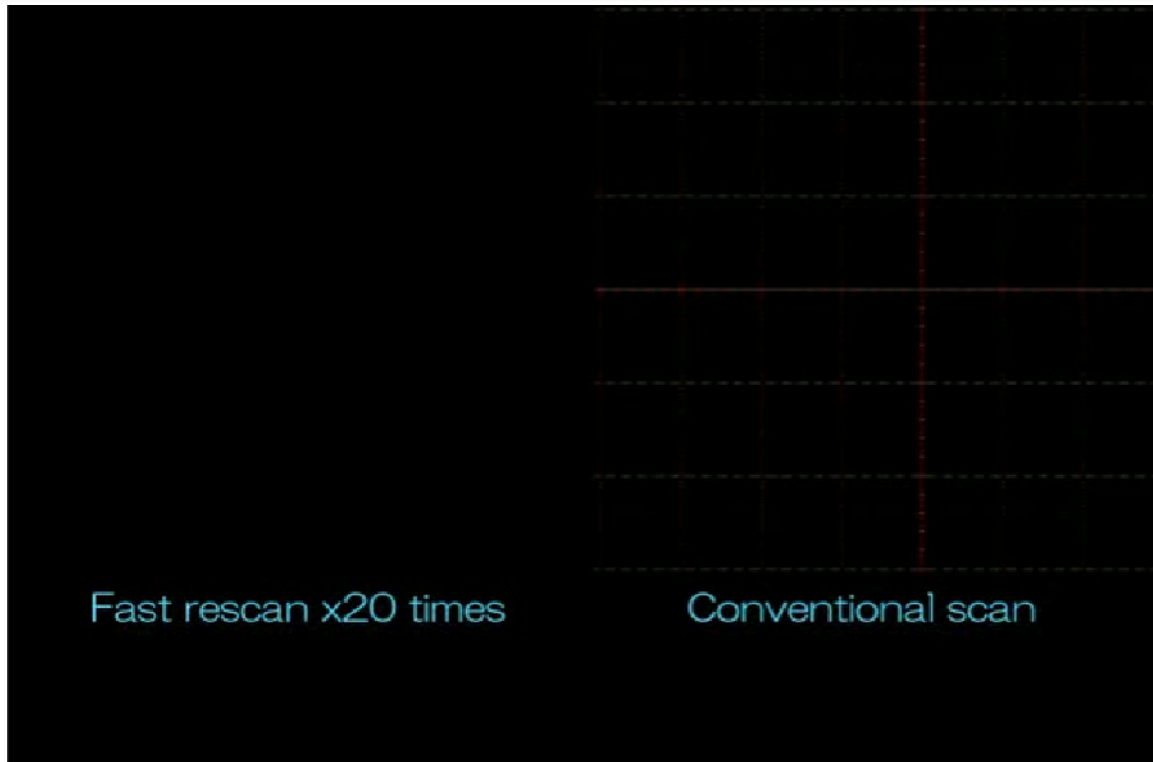
Moving target

By monitoring patient's respiration, errors in dose distribution can be reduced!

Fast rescanning

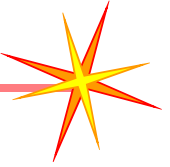


Comparison between **fast rescan** and **conventional scanning**



Fast rescan x20 times

Conventional scan

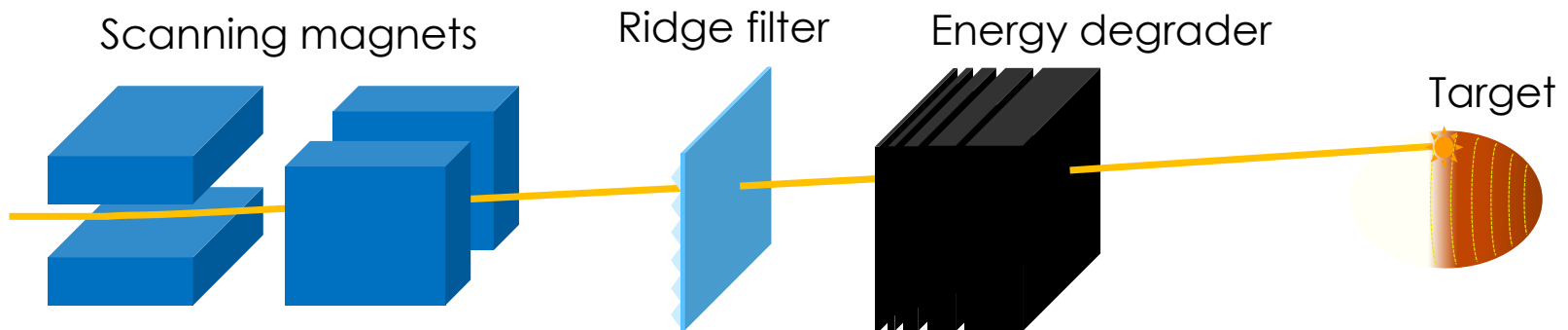
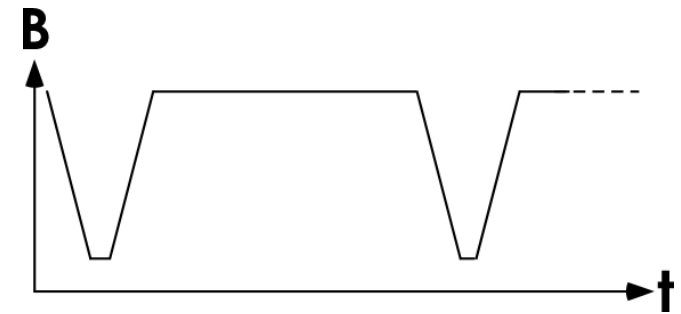


Recent developments #2 (Multiple-flattop operation)

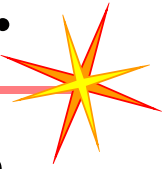
Depth-dose distribution



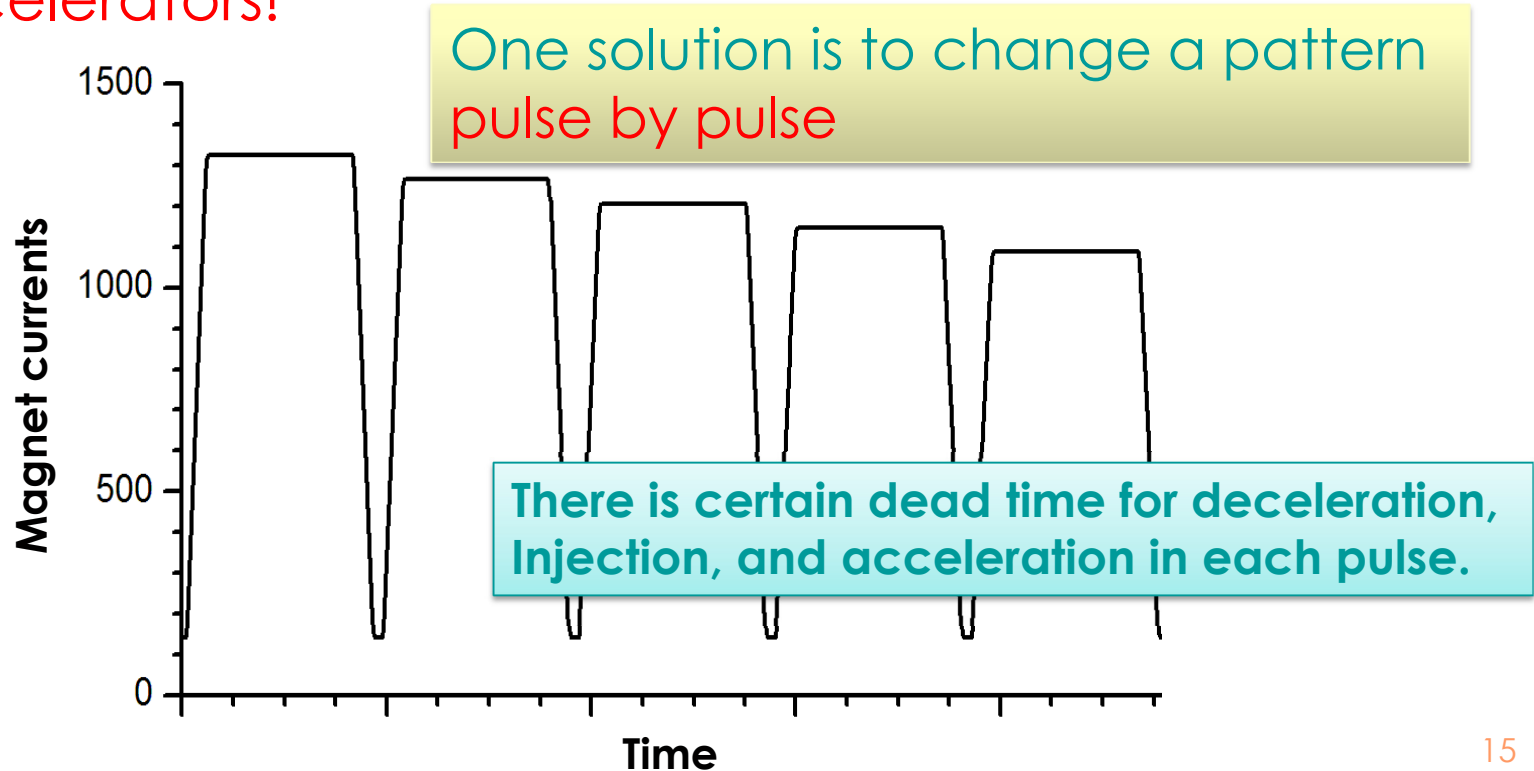
- **Conventional synchrotron operation**
 - Fixed operation cycle
 - Single energy
- **Energy degrader has to be used**
 - Enlarge a size of beam spots
 - Produce fragments



For scanning irradiation....



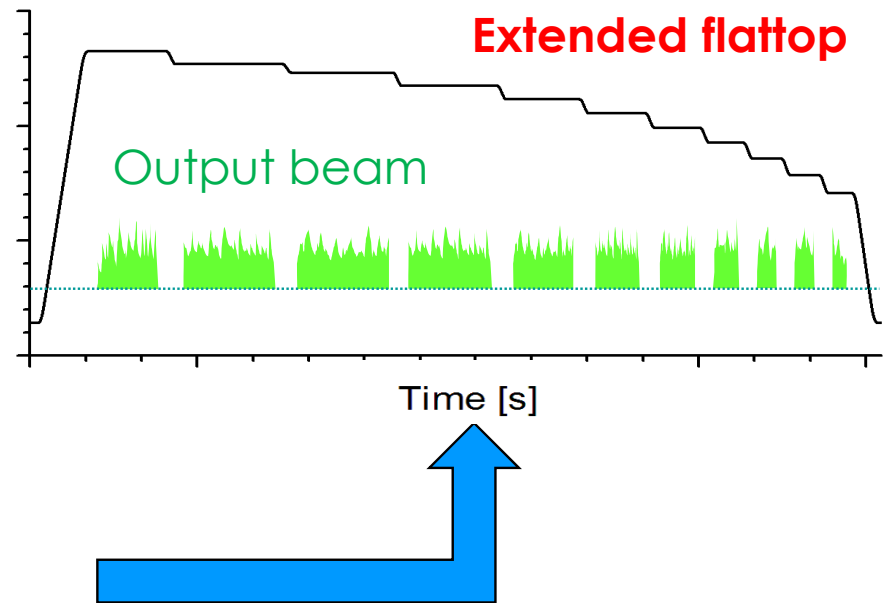
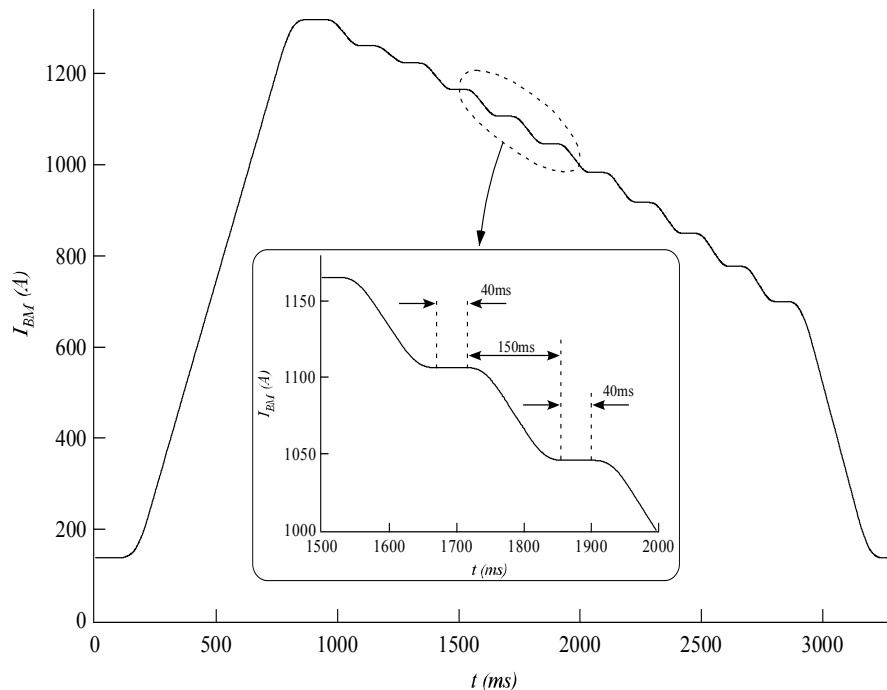
- To take full advantage of the scanning irradiation,
 - beam energy has to be changed directly from accelerators!



