

Present status of a superconducting rotating gantry for carbon therapy

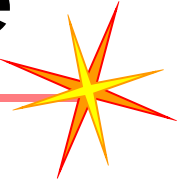


Yoshiyuki Iwata

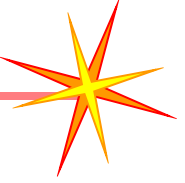
National Institute of Radiological Sciences (NIRS)



2015/9/11

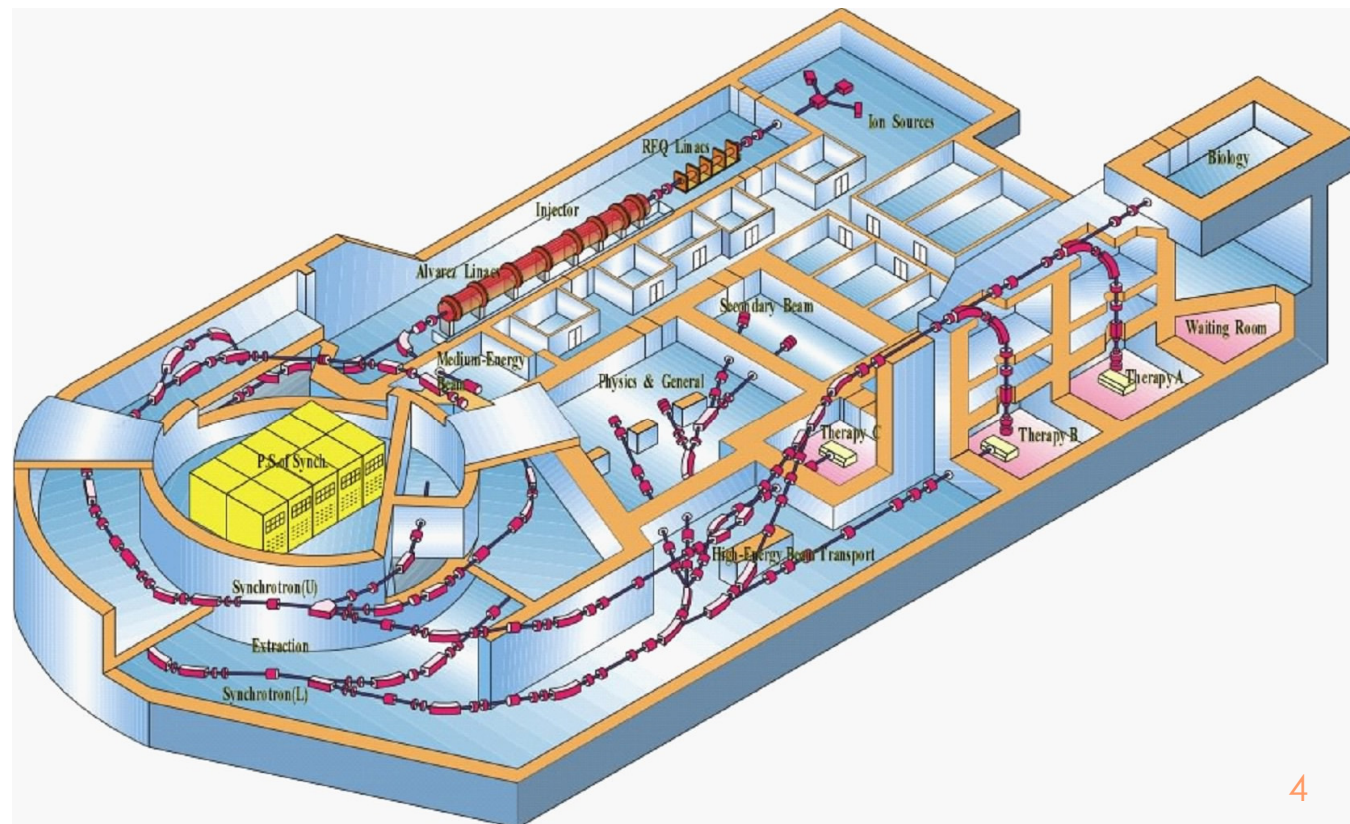
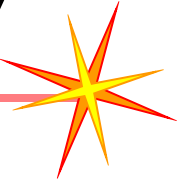


- Introduction
- Gantry developments
 - Superconducting magnets
 - Construction of gantry structure
- Summary

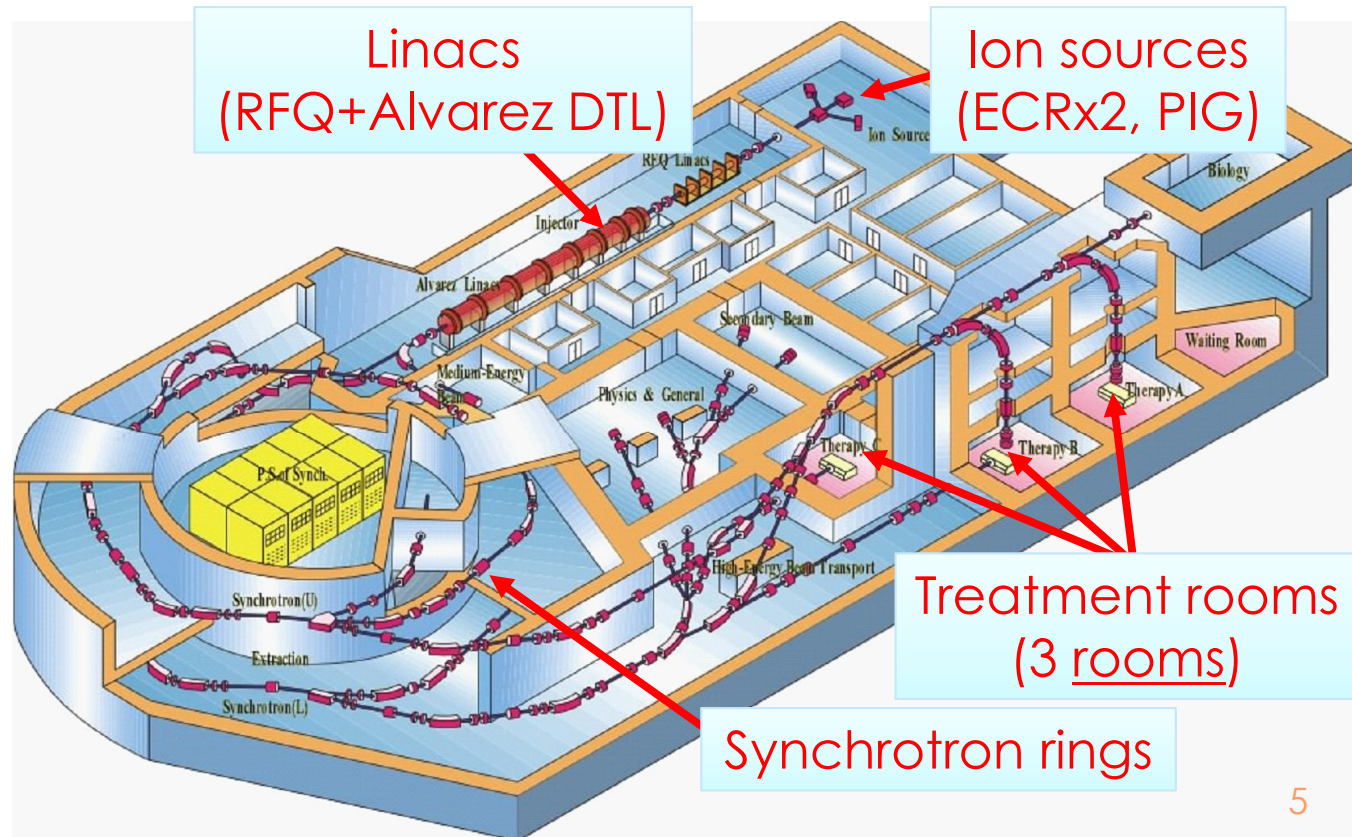
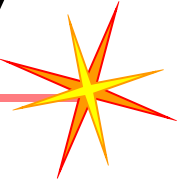


Introduction

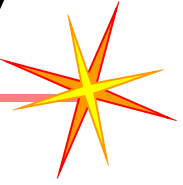
Carbon radiotherapy



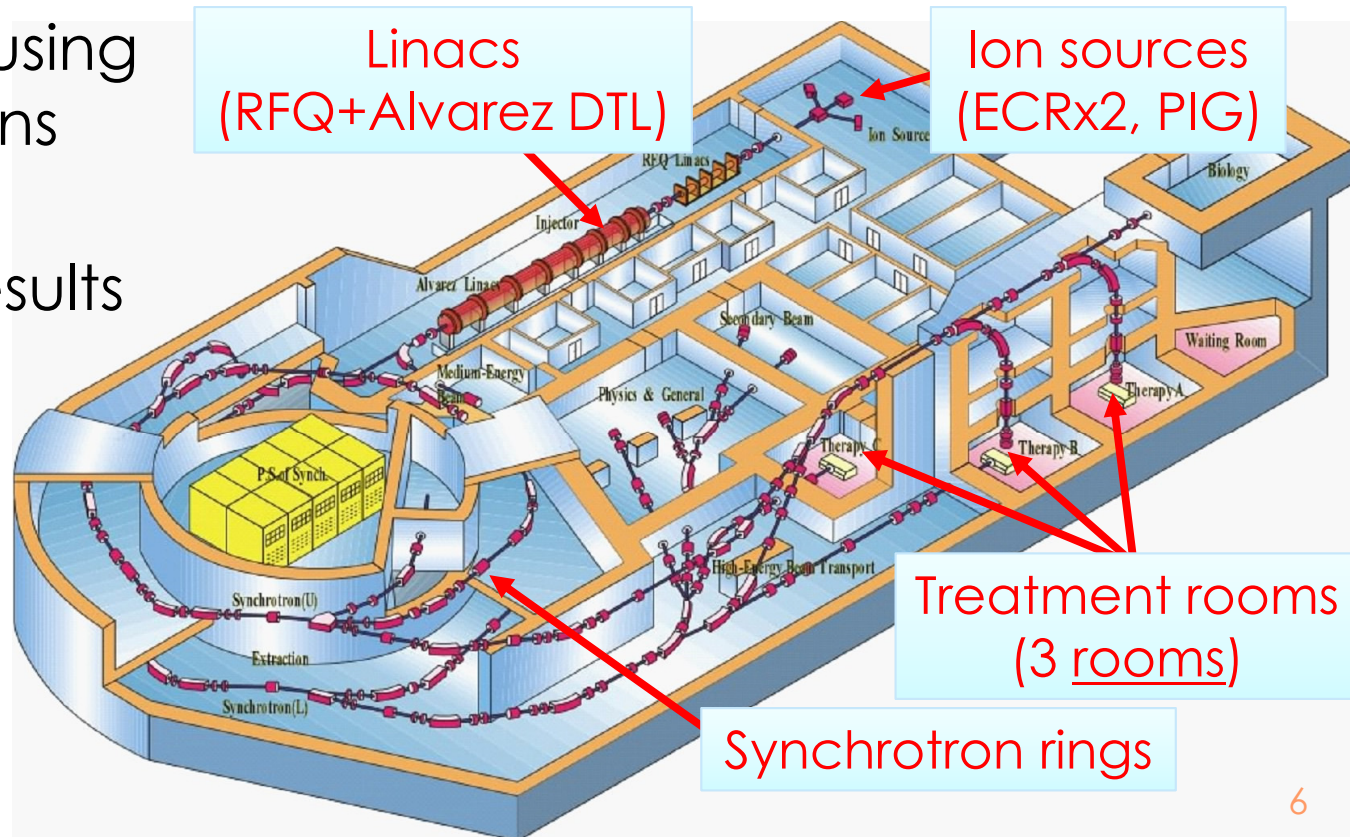
Carbon radiotherapy



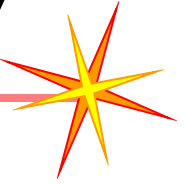
Carbon radiotherapy



- Heavy Ion Medical Accelerator in Chiba (HIMAC)
- Ion species: p ~ Xe
- $E/A=800$ MeV for $q/m=1/2$
- Cancer treatments using energetic carbon ions since 1994
- Successful clinical results
~9000 patients