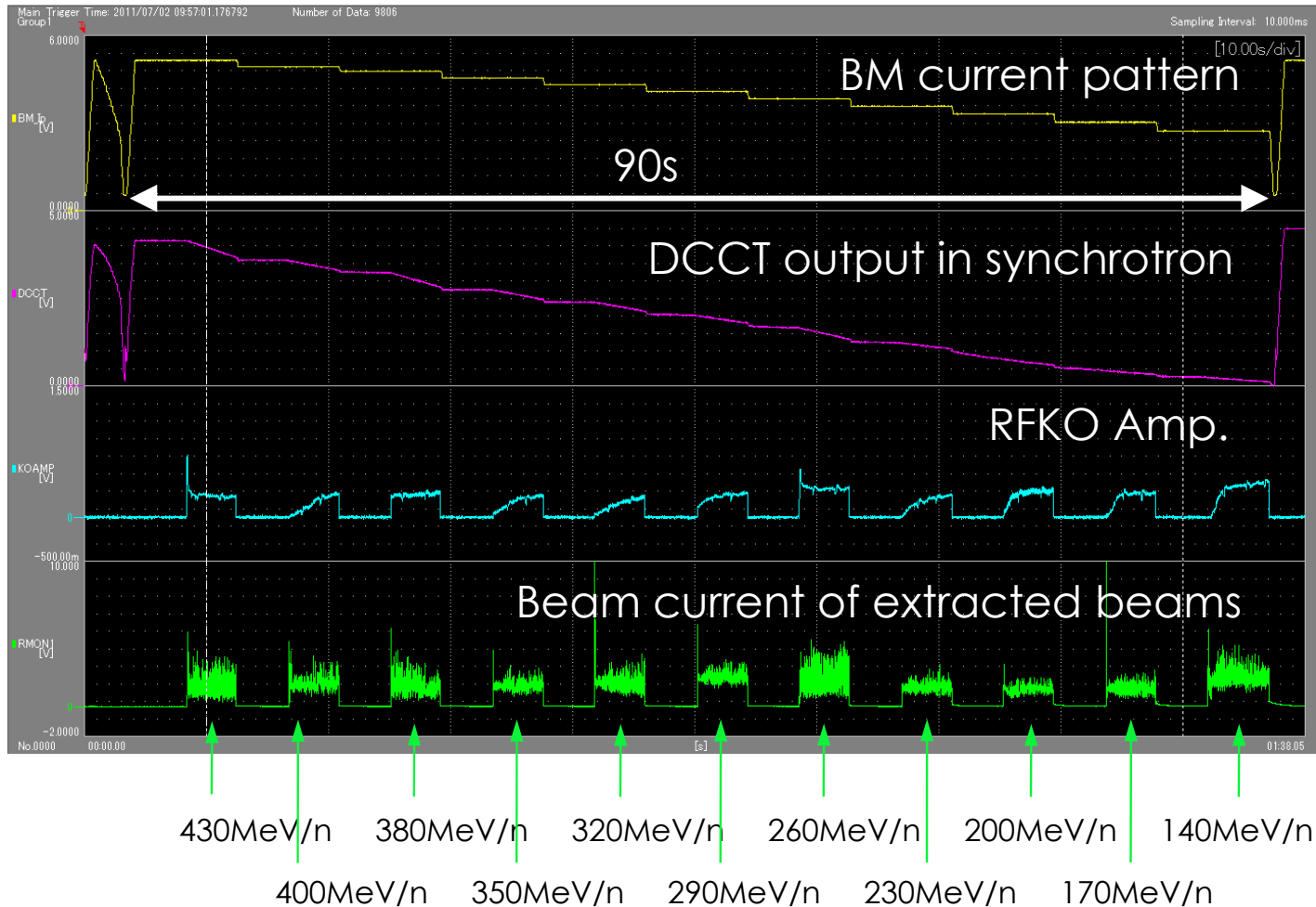
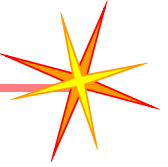
Multiple-flattop operation



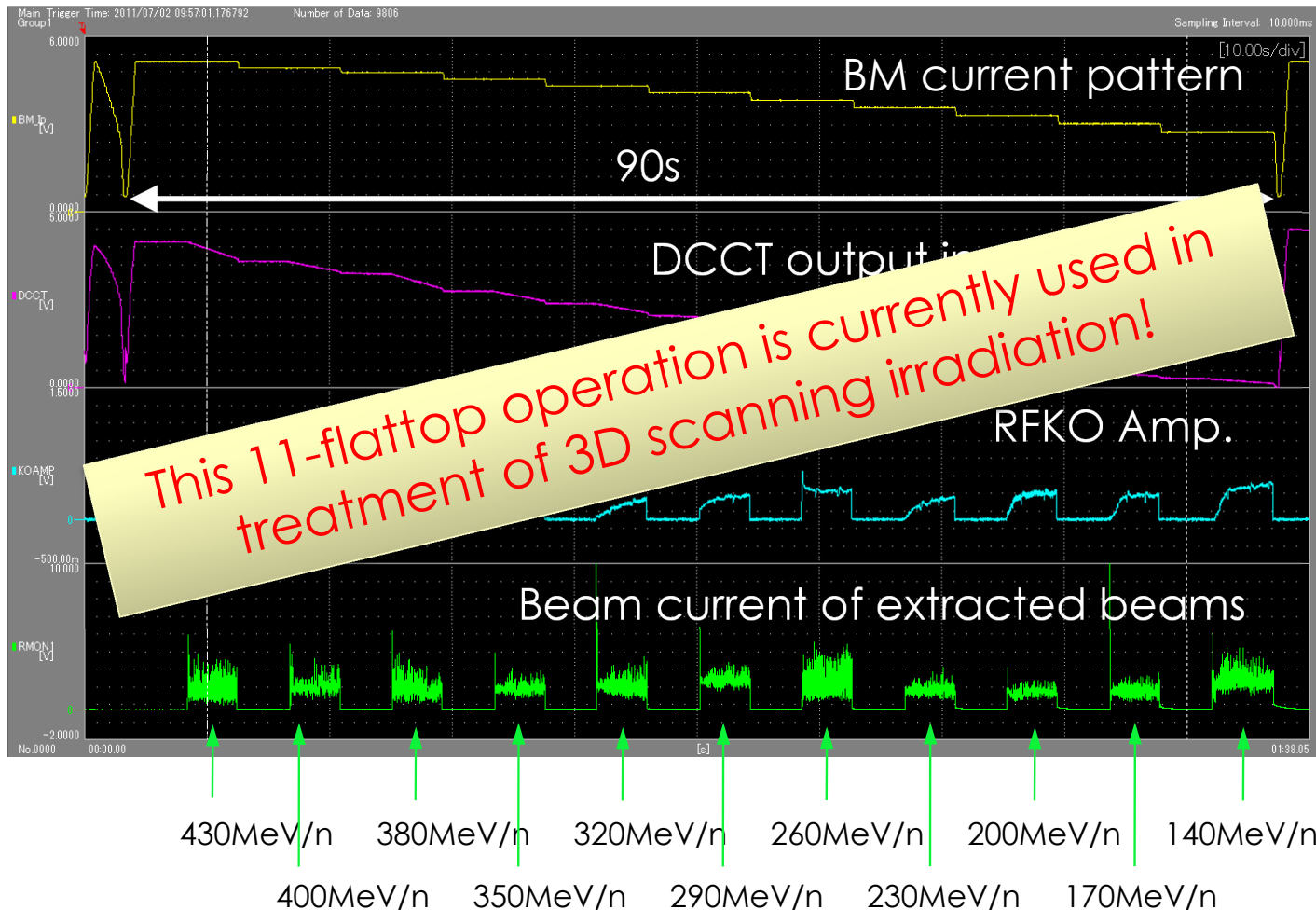
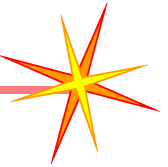
- Operation pattern having multiple flattops
- Each flattop can be extended
- **Beams having various energies can be extracted!**



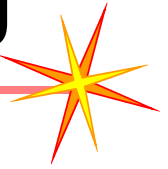
Operation with 11-flattop pattern



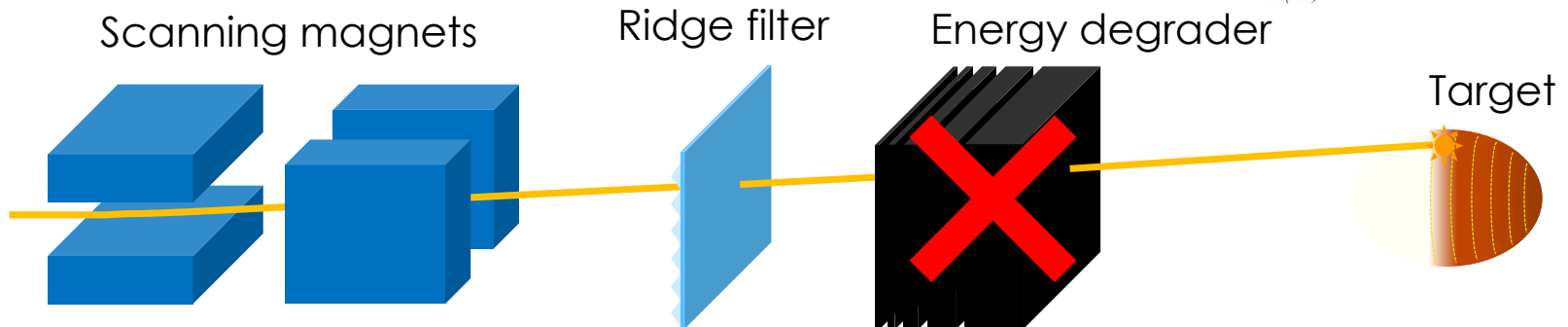
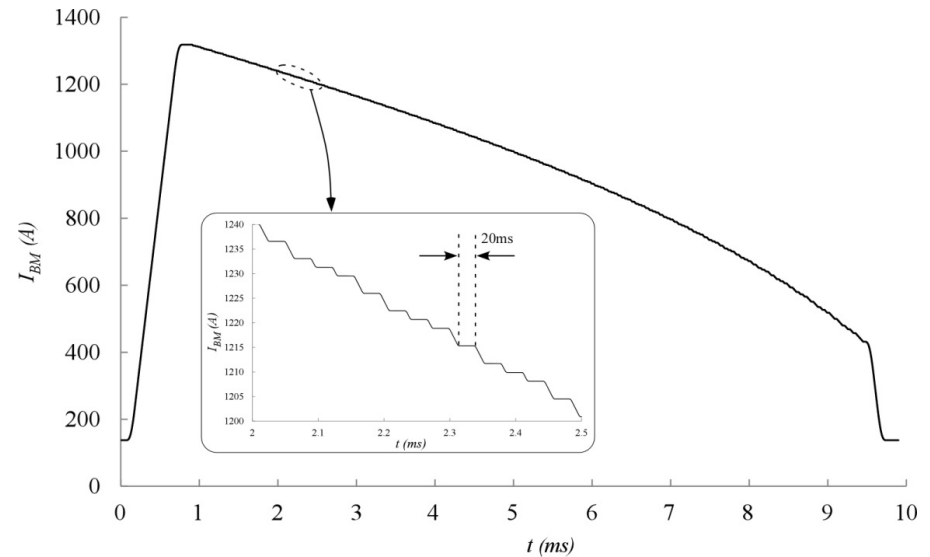
Operation with 11-flattop pattern