New treatment facility



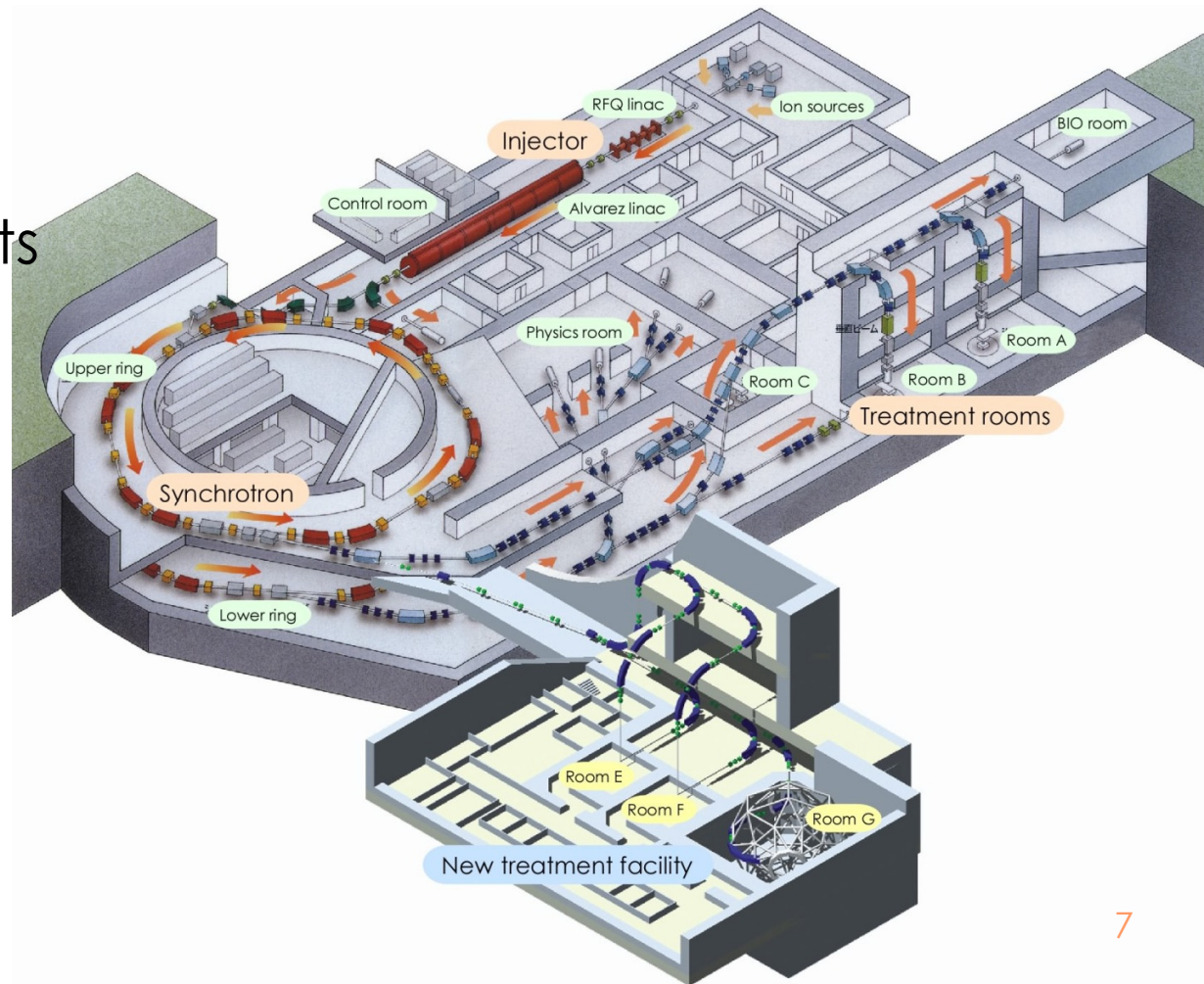
- Construction completed in FY2010
- 3 treatment rooms

- Room E & F

Fixed H&V scanning ports
(in treatment operation)

- **Room G**

**Rotating gantry port
(Under construction)**



New treatment facility

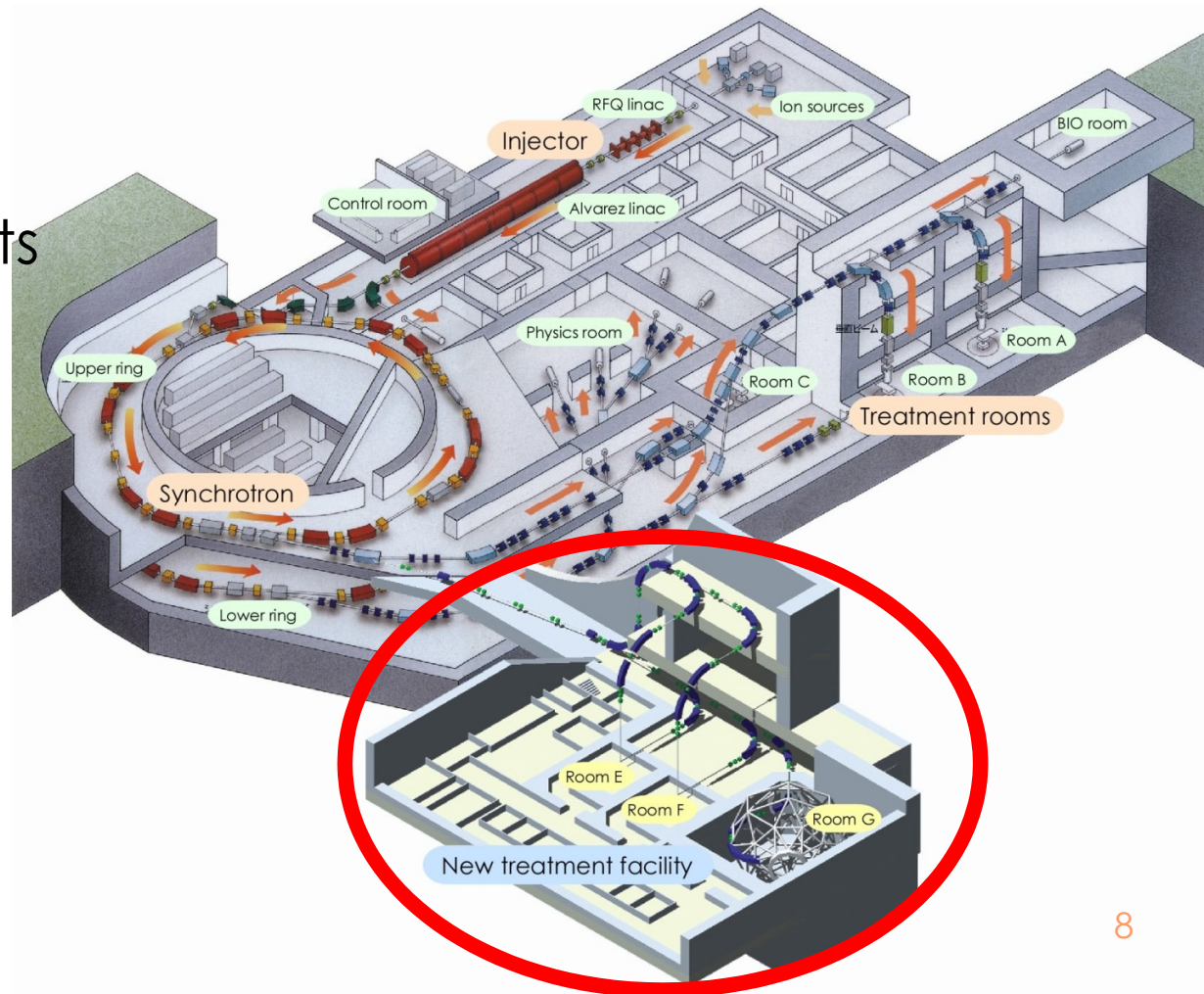
- Construction completed in FY2010
- 3 treatment rooms

- Room E & F

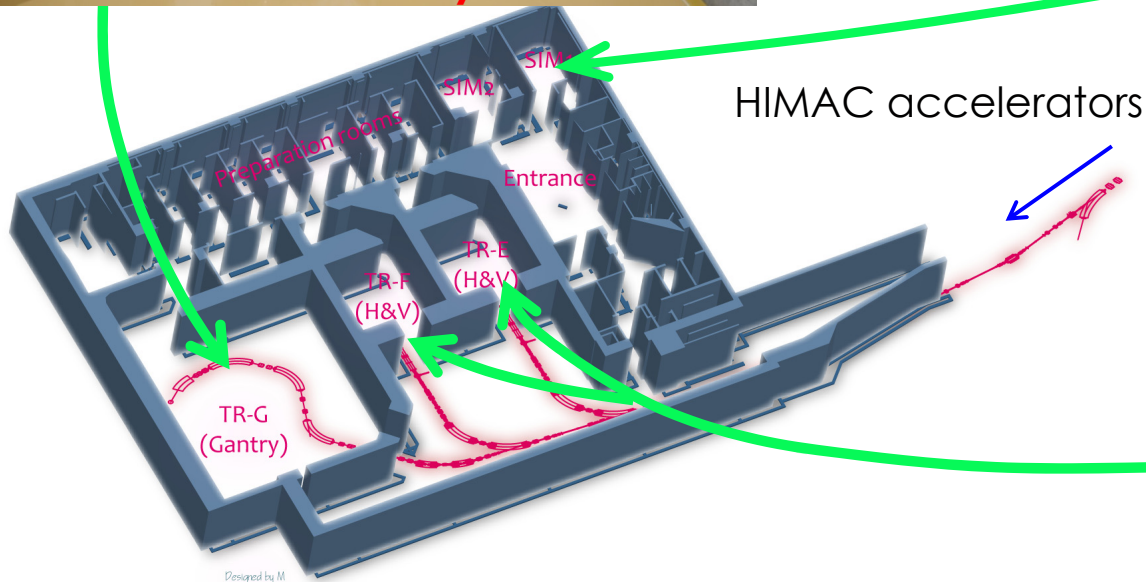
Fixed H&V scanning ports
(in treatment operation)

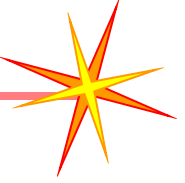
- Room G**

Rotating gantry port
(Under construction)



Treatment floor (B2F)



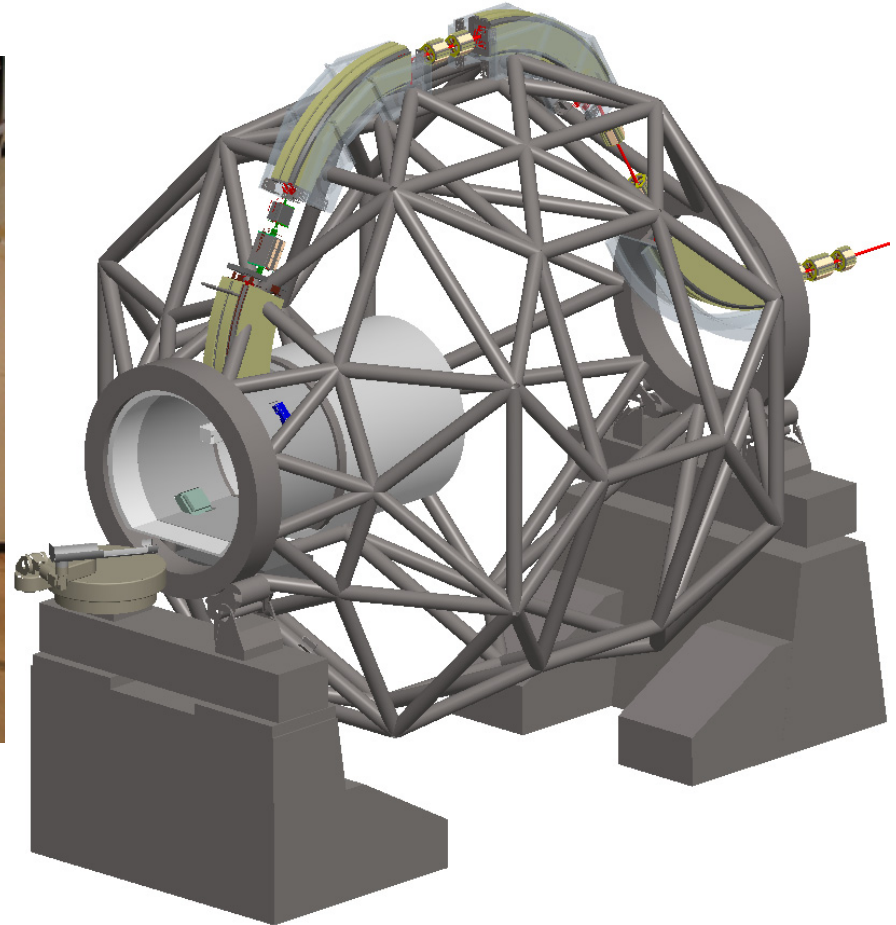


Rotating gantry in hadron radiotherapy

Needs for a rotating gantry



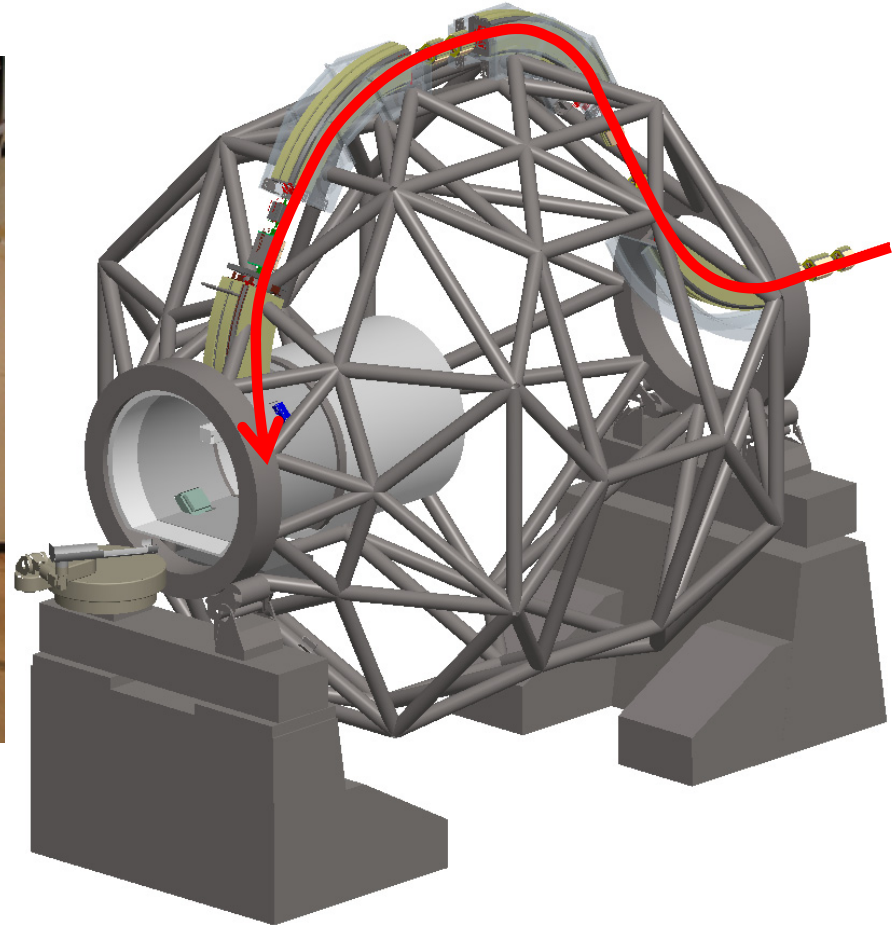
Irradiation with the existing fixed port



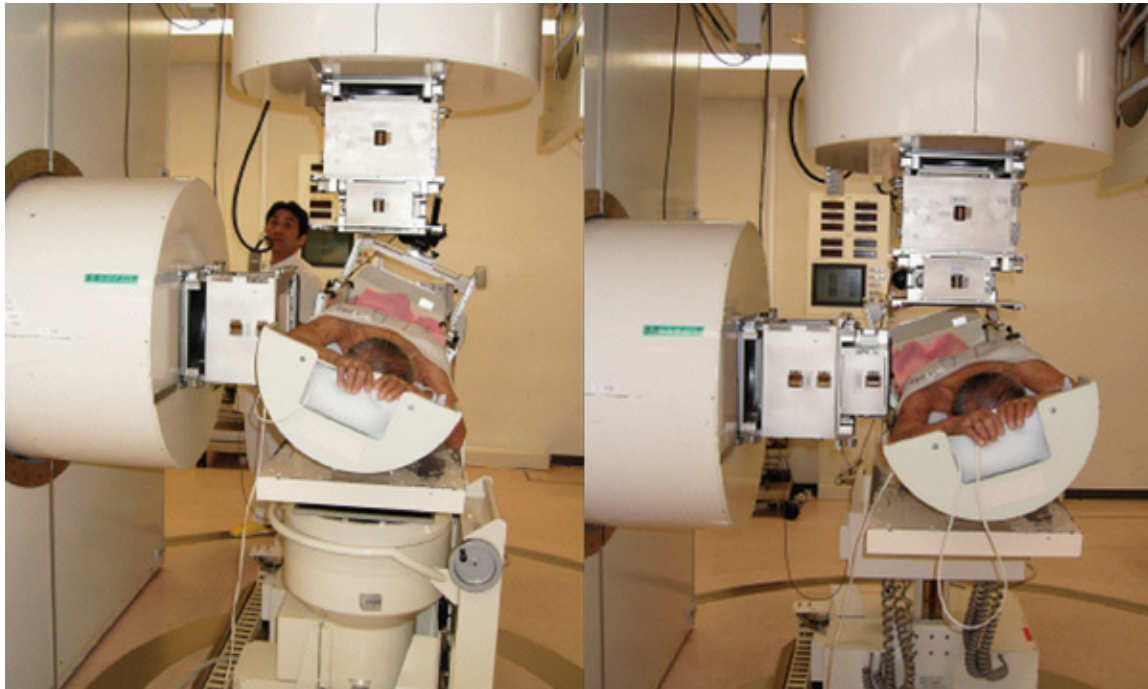
Needs for a rotating gantry



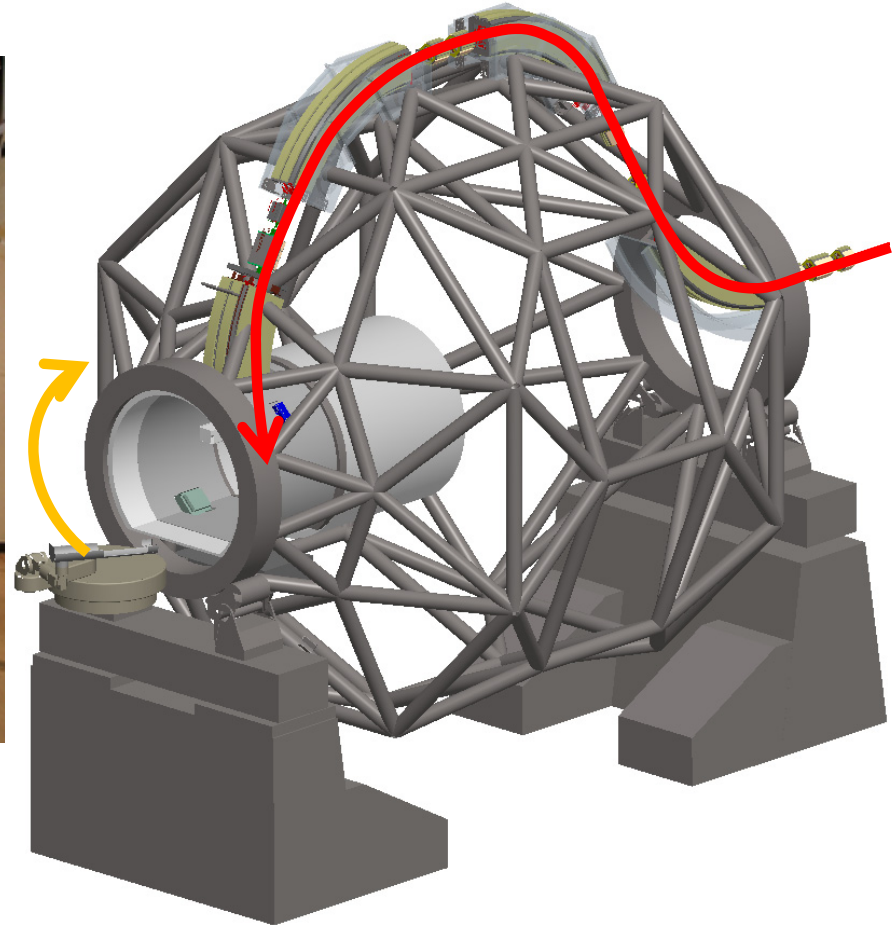
Irradiation with the existing fixed port



Needs for a rotating gantry



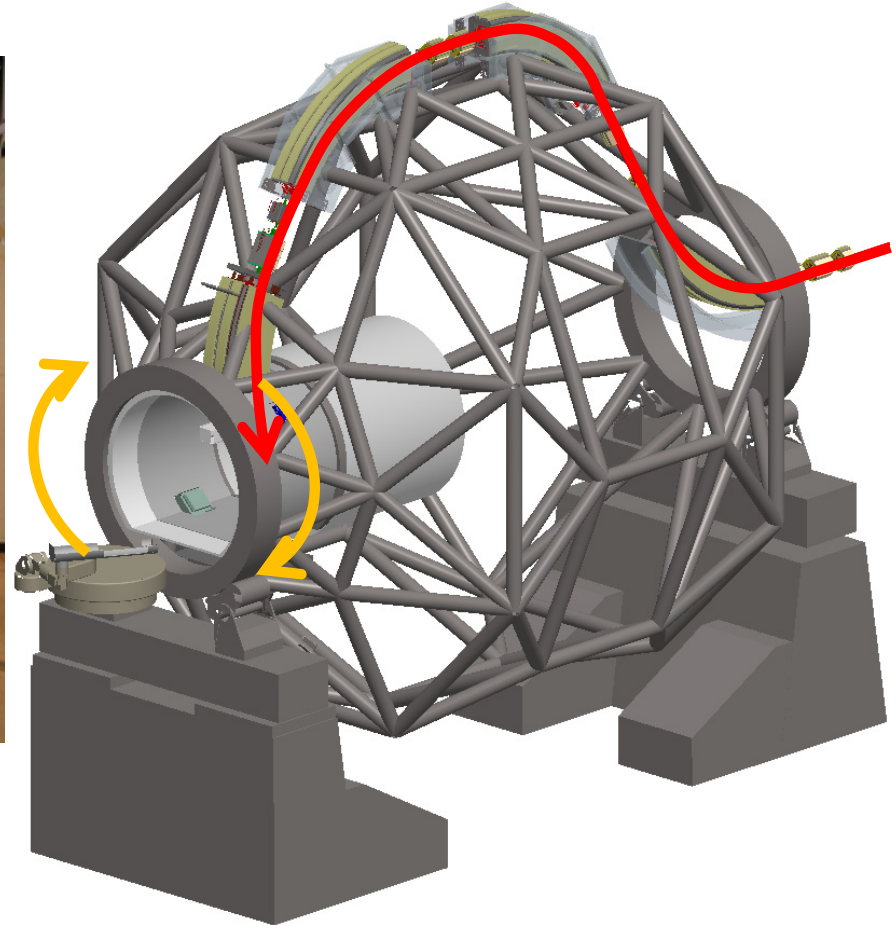
Irradiation with the existing fixed port



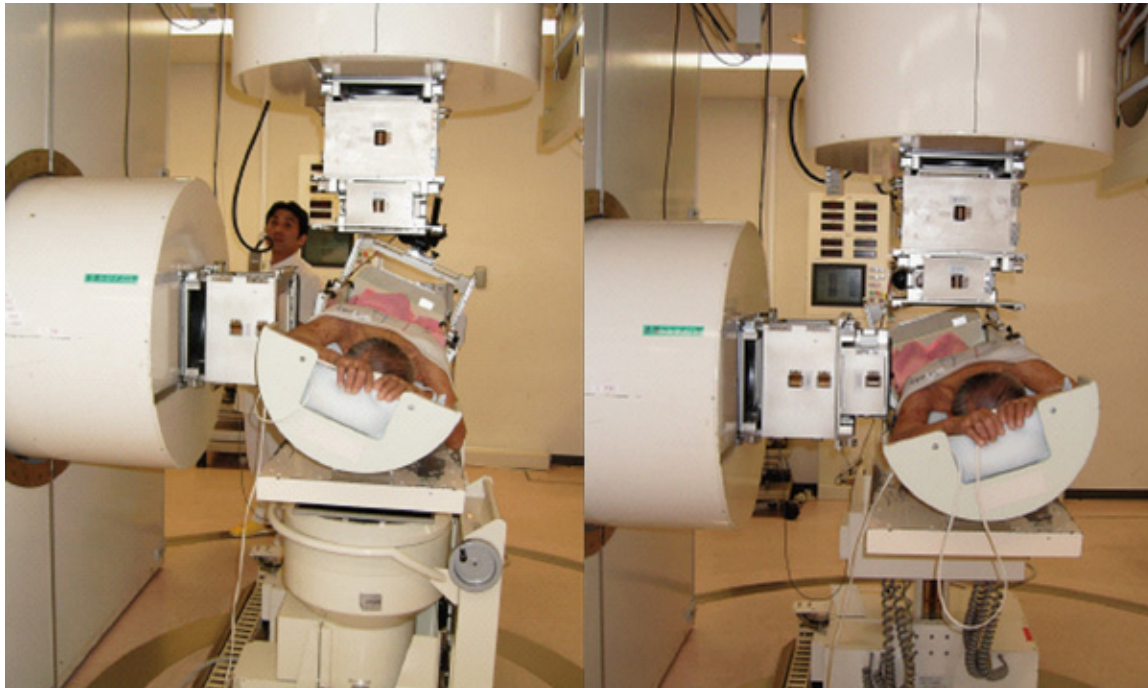
Needs for a rotating gantry



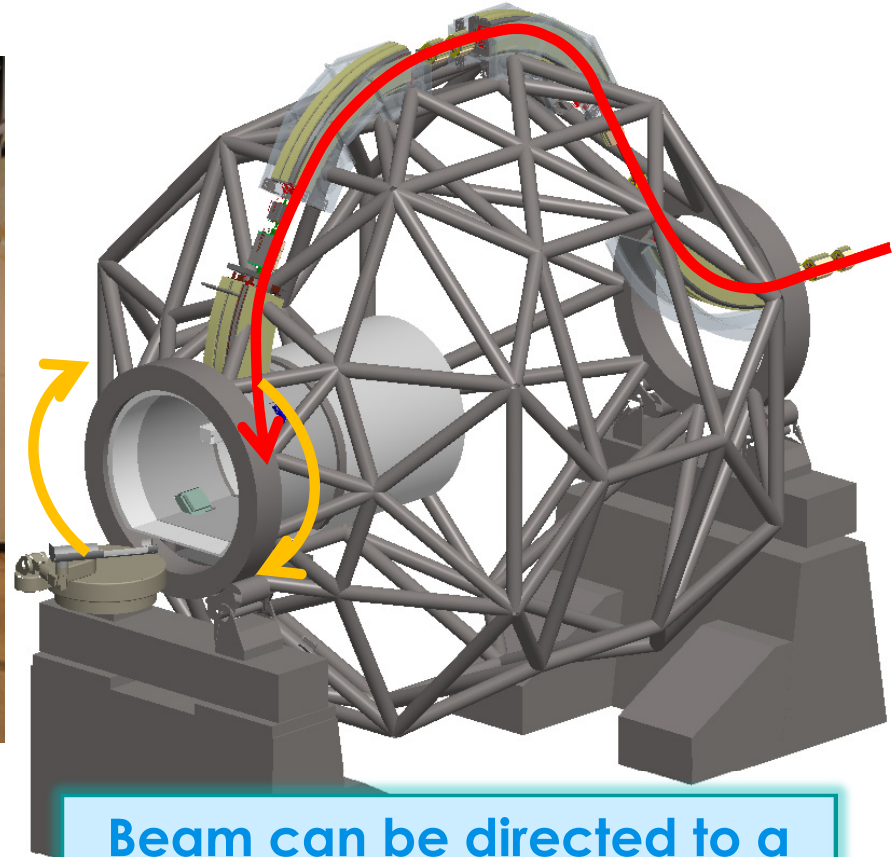
Irradiation with the existing fixed port