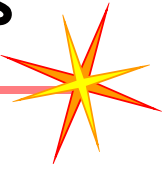
Full energy scanning



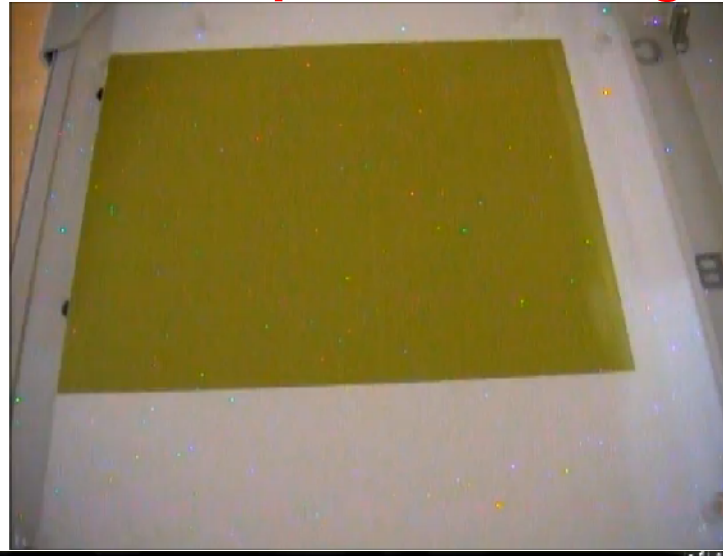
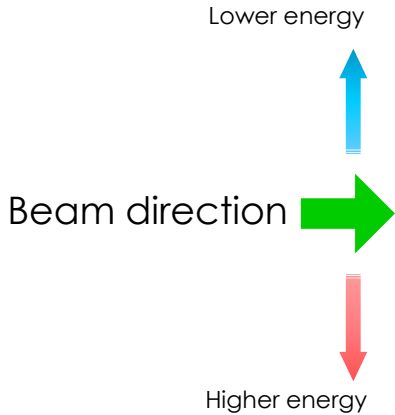
- Beam energy is varied by 1 or 2 mm step in water range
- $E=430 - 56 \text{ MeV/u}$
- 201-flattop pattern
- No energy degrader



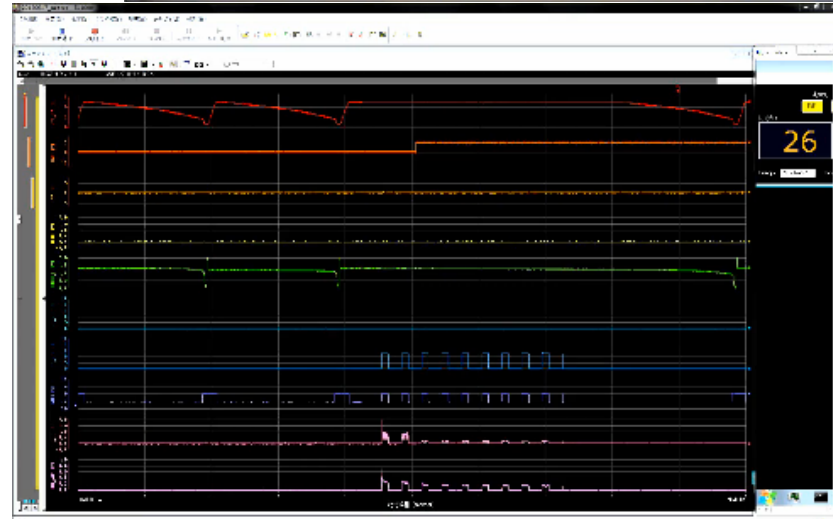
Beam acceleration and extraction tests



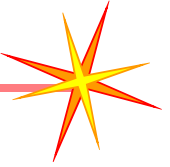
3mm step in water range



- Current pattern of BM ■
- Scanning magnet (X) ■
- Scanning magnet (Y) ■
- Extracted beam ■
- Beam current in ring ■
- Irradiation gate ■

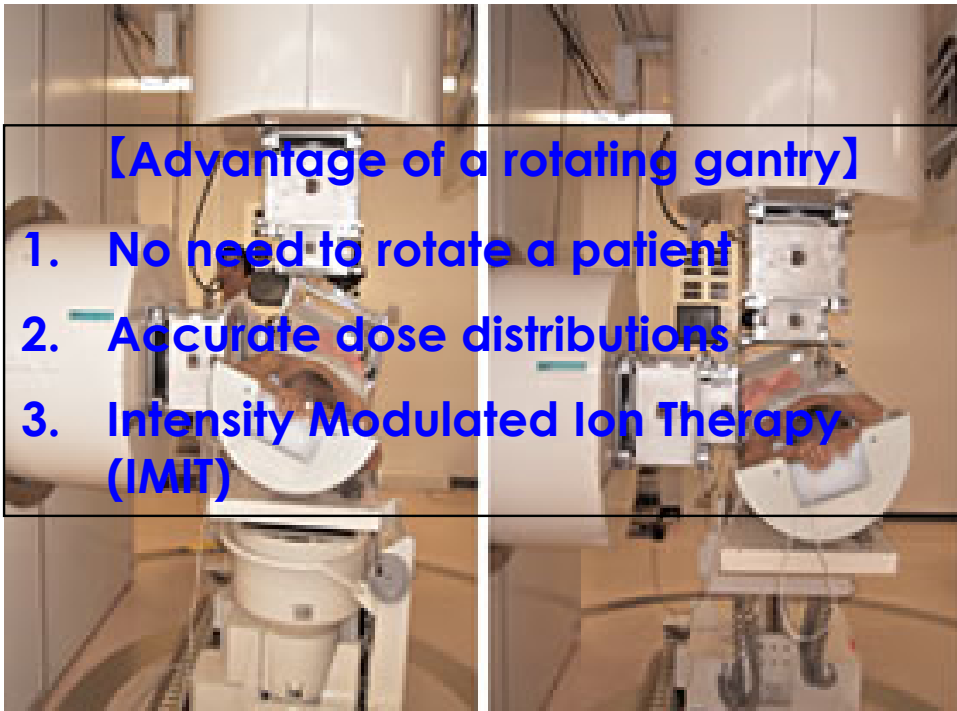


Energy ID



Recent developments #3 (SC rotating-gantry)

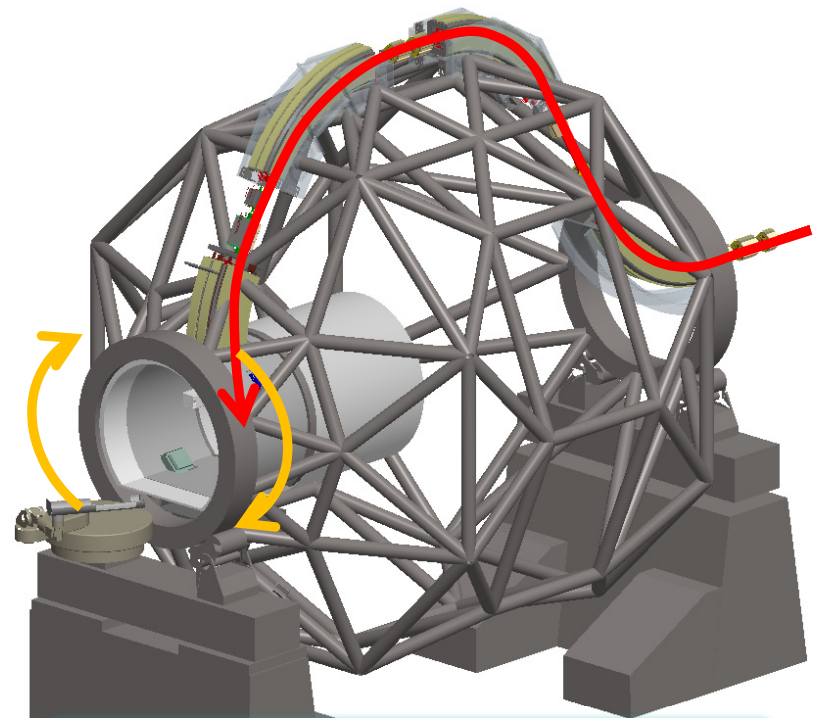
Needs for a rotating gantry



[Advantage of a rotating gantry]

1. No need to rotate a patient
2. Accurate dose distributions
3. Intensity Modulated Ion Therapy (IMIT)

Irradiation with the existing fixed port



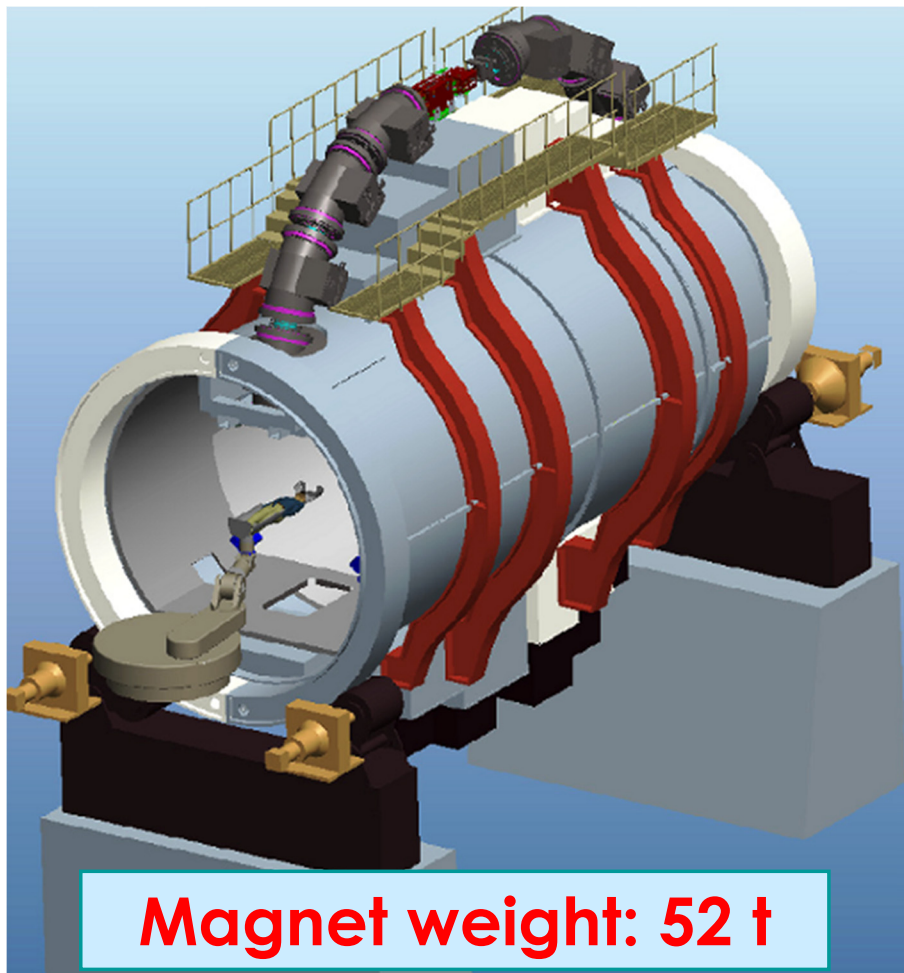
Beam can be directed to a target from **any of medically desirable angles**

Rotating gantry for carbon therapy

- **Only one gantry in the world**
 - Heidelberg Ion Beam Therapy Center (HIT)
- Size and weight
 - Radius: 6.5m
 - Length: 25m
 - Weight: 670t
(Rotating part: 600t)



Superconducting rotating-gantry



Use of superconducting (SC) magnets

Ion kind	: ^{12}C
Irradiation method	: 3D Scanning
Beam energy	: 430 MeV/n
Maximum range	: 30 cm in water
Scan size	: $\square 200 \times 200 \text{ mm}^2$
Radius	: 5.45 m
Length	: 13 m