Needs for a rotating gantry



Irradiation with the existing fixed port



Beam can be directed to a target from **any of medically desirable angles**

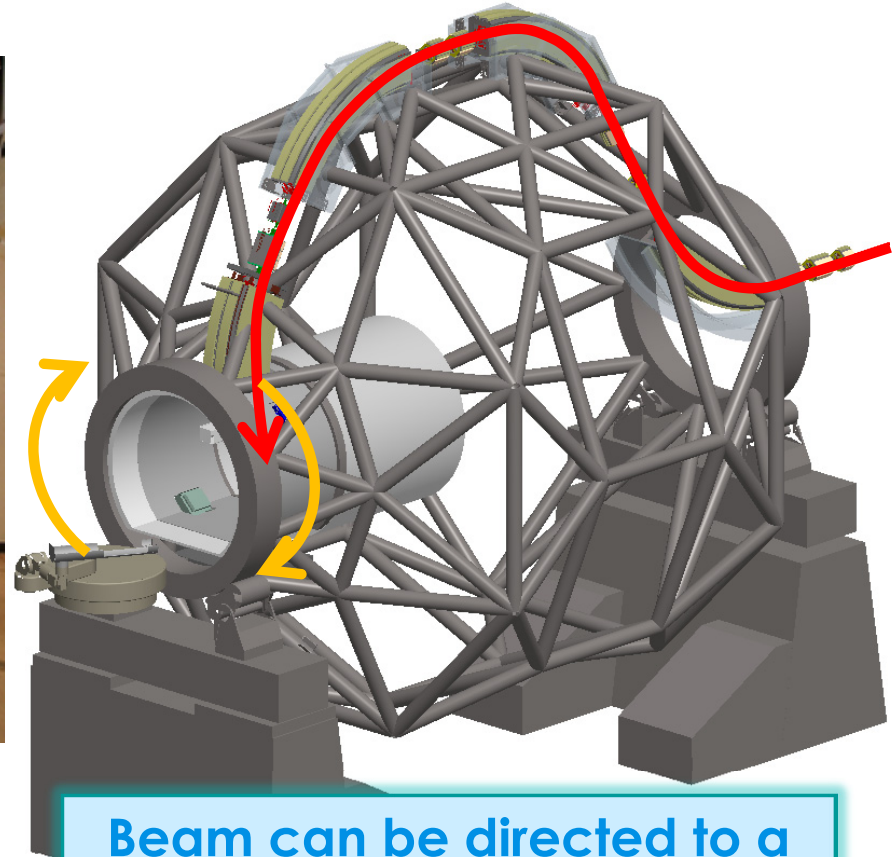
Needs for a rotating gantry



【Advantage of a rotating gantry】

1. No need to rotate a patient
2. Accurate dose distributions
3. Intensity Modulated Particle Therapy (IMPT)

Irradiation with the existing fixed port



Beam can be directed to a target from **any of medically desirable angles**

Rotating gantry for hadron therapy

- **Proton therapy**
 - Gantry is commonly used
 - Commercially available
- **Carbon therapy**
 - Required B_p is 3 times higher
 - Magnets will be very large and heavy
 - Difficult to
 - Design
 - Construct



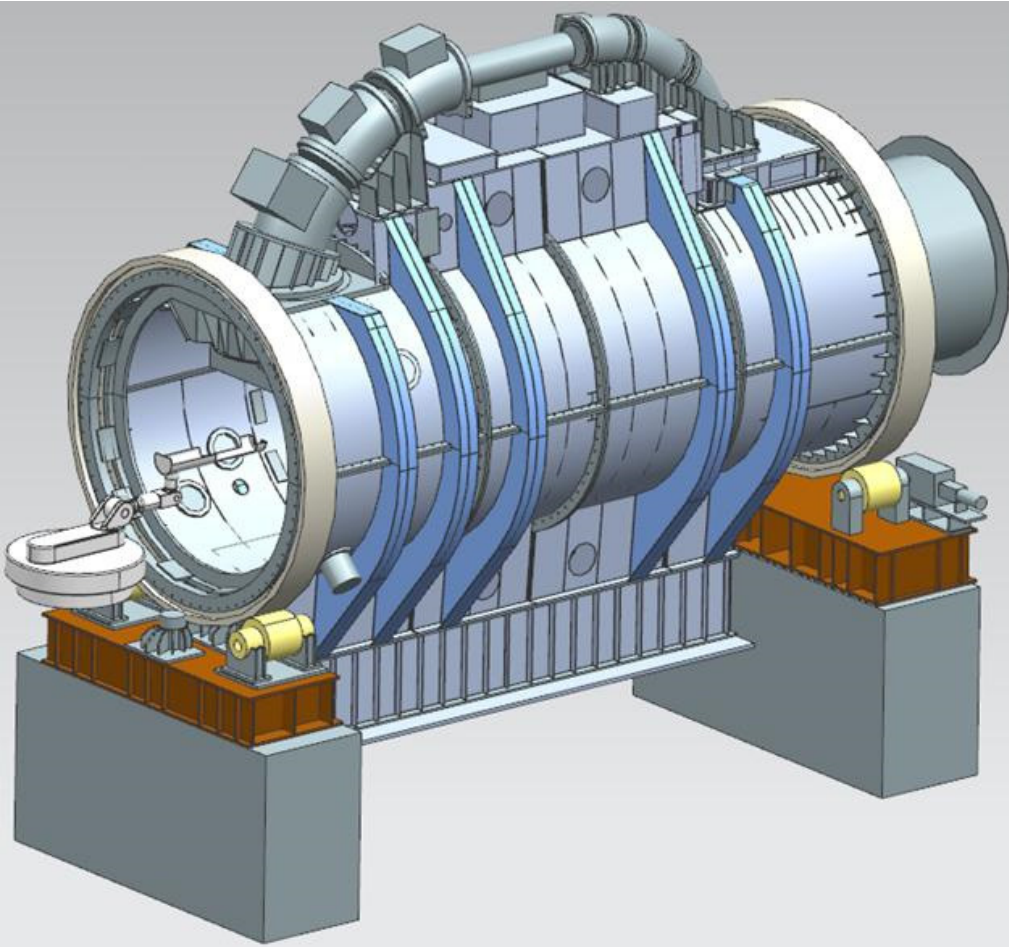
Rotating gantry for carbon therapy

- **Only one gantry in the world**
 - Heidelberg Ion Beam Therapy Center (HIT)
 - World first carbon-gantry
 - Clinical use since November 2012
 - Weight: 600 tons
(rotating part)



<http://idw-online.de/pages/de/news504069>

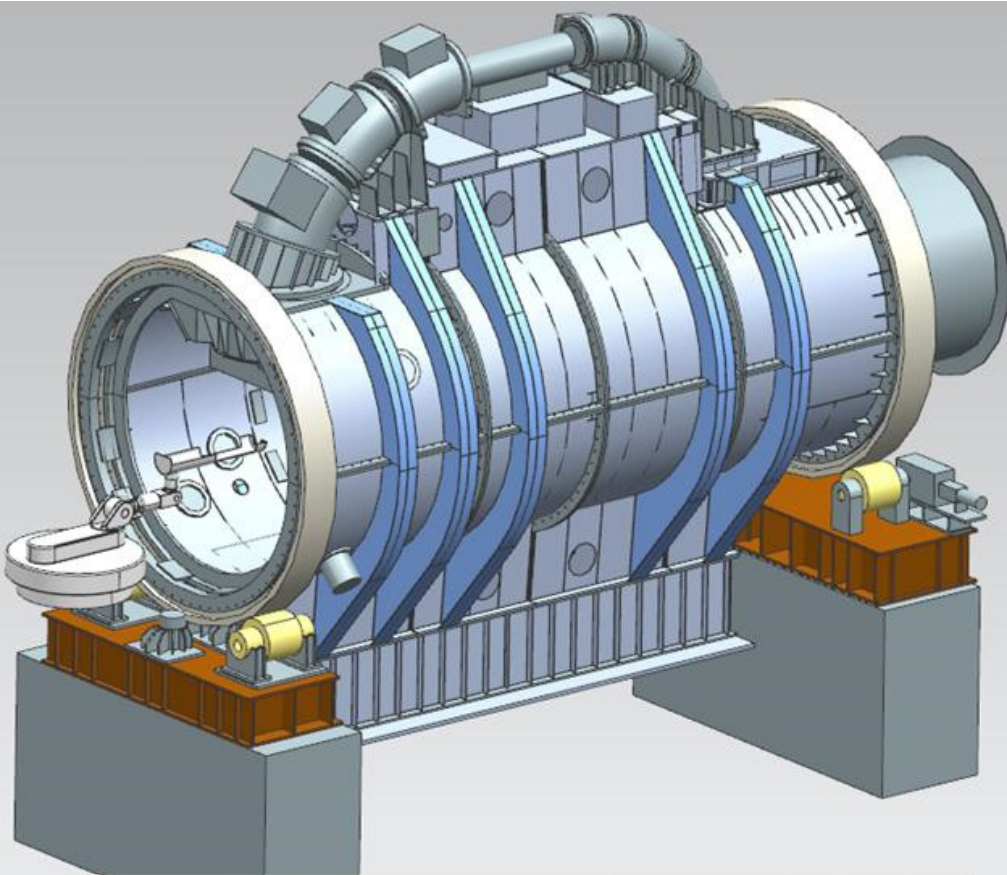
Superconducting rotating-gantry



Use of superconducting (SC) magnets

Ion kind : ^{12}C
 Irradiation method: 3D Scanning
 Beam energy : 430 MeV/n
 Maximum range : 30 cm in water
 Scan size : $\square 200 \times 200 \text{ mm}^2$
 Beam orbit radius : 5.45 m
 Length : 13 m

Superconducting rotating-gantry



Weight: order of 300 tons

Use of superconducting (SC) magnets

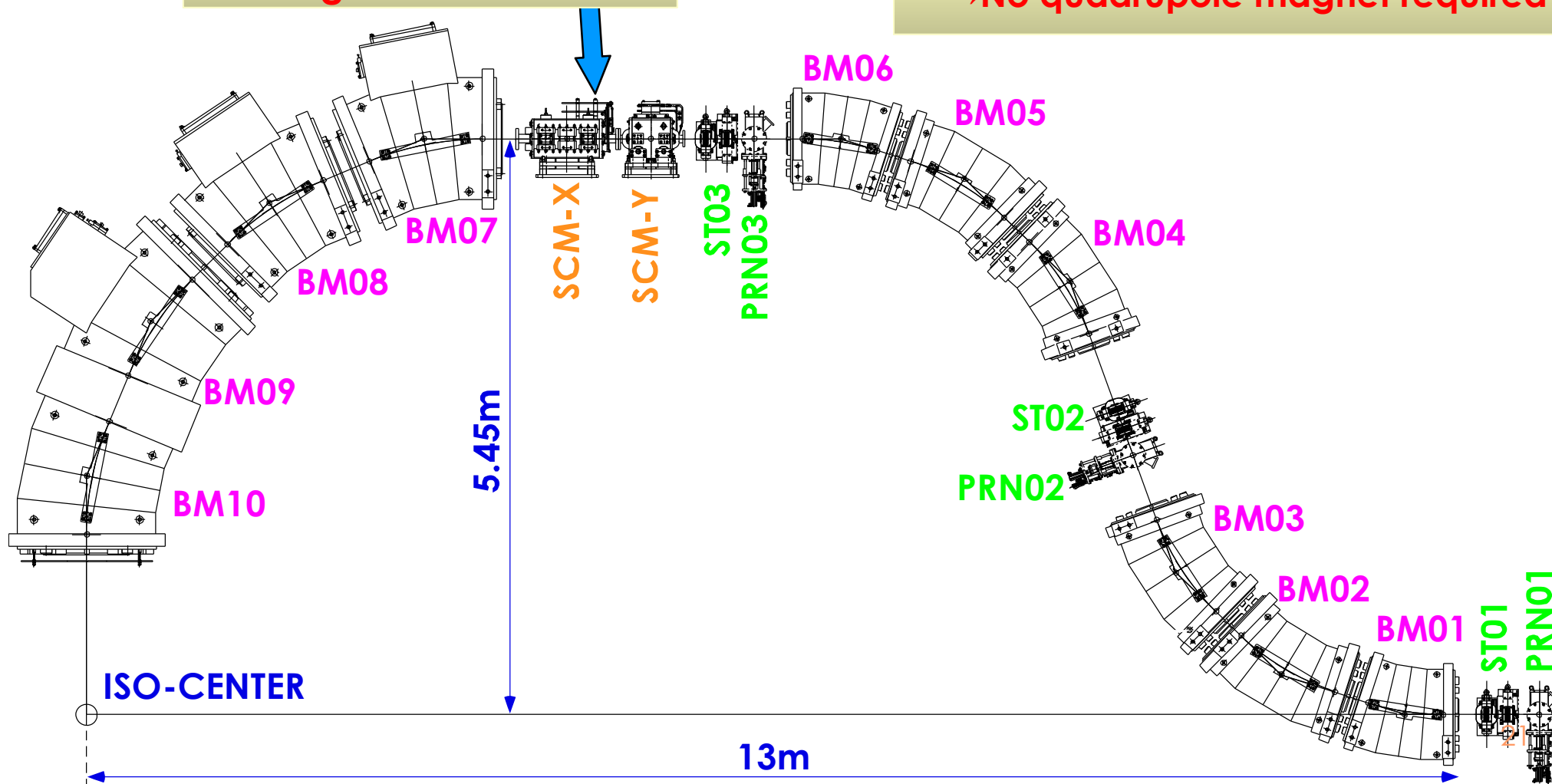
Ion kind : ^{12}C
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 Length : 13 m

The size and weight are considerably reduced

Layout of the SC gantry

Scanning magnets on top
→ Large scan size

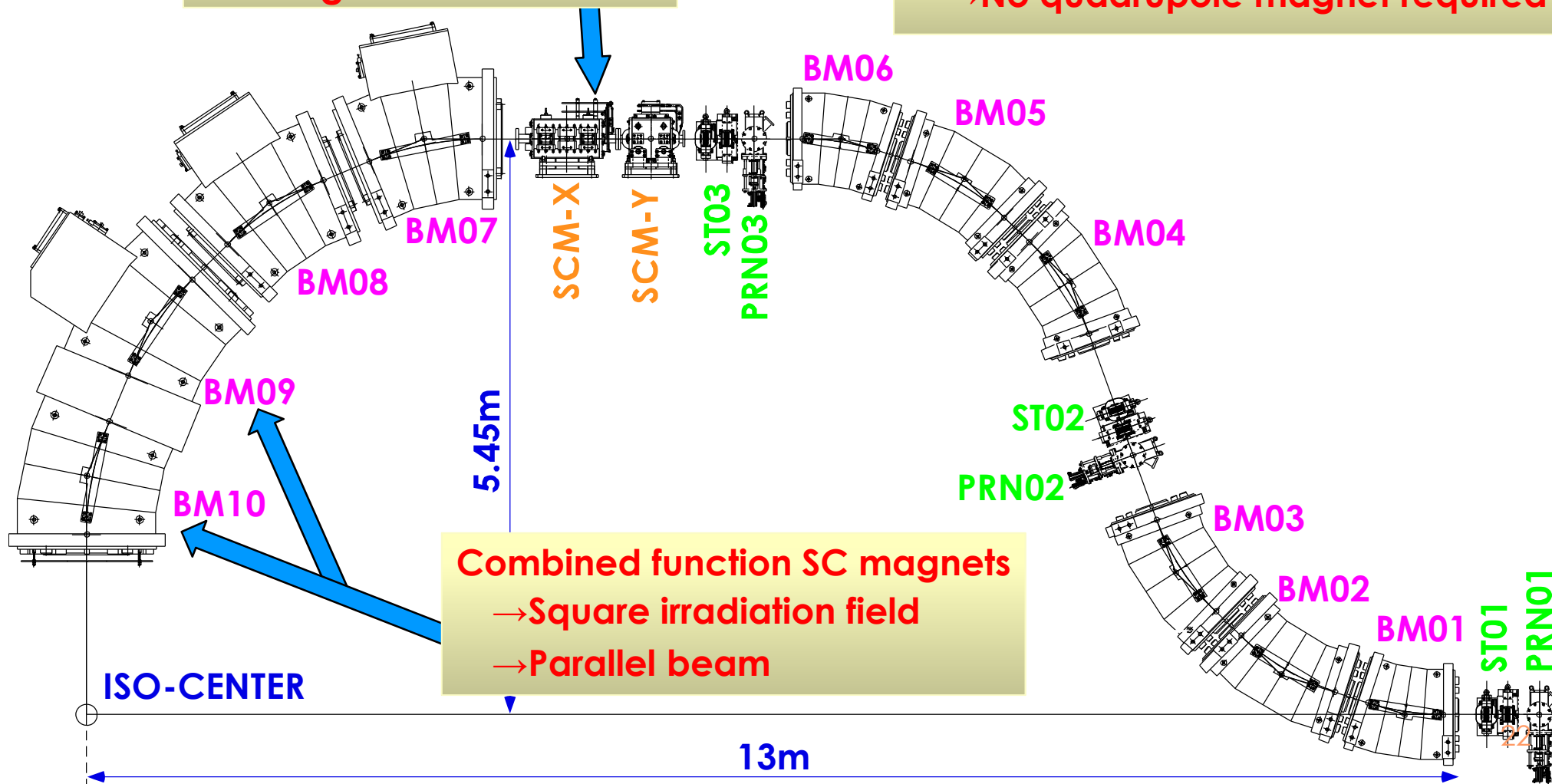
Combined function SC magnets
→ No quadrupole magnet required



Layout of the SC gantry

Scanning magnets on top
→ Large scan size

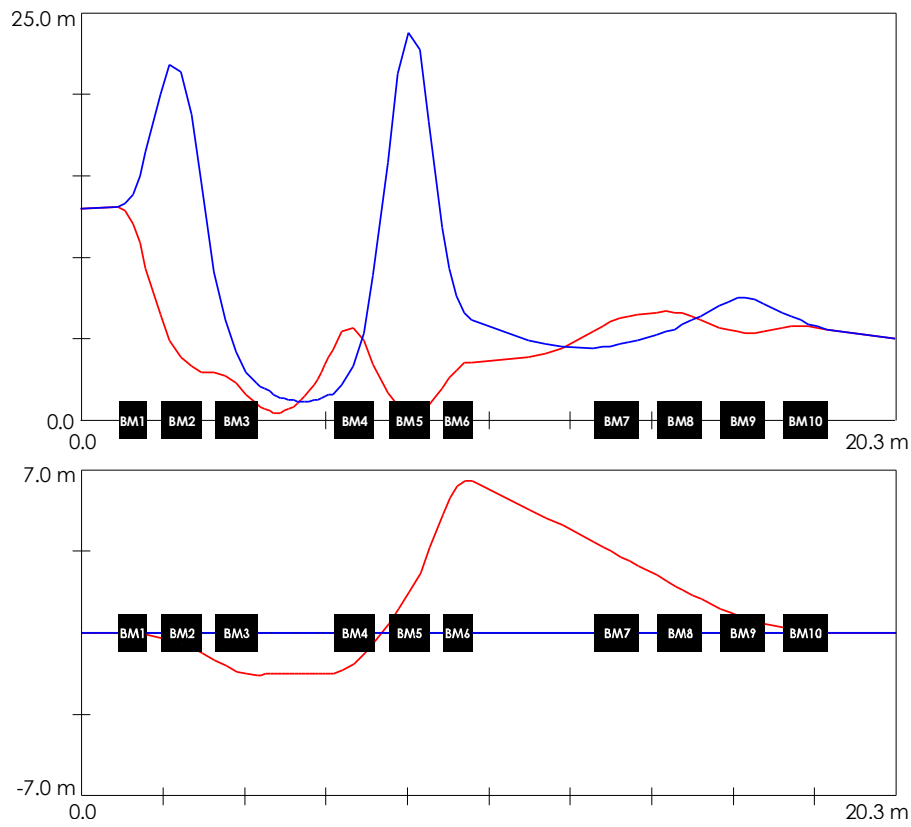
Combined function SC magnets
→ No quadrupole magnet required



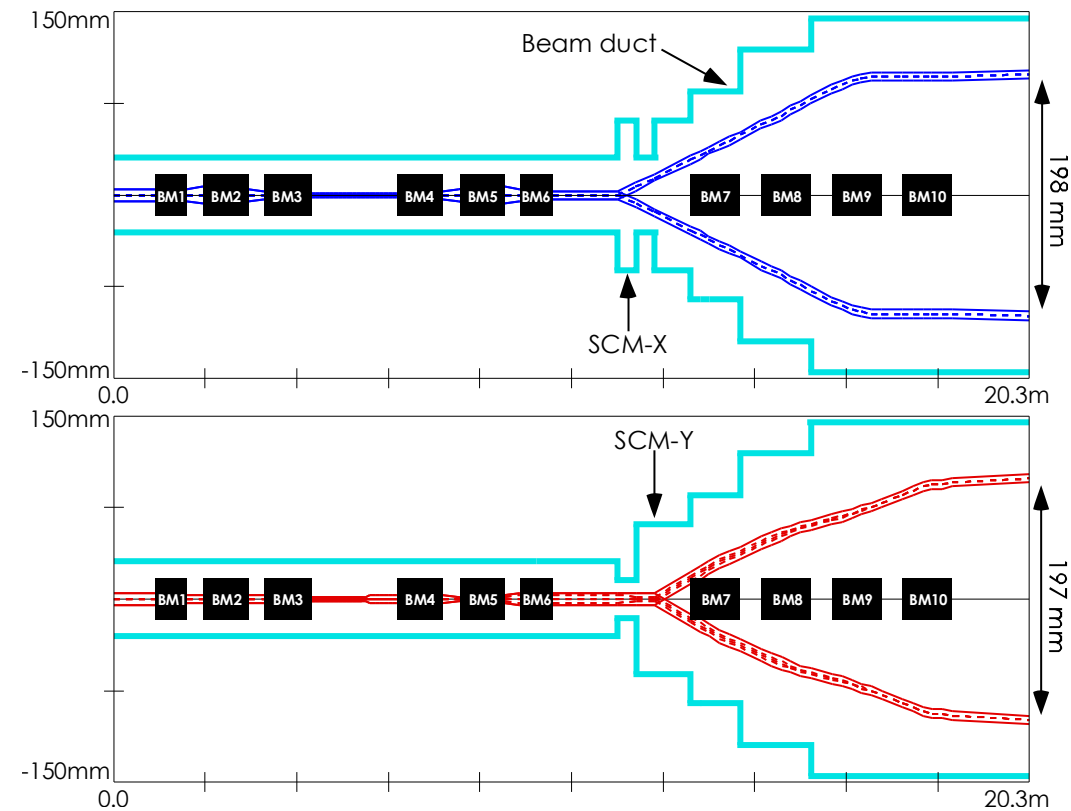
Beam optics design

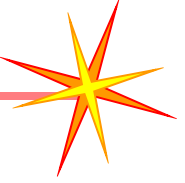


Beta and dispersion functions



Beam envelope functions with kicks of scanning magnets





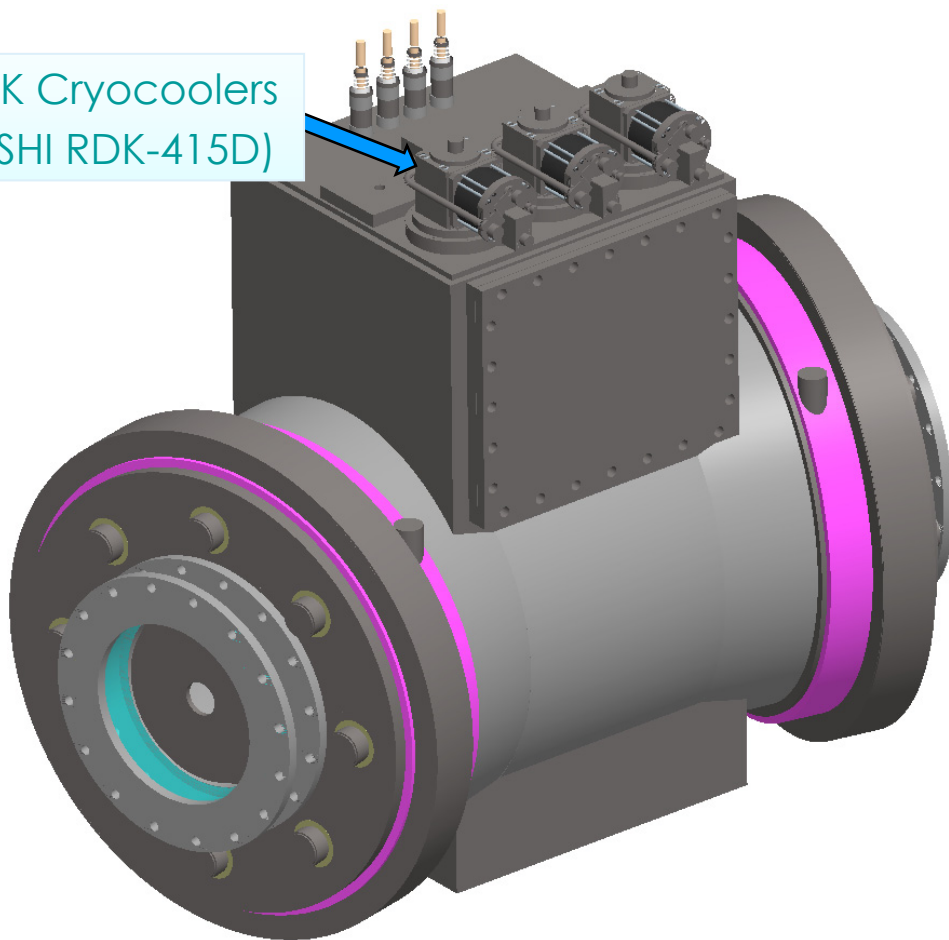
Development of superconducting magnets

Development of curved SC magnets



SC magnet (BM02-05)

4K Cryocoolers
(SHI RDK-415D)

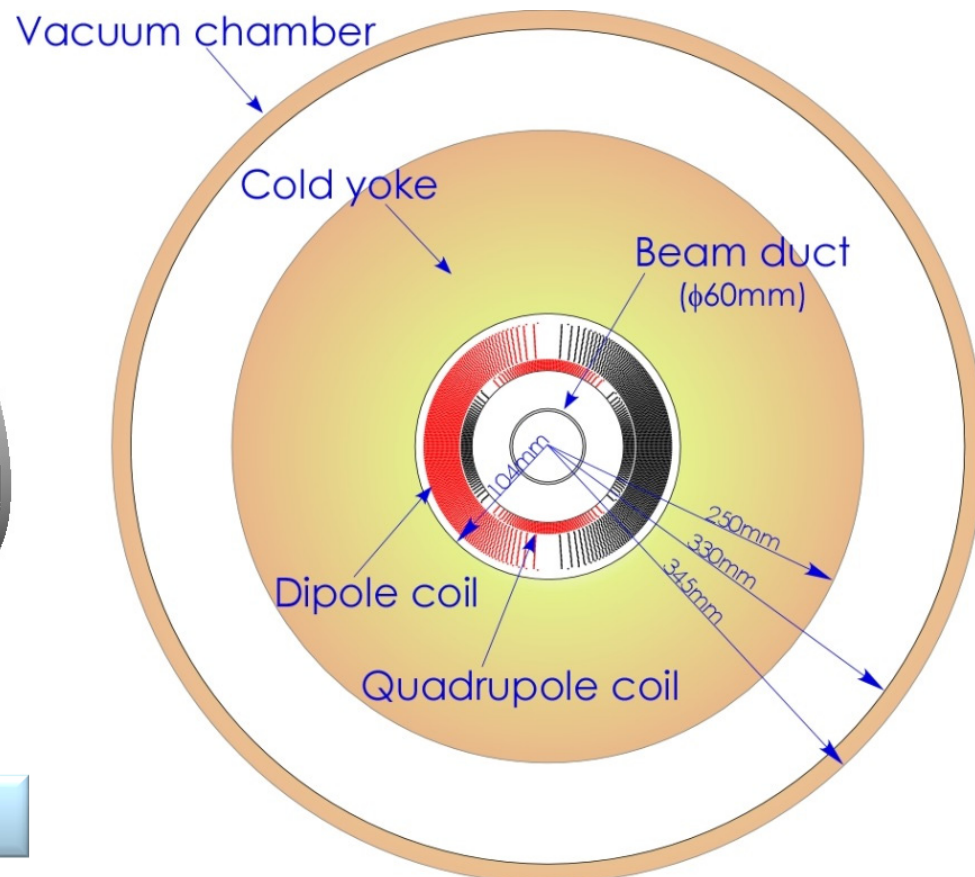
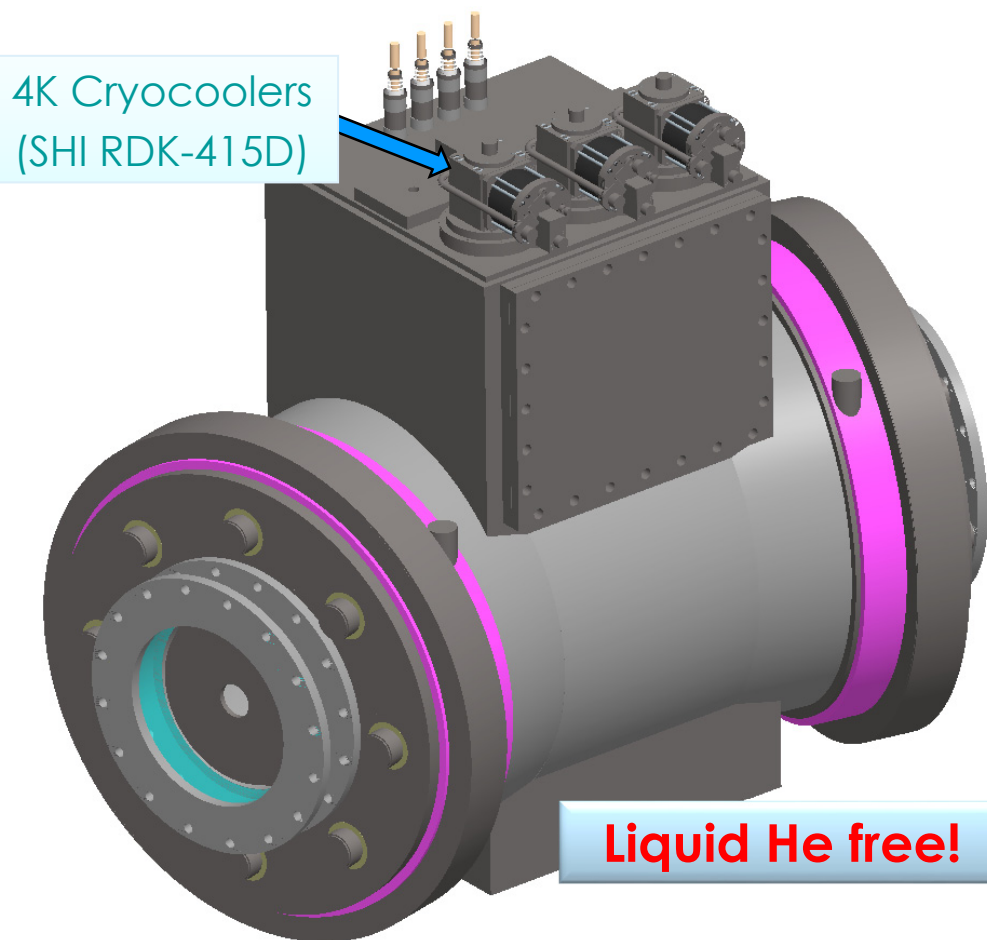