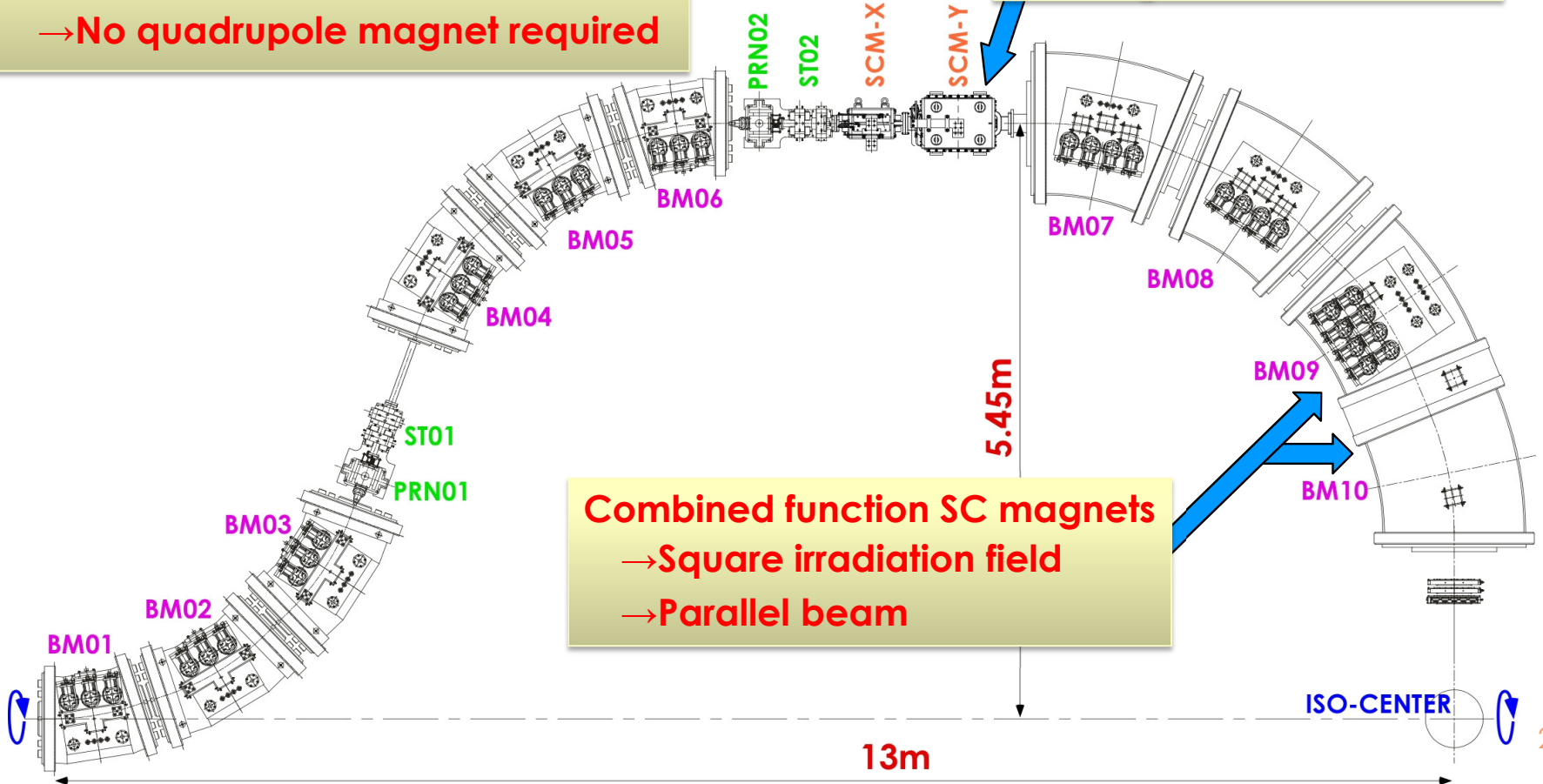
The size and weight are comparable to those of proton gantries!

Magnet weight: 52 t

Layout of the SC gantry

Combined function SC magnets
(BM01~BM06)
→ No quadrupole magnet required

Scanning magnets on top
→ Large scan size

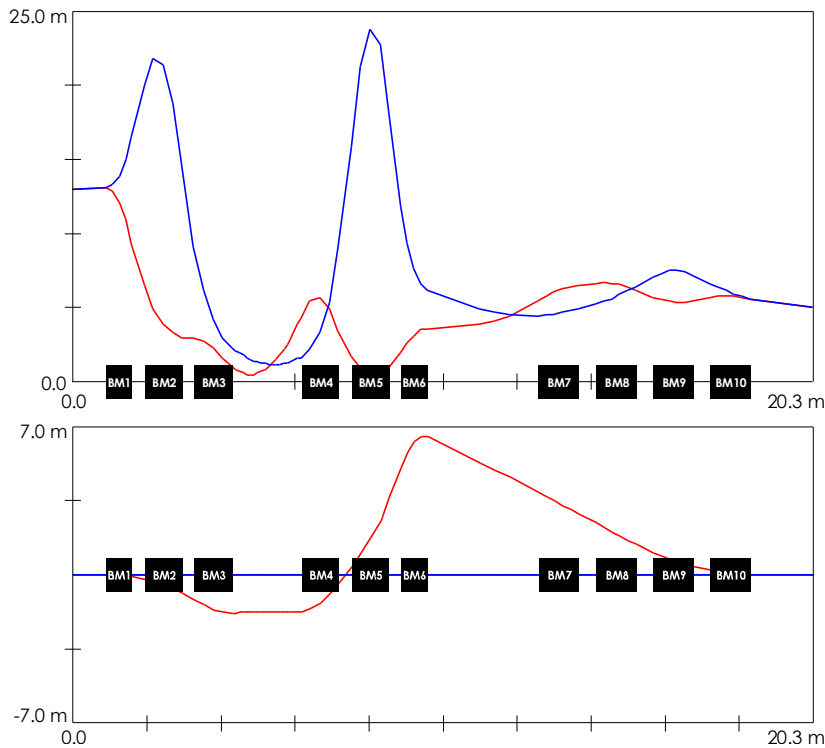


Combined function SC magnets
→ Square irradiation field
→ Parallel beam

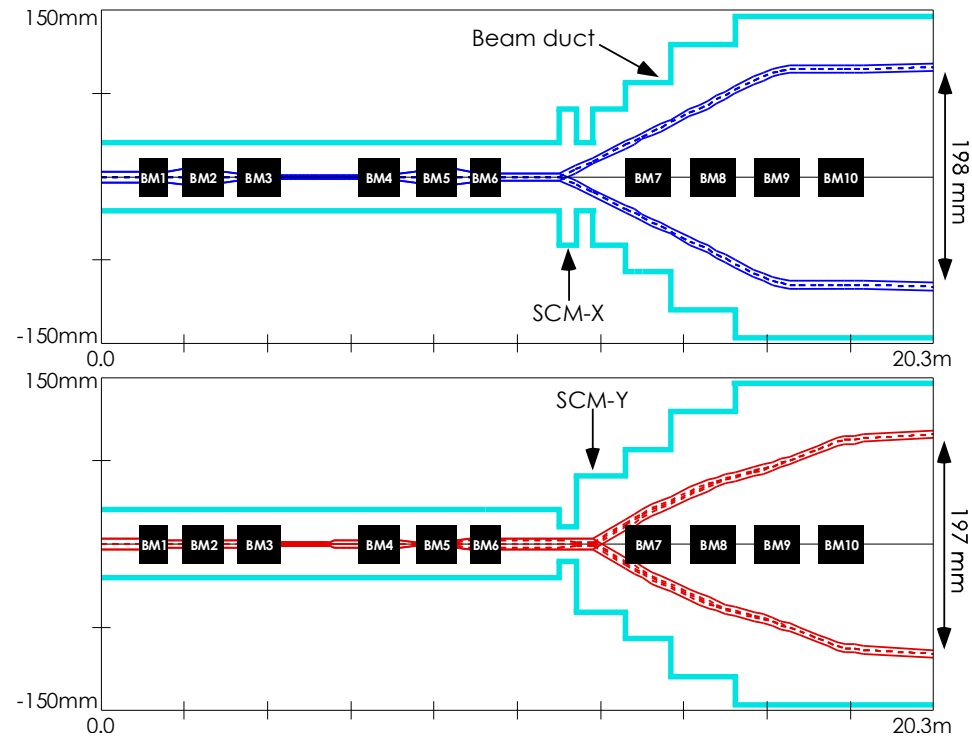
Beam optics design



Beta and dispersion functions



Beam envelope functions with kicks of scanning magnets

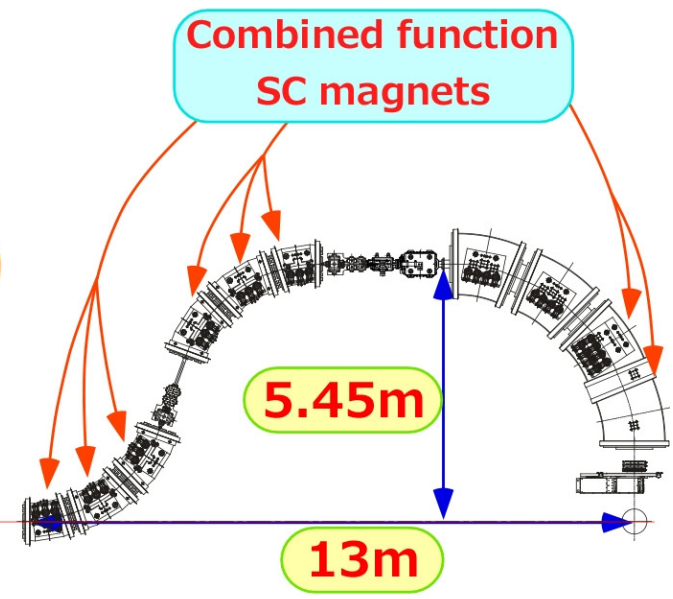
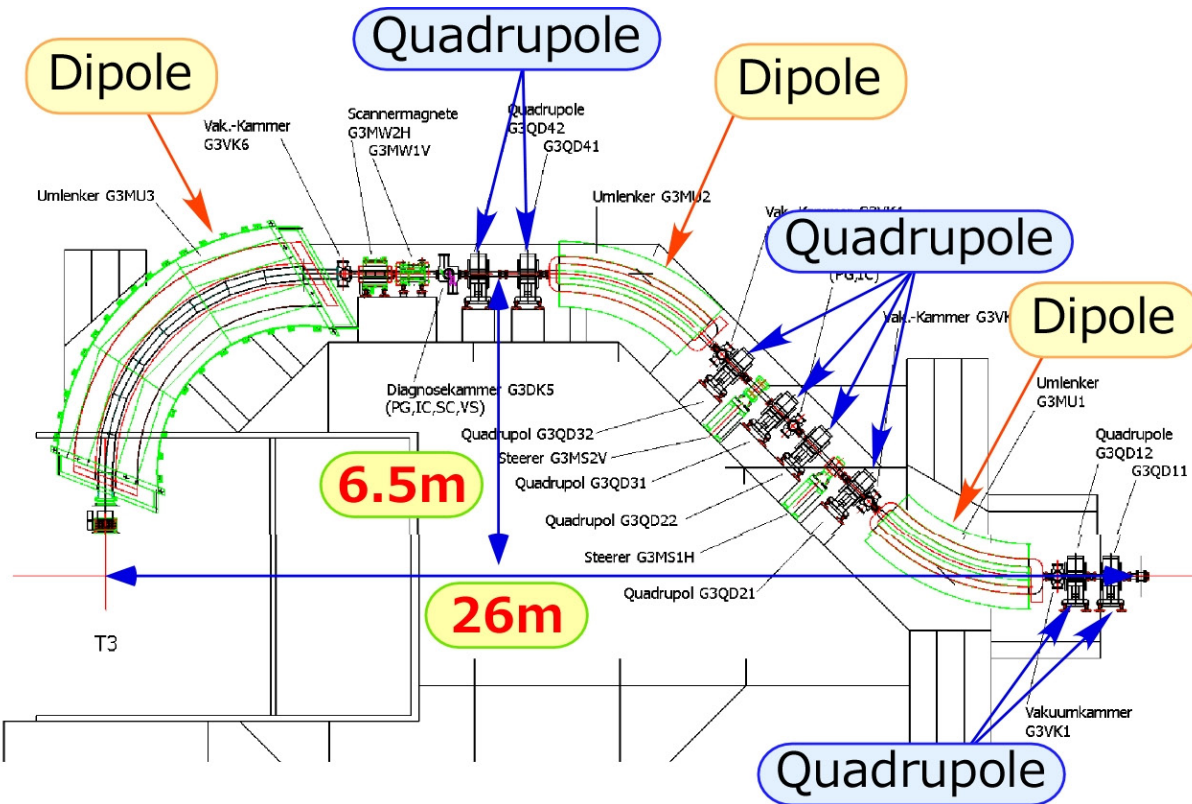