Development of curved SC magnets



SC magnet (BM02-05)

Cross-sectional view

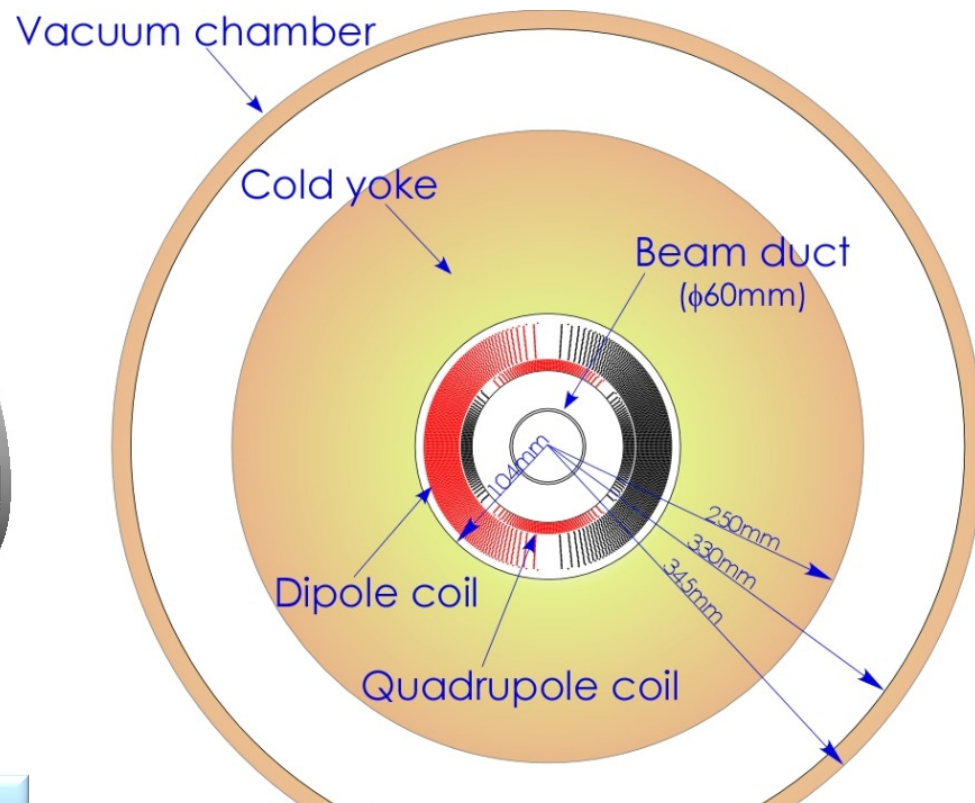
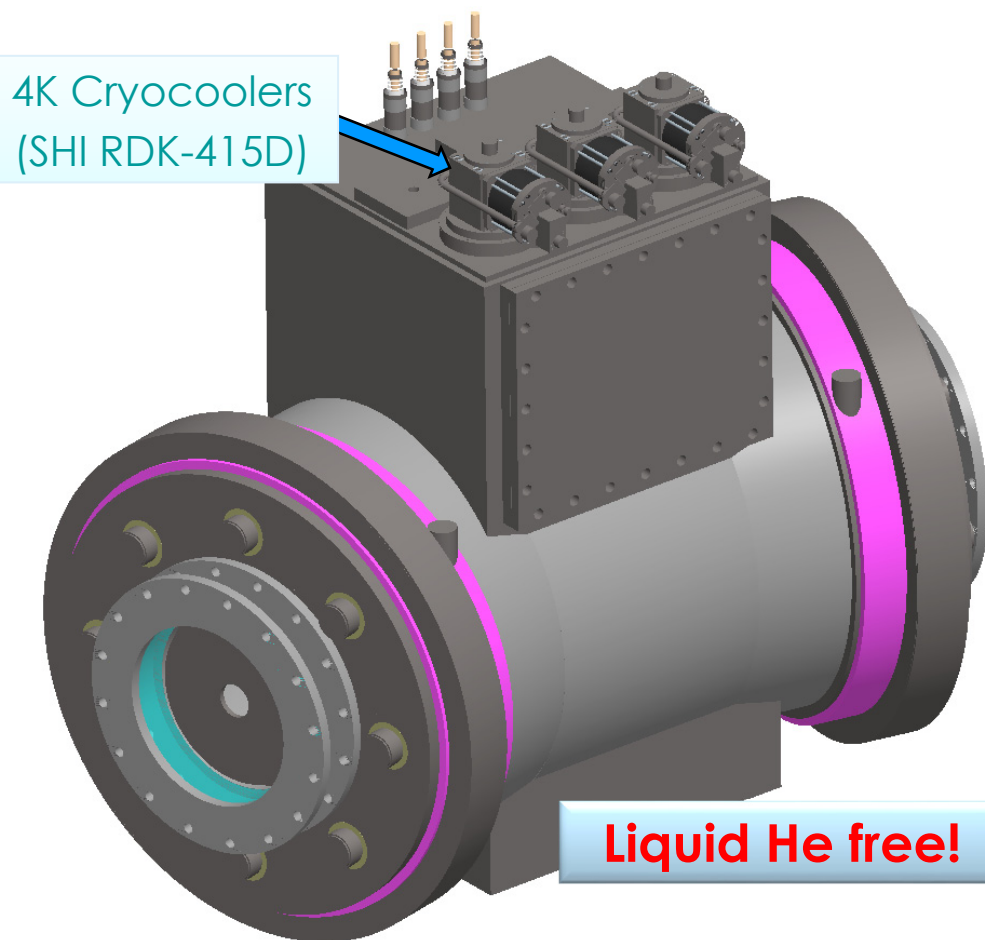


Development of curved SC magnets



SC magnet (BM02-05)

Cross-sectional view

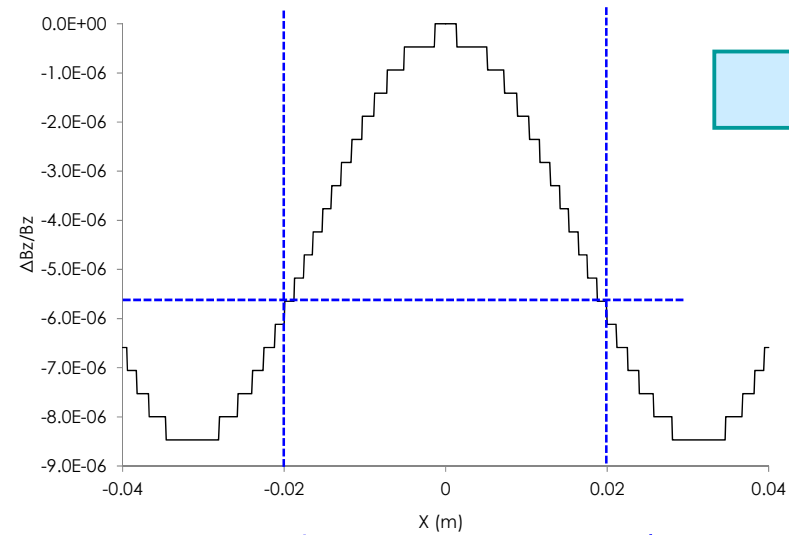
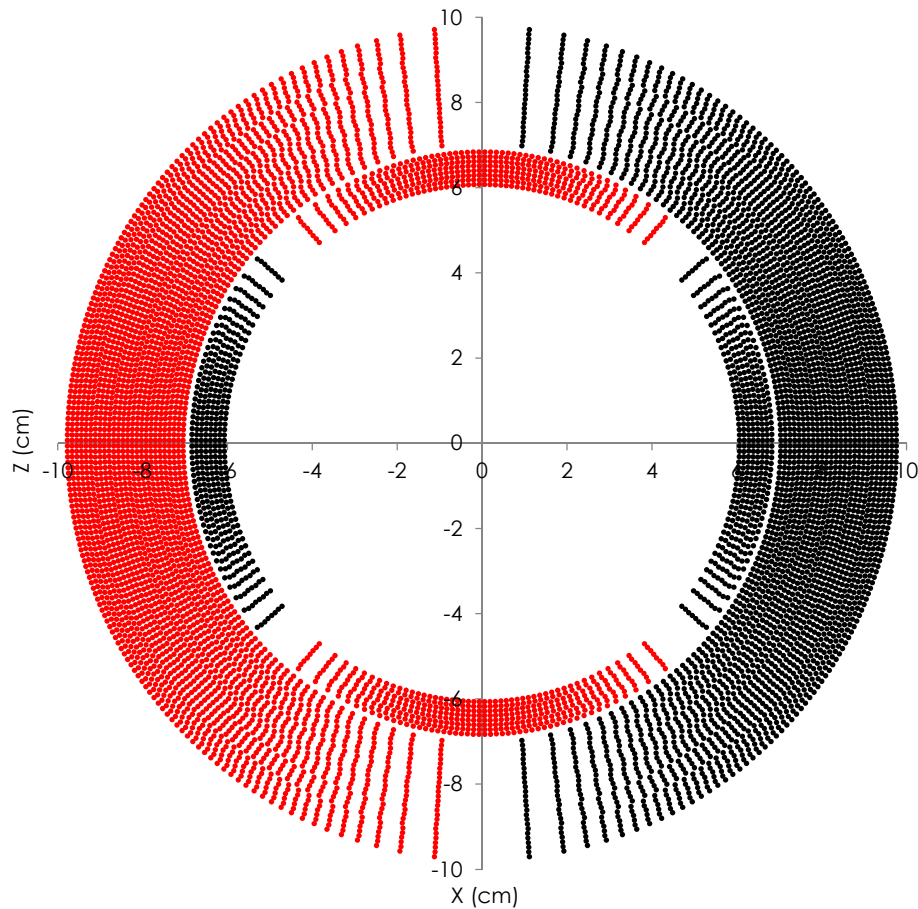


Dipole and quadrupole coils can be independently excited

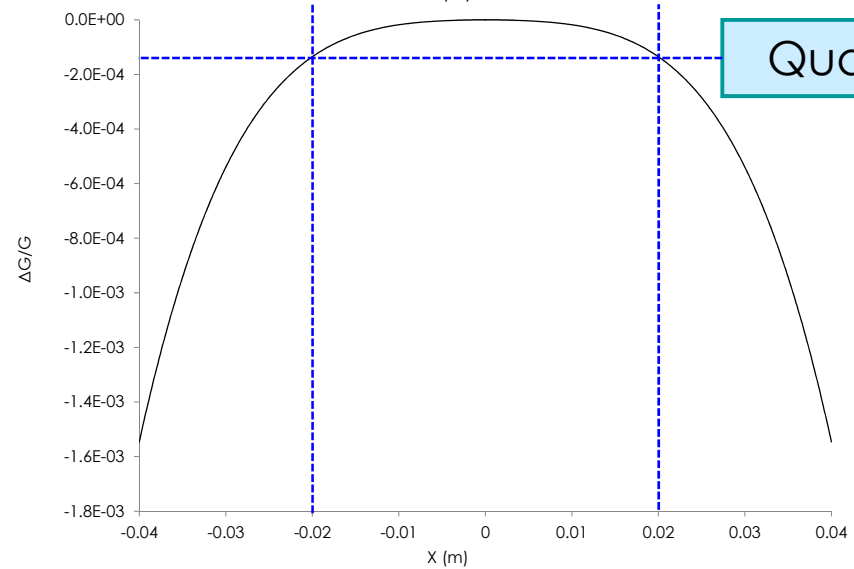
Design of superconducting coils



2D field calculation
(BM02-BM05)



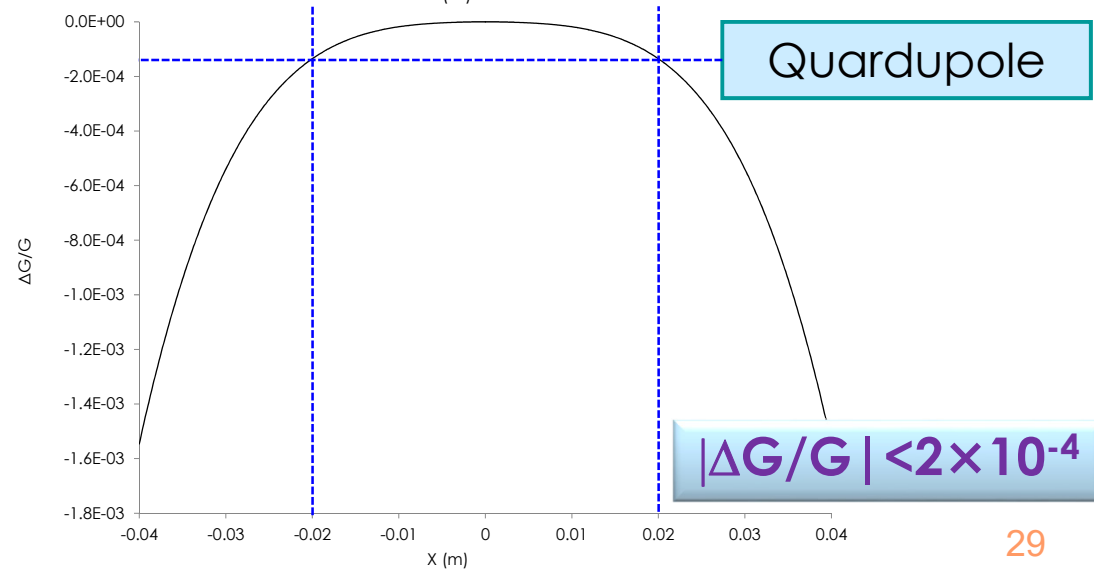
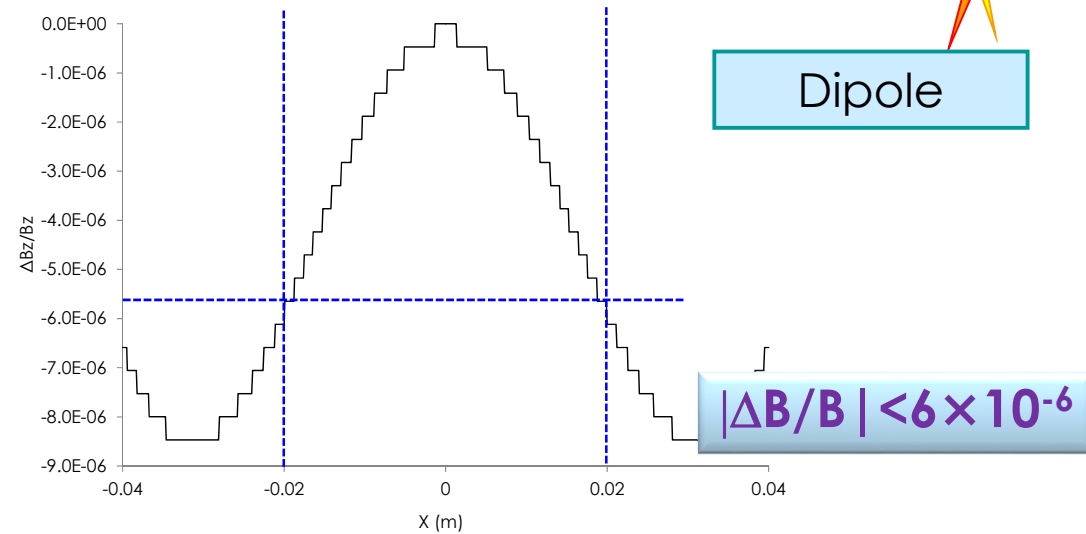
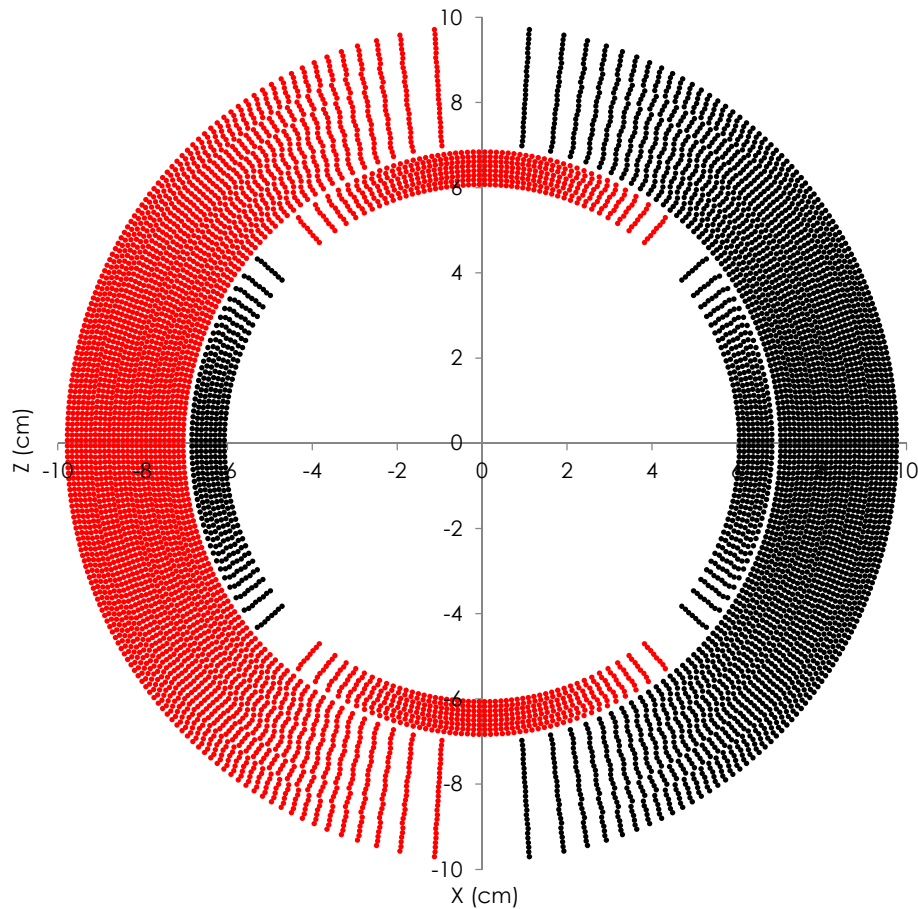
Dipole



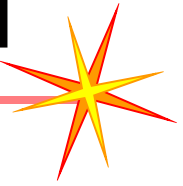
Quardupole

Design of superconducting coils

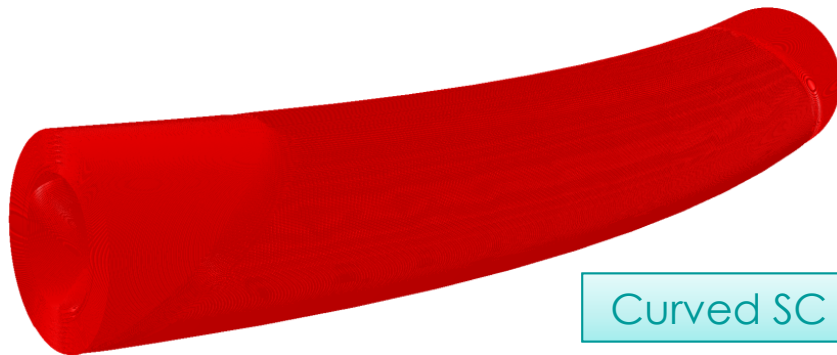
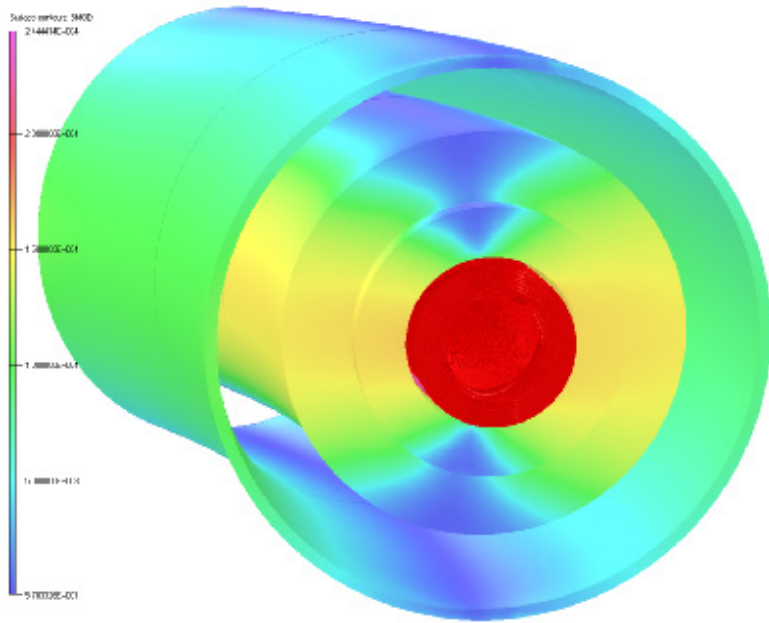
2D field calculation
(BM02-BM05)