Comparison in size



HIT gantry

NIRS SC-gantry



Length and weight are reduced by ~1/2

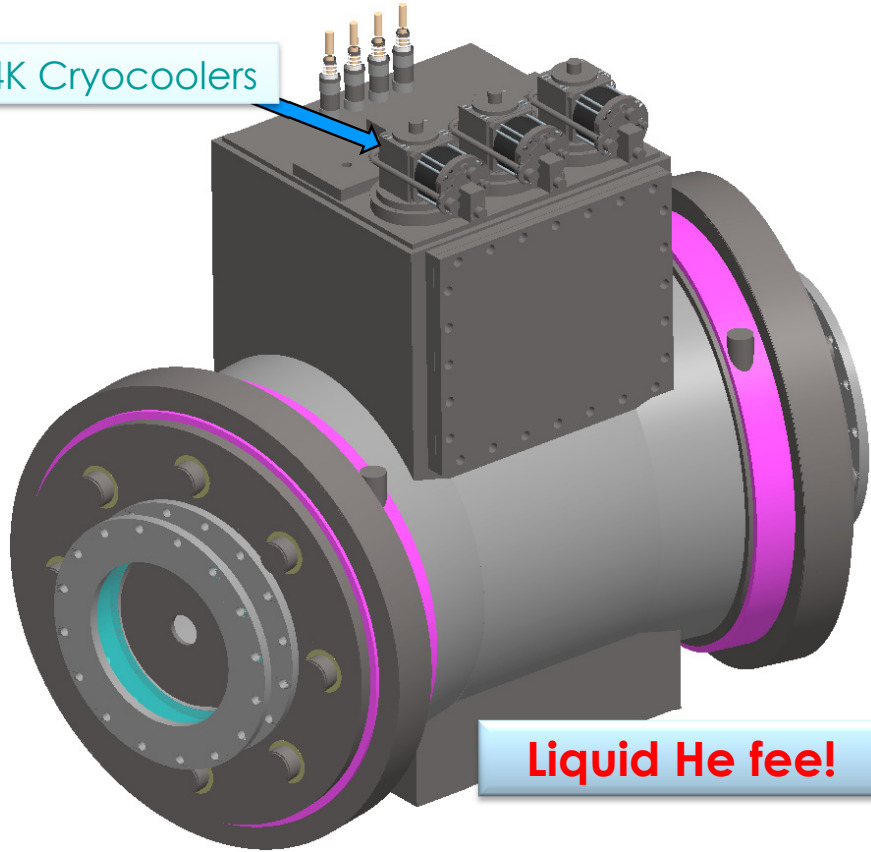
Development of curved SC magnets



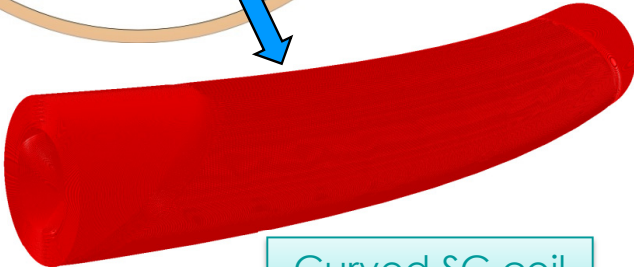
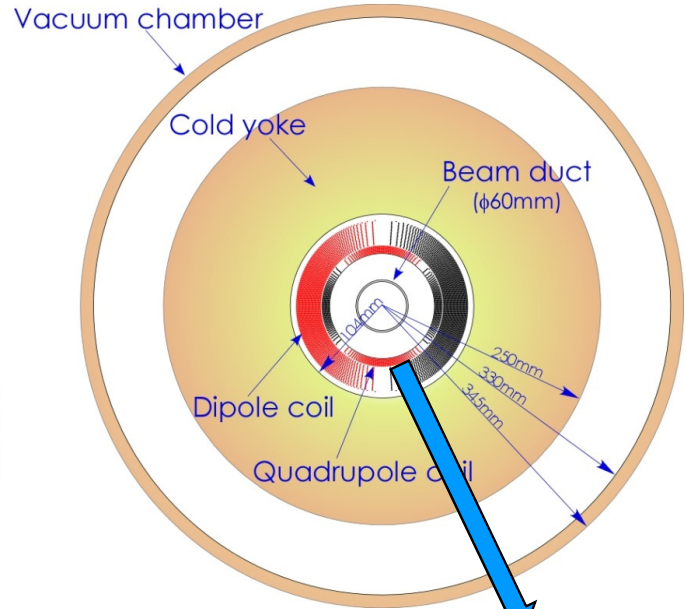
SC magnet (BM02-05)

Cross-sectional view

4K Cryocoolers



Liquid He fee!

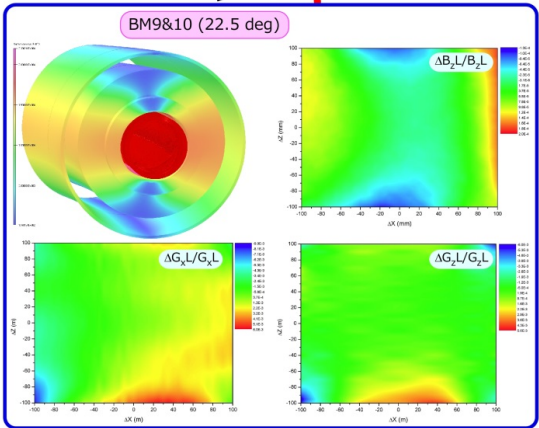
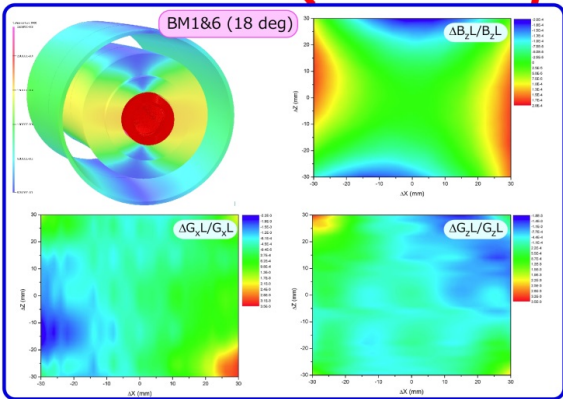
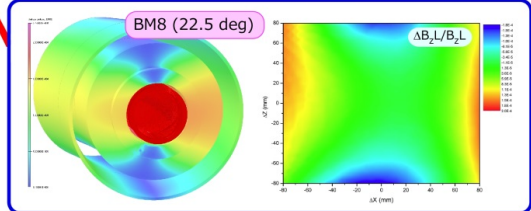
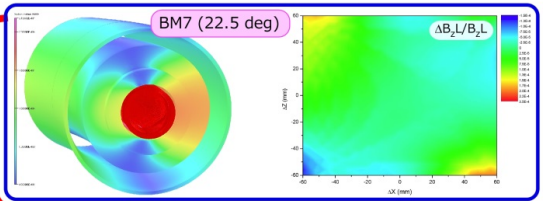
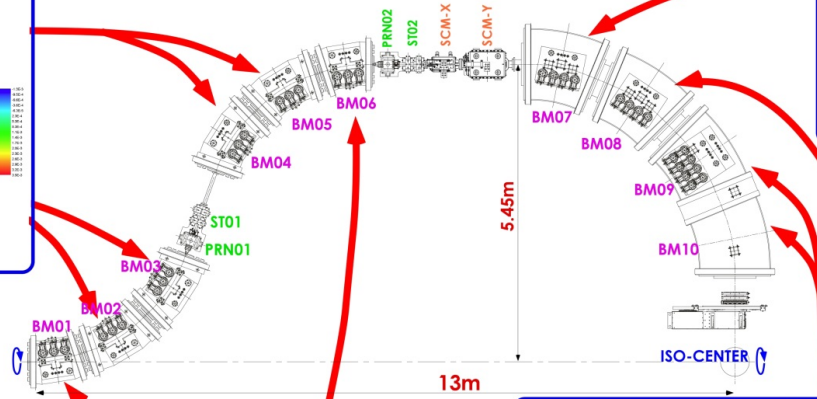
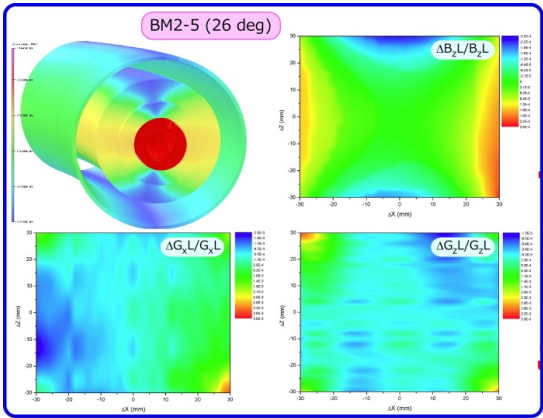


Curved SC coil

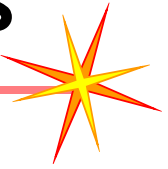
Design of SC magnets



All the SC magnets were designed by using a 3D magnetic field solver



Beam tracking simulations

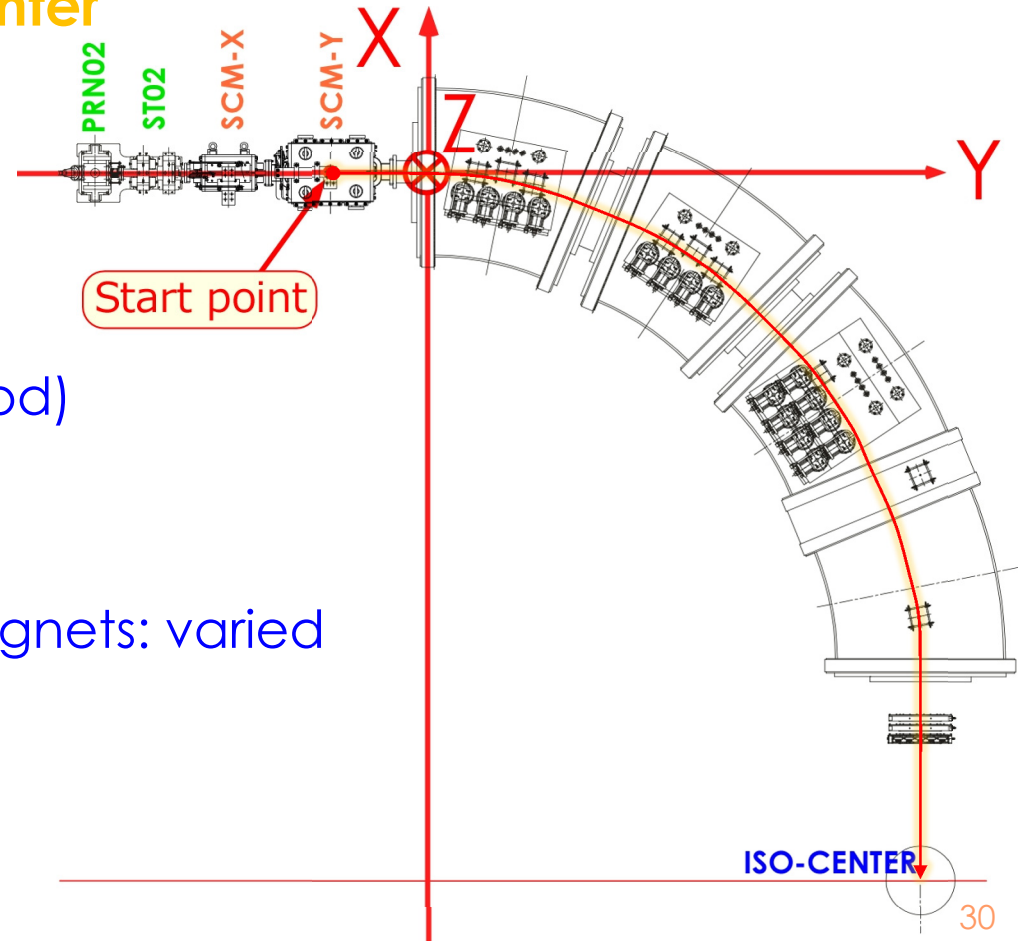


- **Beam tracking to the isocenter**

- Field map data
(from Opera-3d code)
- Numerical integration of
equation of motion
(4th order Runge-Kutta method)

- **Beam profile at isocenter**

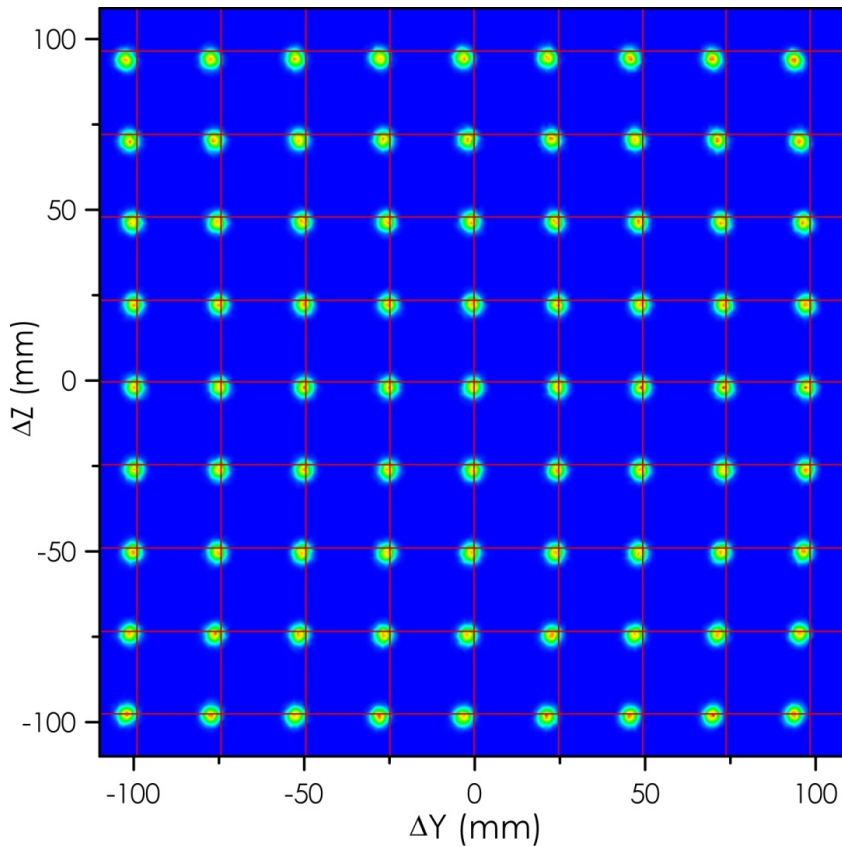
- Kick angle of scanning magnets: varied
- 81 spots at isocenter



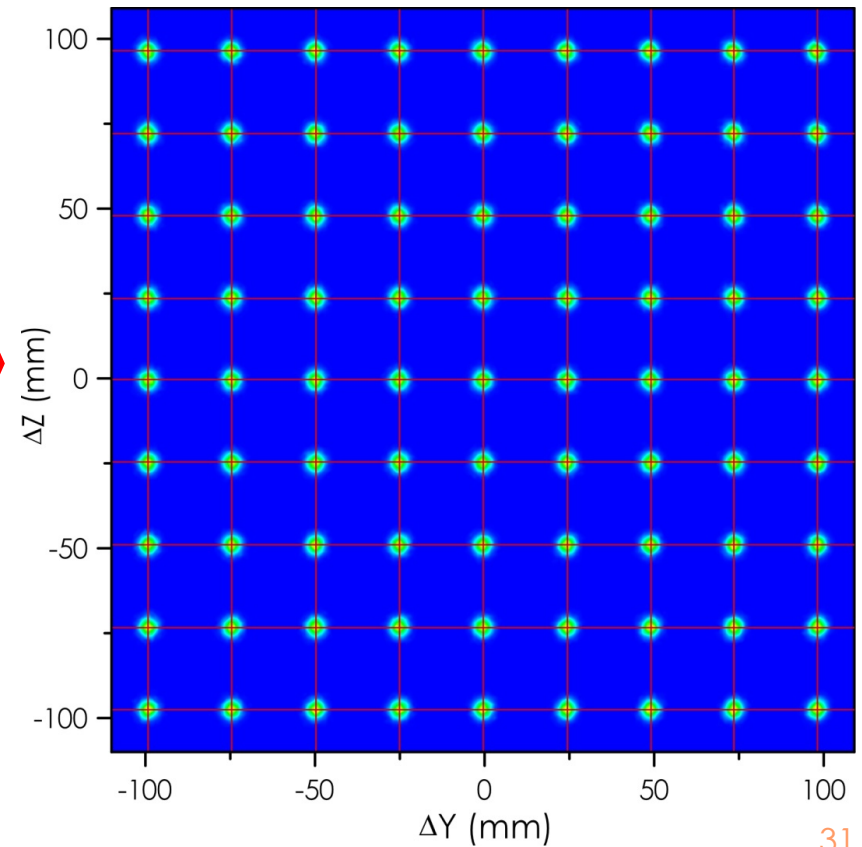
Beam tracking simulations



Phase space distribution of three beam spots



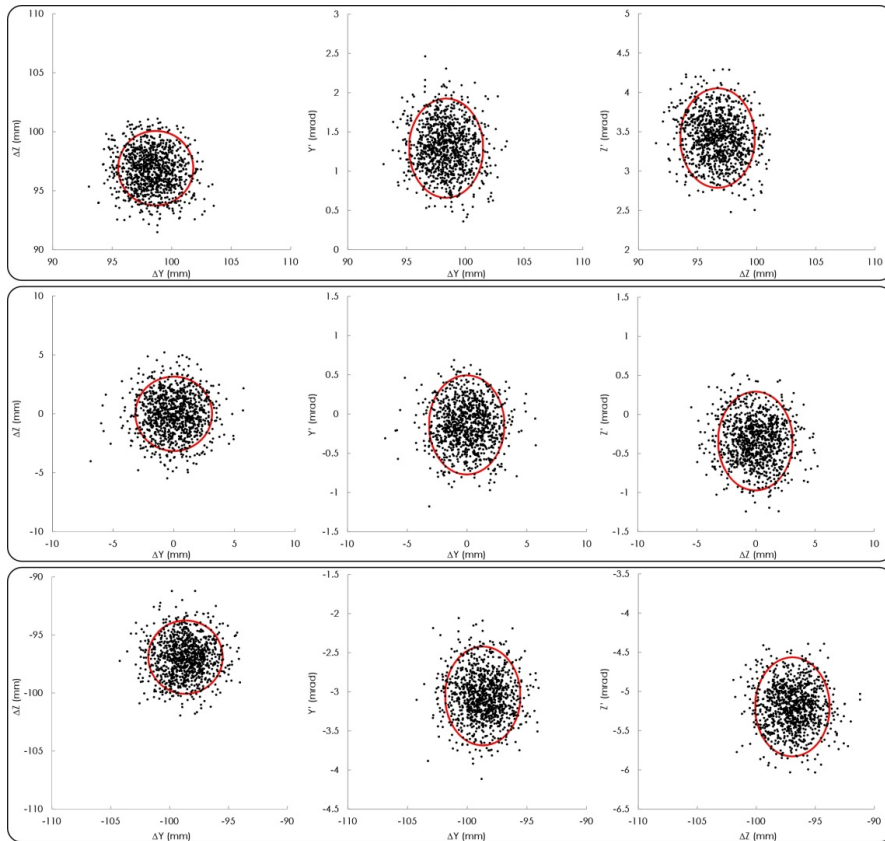
Beam profile after correction with the scanning magnets



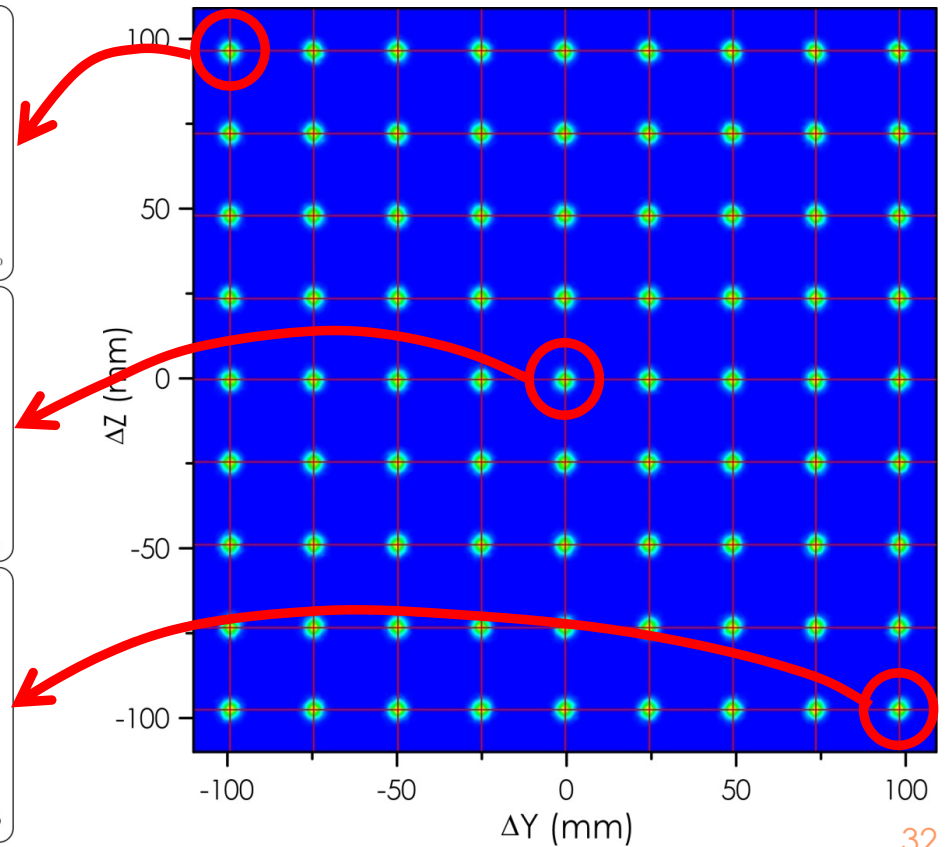
Beam tracking simulations

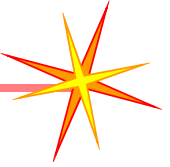


Phase space distribution of three beam spots



Beam profile after correction with the scanning magnets





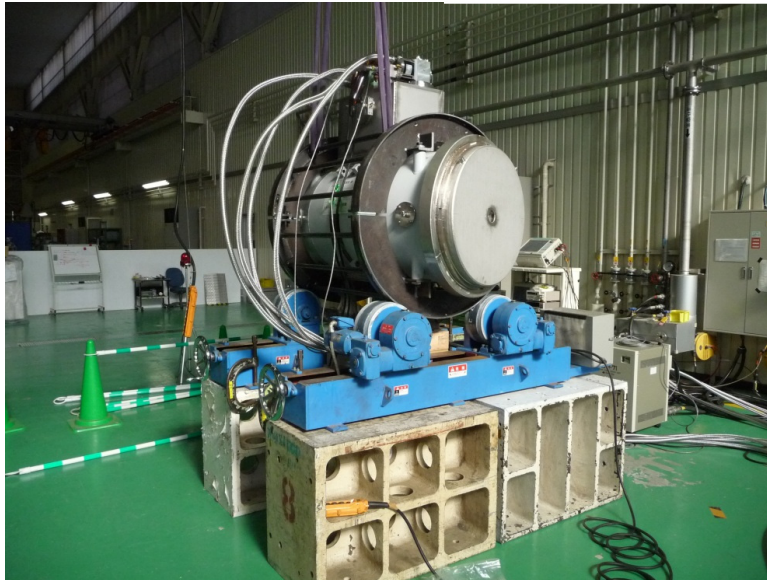
Construction and tests of SC magnets

Rotation tests



- Model SC magnet (Toshiba corp.)
- Rotation over ± 180 degrees
- Applying maximum coil-current

No quench observed!

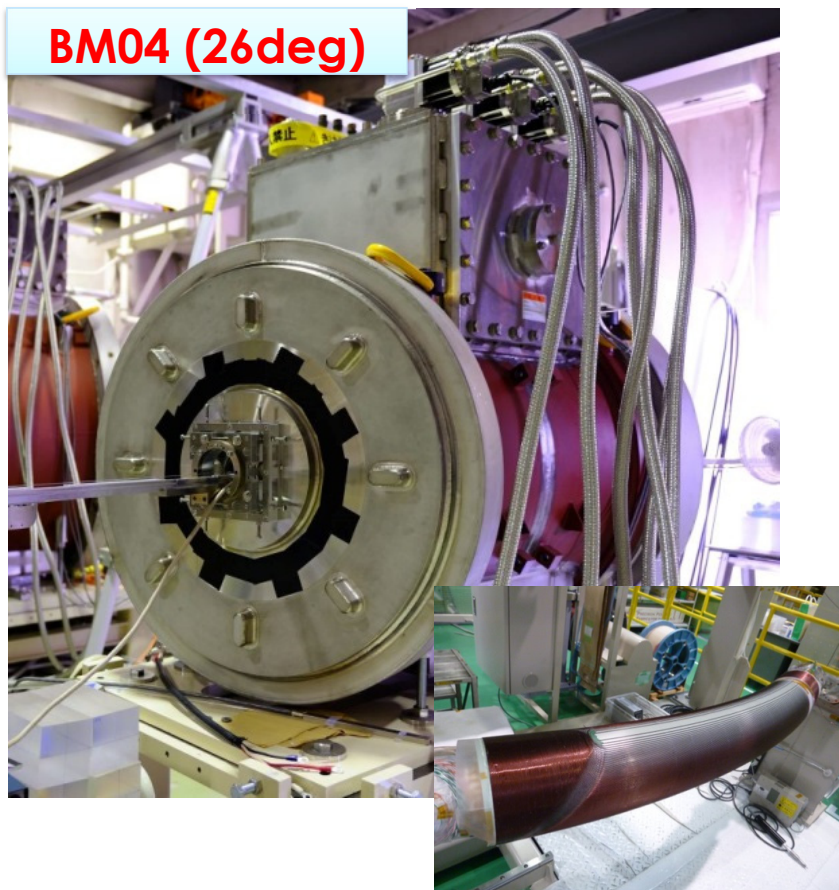


Construction of SC magnets

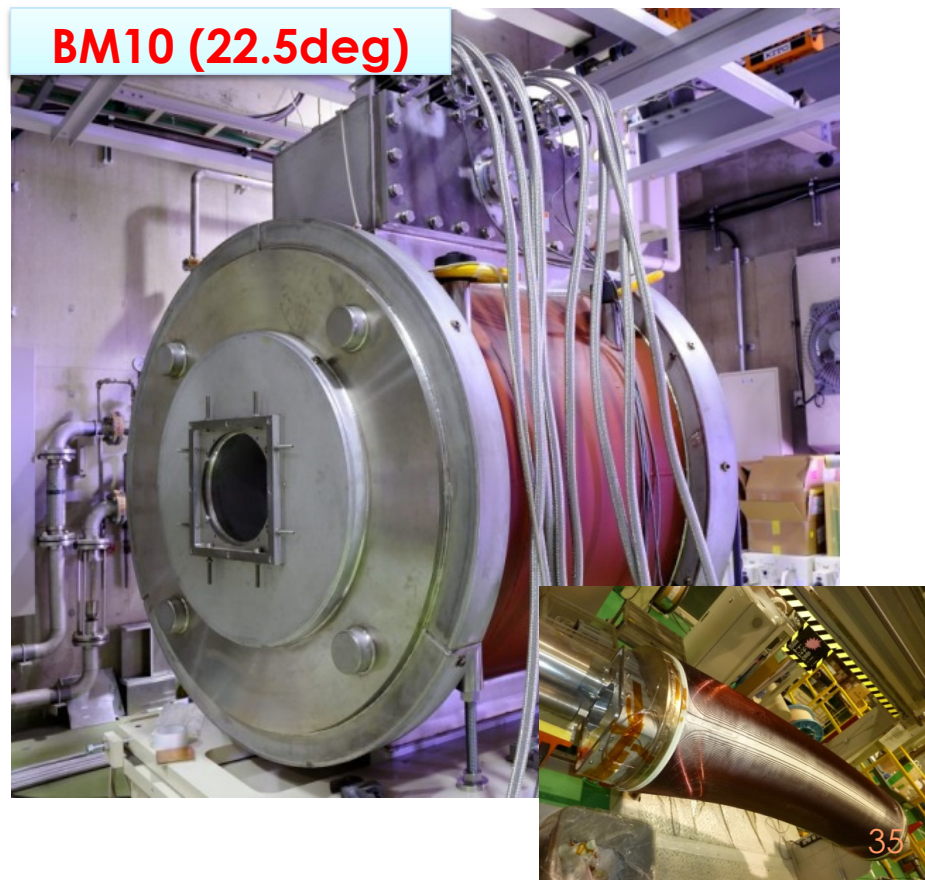


We have constructed 5 out of 10 SC magnets

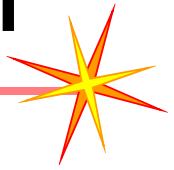
BM04 (26deg)



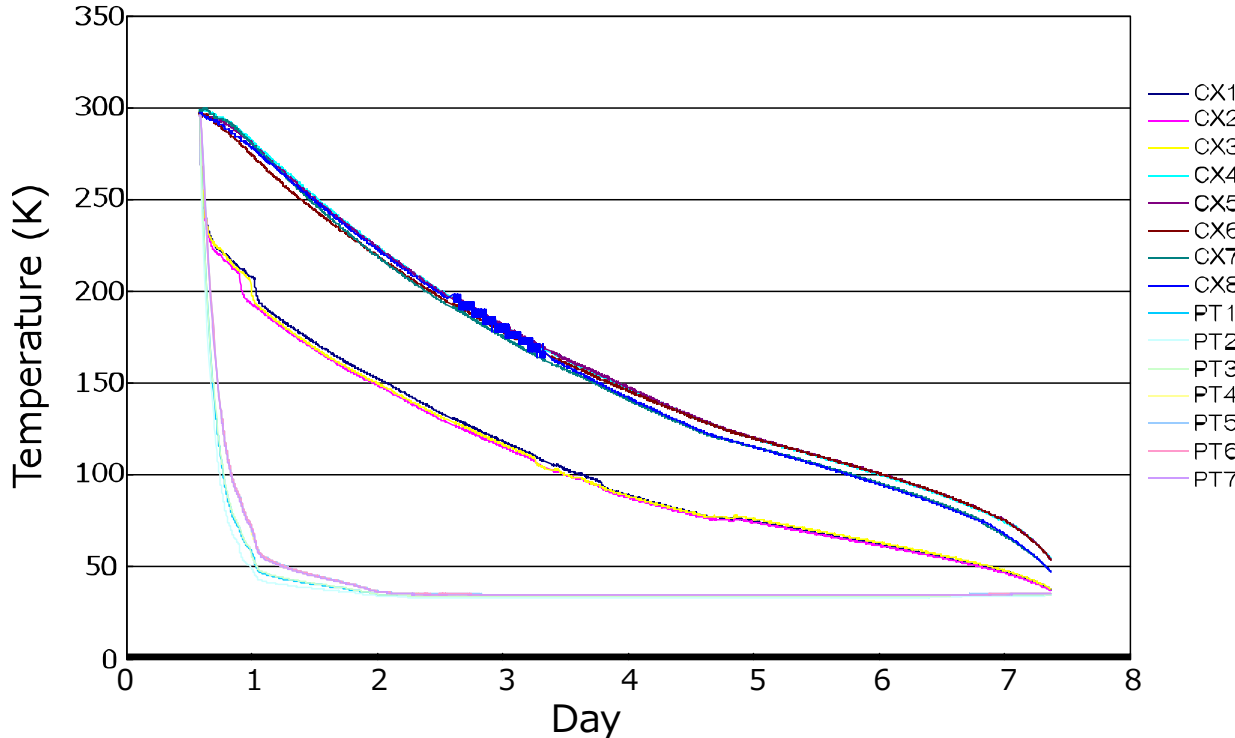
BM10 (22.5deg)



Initial cooling of SC magnet



- Precool with liquid nitrogen
- It took a week to cool down by 4K

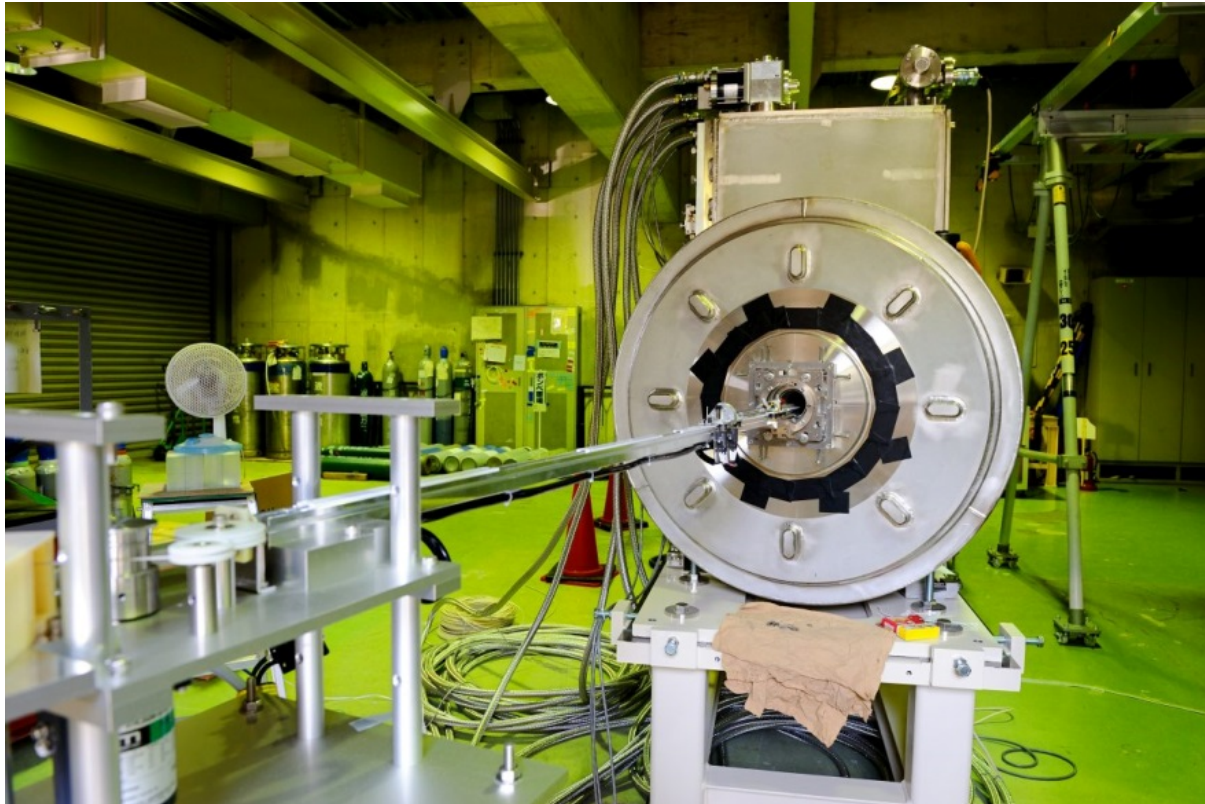


CX1: Cryocooler#1 2nd stage
 CX2: Cryocooler#2 2nd stage
 CX3: Cryocooler#3 2nd stage
 CX4: SC coil (inner)
 CX5: SC coil (middle)
 CX6: SC coil (outer)
 CX7: Yoke (right face)
 CX8: Yoke (left face)
 PT1: Cryocooler#1 1st stage
 PT2: Cryocooler#2 1st stage
 PT3: Cryocooler#3 1st stage
 PT4: HTCPL Dipole (P)
 PT5: HTCPL Dipole(N)
 PT6: HTCPL Quadrupole (P)
 PT7: HTCPL Quadrupole (N)

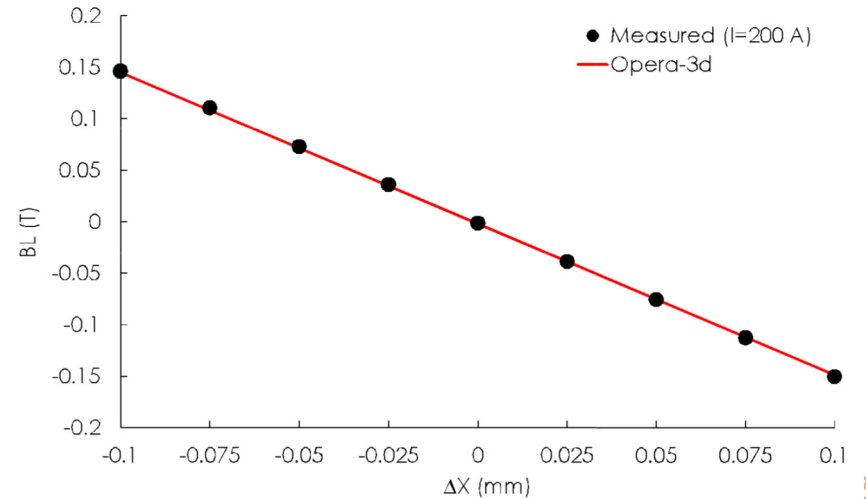
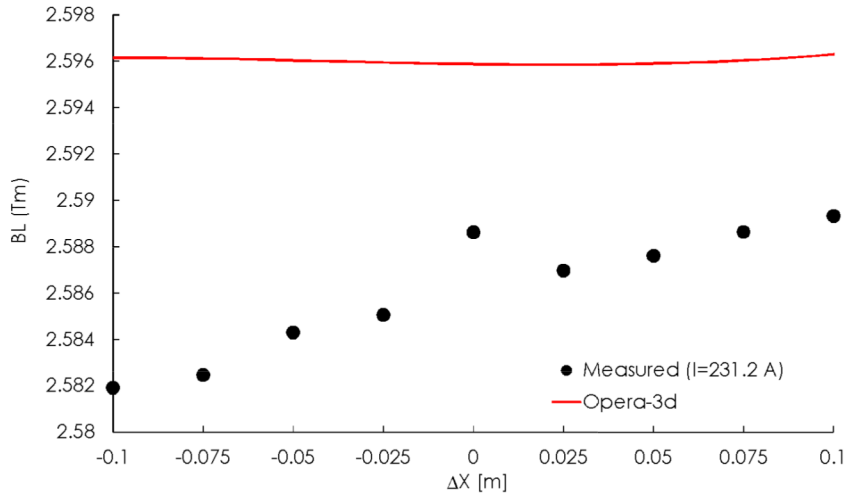
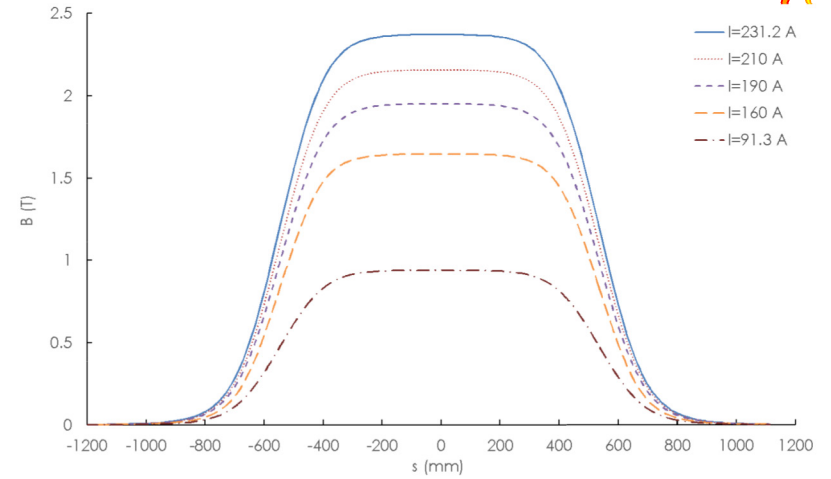
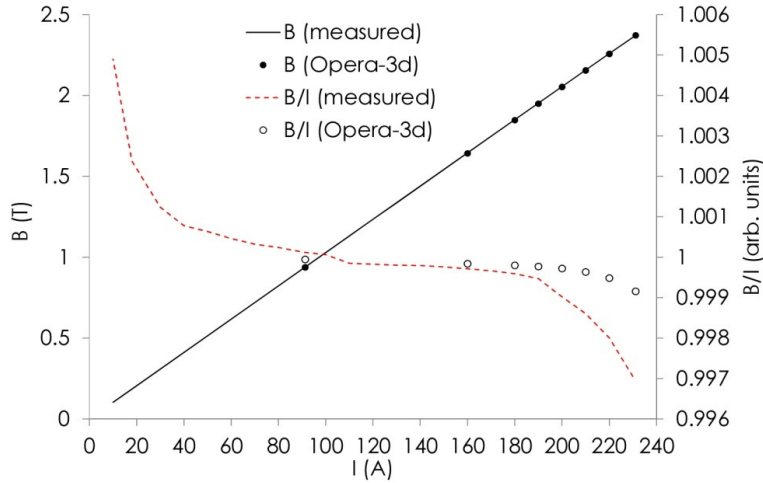
Field measurements



- Magnetic field measurements were performed
 - to verify the SC magnet design



Some results for BM10

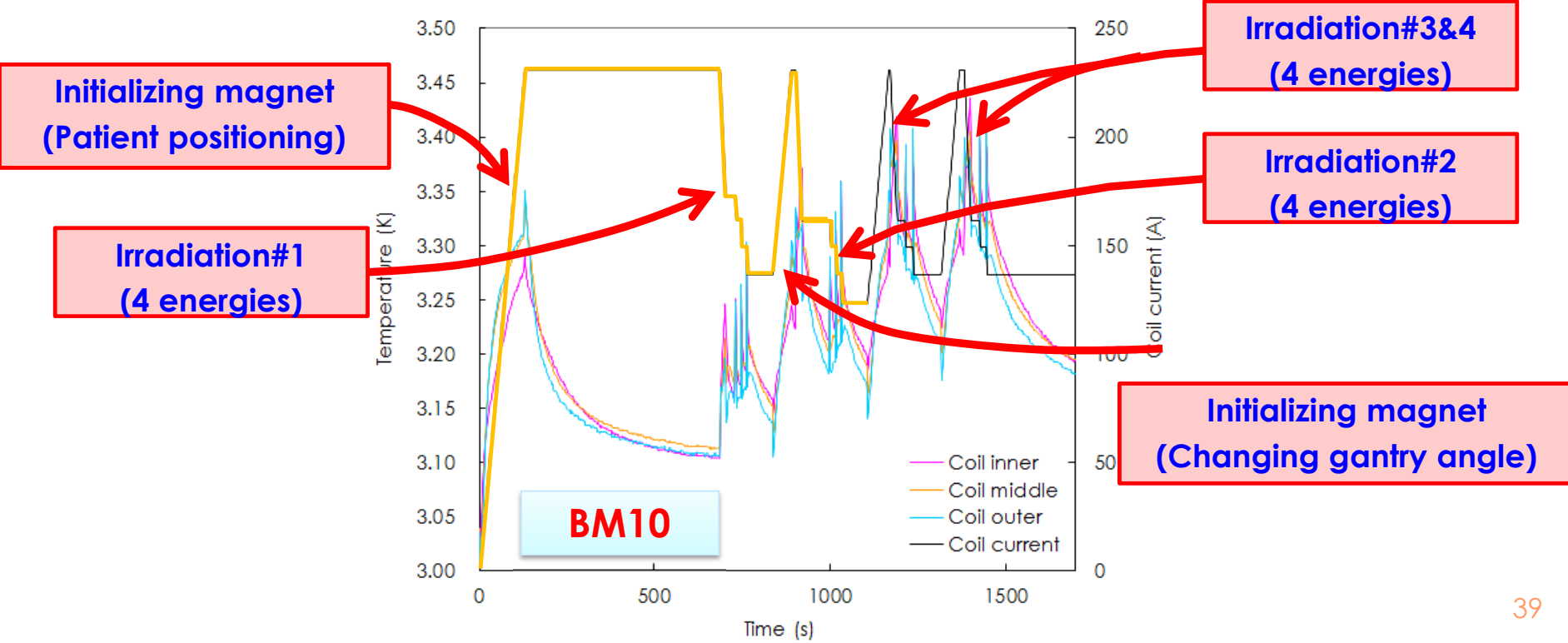


Fast slewing tests (1)

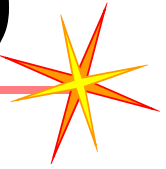


- Simulating irradiation for
 - lung cancer (4 shots), using
 - Multiple-energy operation using 1 1-flattop pattern

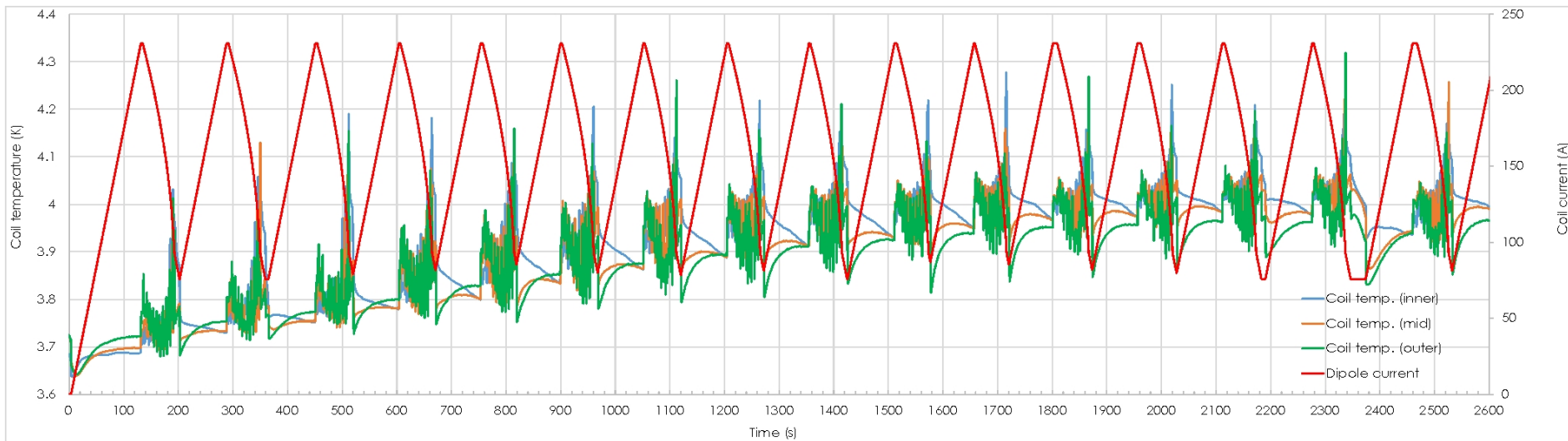
No quench observed!

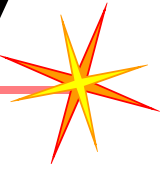


Fast slewing tests (2)



- Simulate 201-flattop pattern (BM10)
- Each flattop : 300ms
- **No quench observed**
- **Average temperature converged around 4.0 K**
- **Similar results for the other SC magnets**





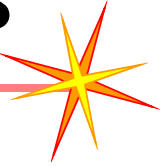
- **3D raster scanning irradiation**
 - **Fast scanning for moving target**
- **Multiple-flattop operation**
 - **11-flattop operation: currently used in treatment**
 - **201-flattop operation: tests succeeded. To be used in treatment operation**





- **Design of the SC rotating-gantry**
 - **Compact (~proton gantries)**
 - **Construction and tests of the 5 SC magnets**
 - **Test results agreed with those designed**
- **Future plan**
 - **All the construction and installation will be made by the end of FY2014 (March 2015)**
 - **Commissioning will be made in FY2015**





- K. Noda, T. Shirai, T. Murakami, T. Furukawa, T. Fujita, K. Shouda, S. Sato, K. Mizushima, Y. Hara, and S. Suzuki (NIRS)
- T. Fujimoto, H. Arai (AEC)
- T. Orikasa, S. Takayama, Y. Nagamoto, T. Yazawa (Toshiba)
- T. Ogitsu (KEK)
- T. Obana (NIFS)
- N. Amemiya (Kyoto Univ.)