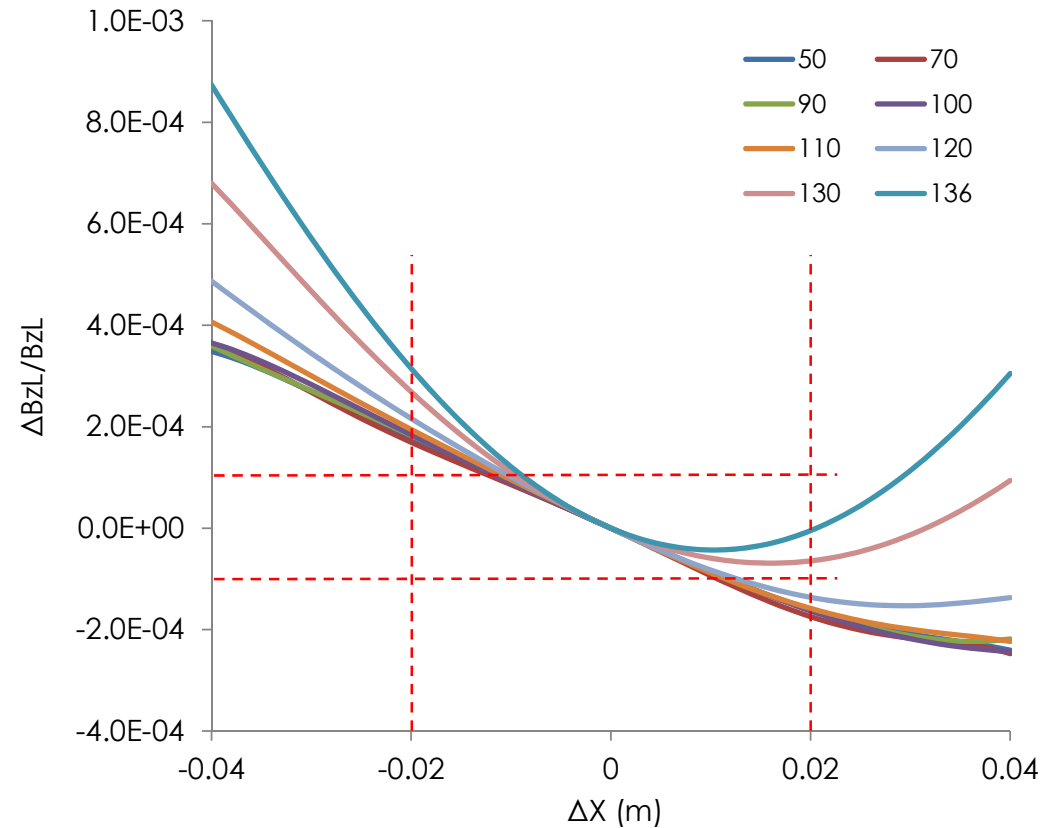
3D field calculation with Opera-3d



SC coils were precisely modelled



Curved SC coil

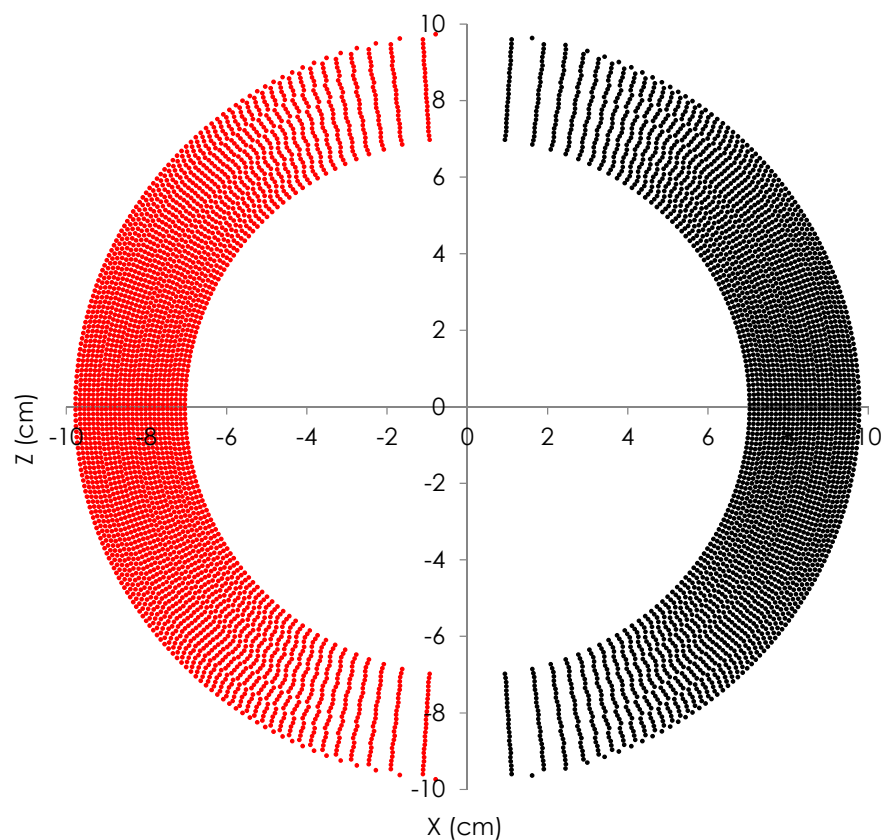


$$|\Delta B_L/B_L| < 4 \times 10^{-4}$$

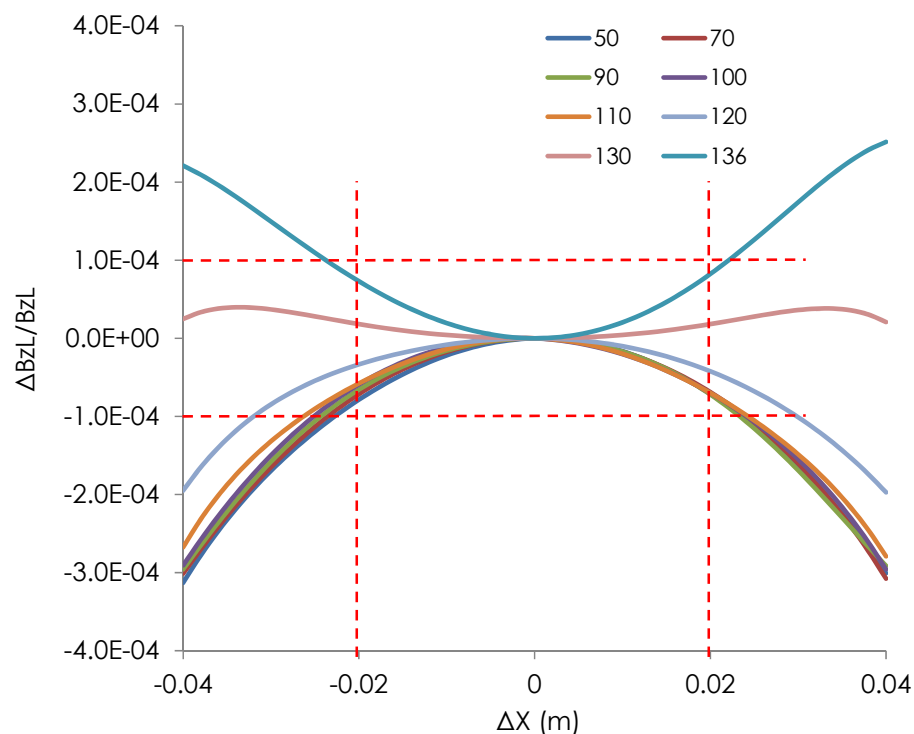
Corrections with the outermost layer



Coil positions of the outermost layer were modified to cancel out the measured multi-pole components



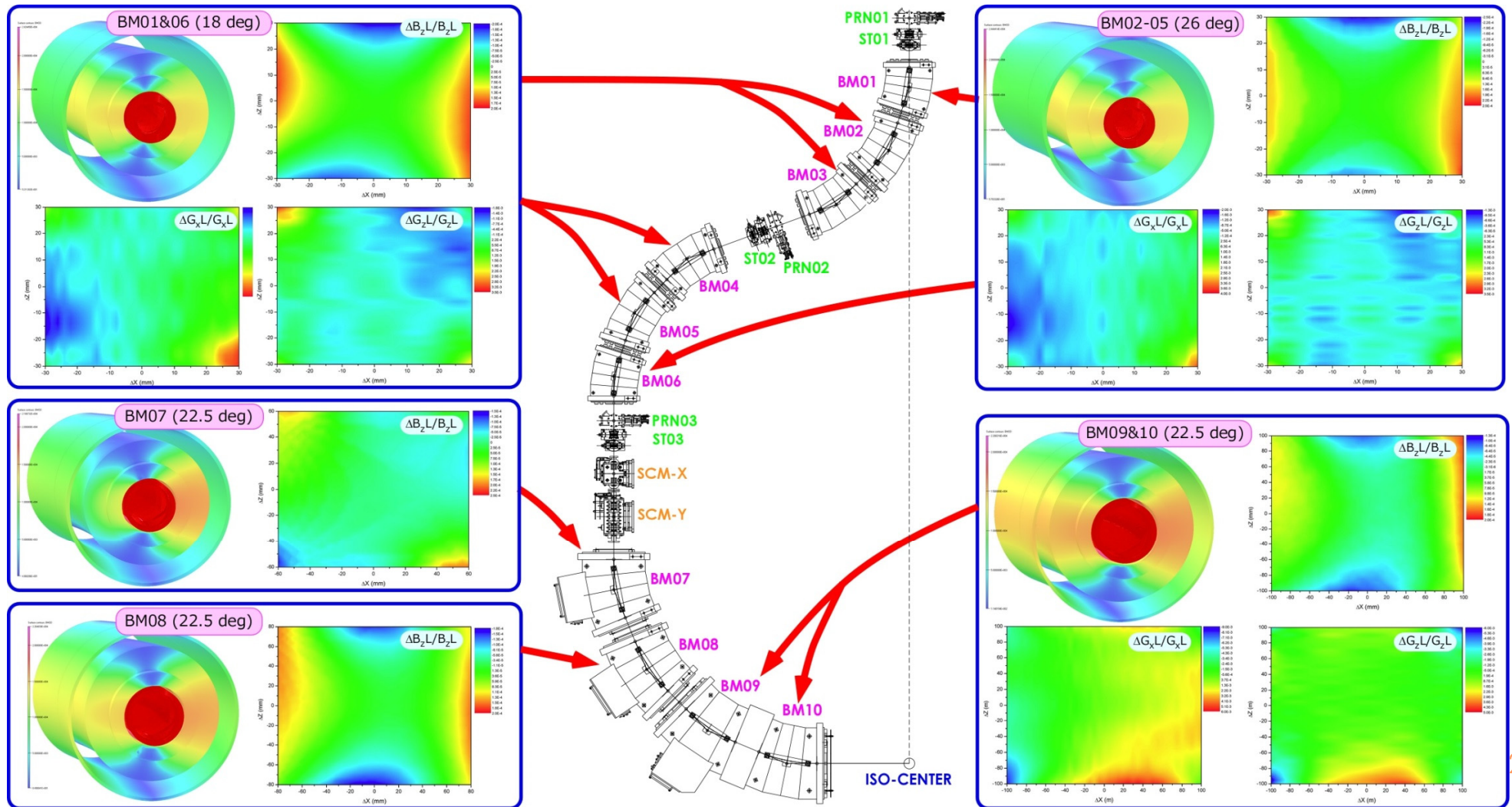
Corrected uniformity



$|\Delta B_L/B_L| < 1 \times 10^{-4}!$

Design of SC magnets

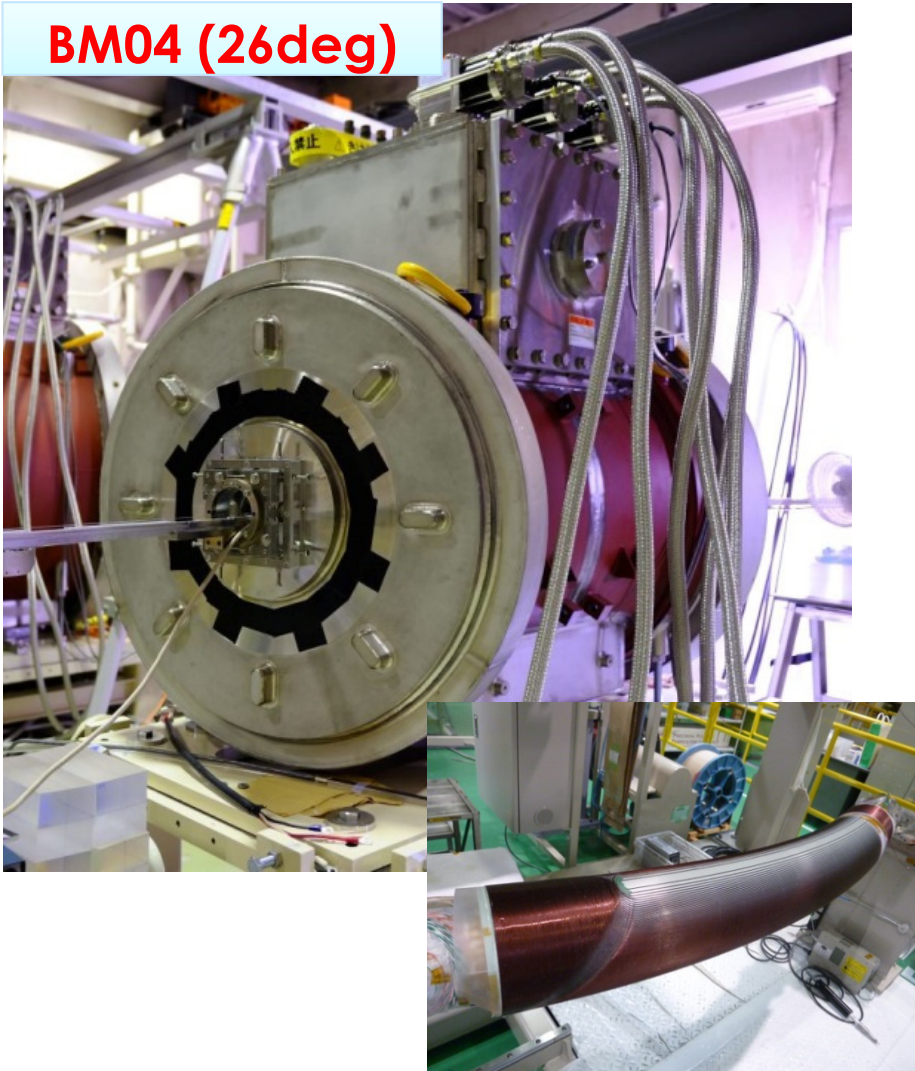
All the SC magnets were designed by using a 3D magnetic field solver



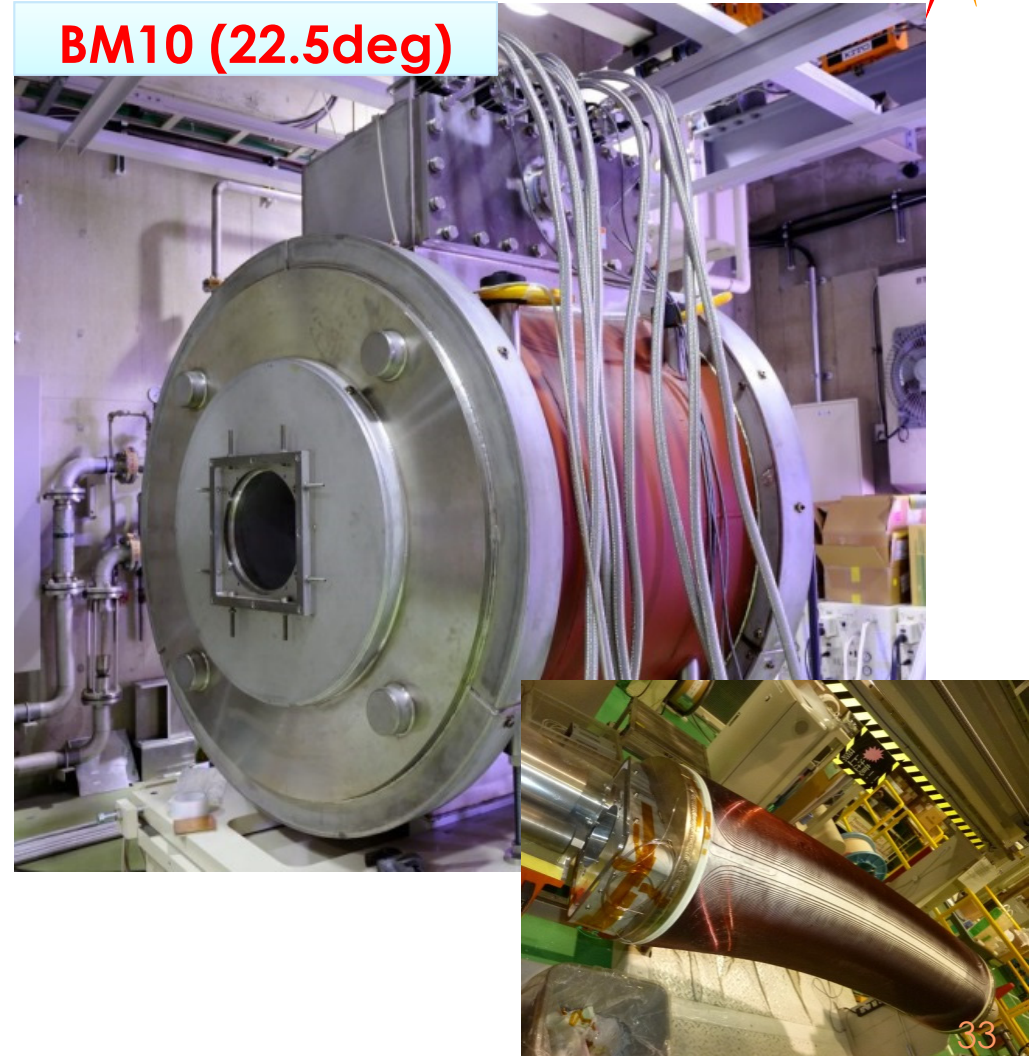
Construction of SC magnets



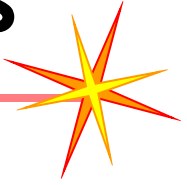
BM04 (26deg)



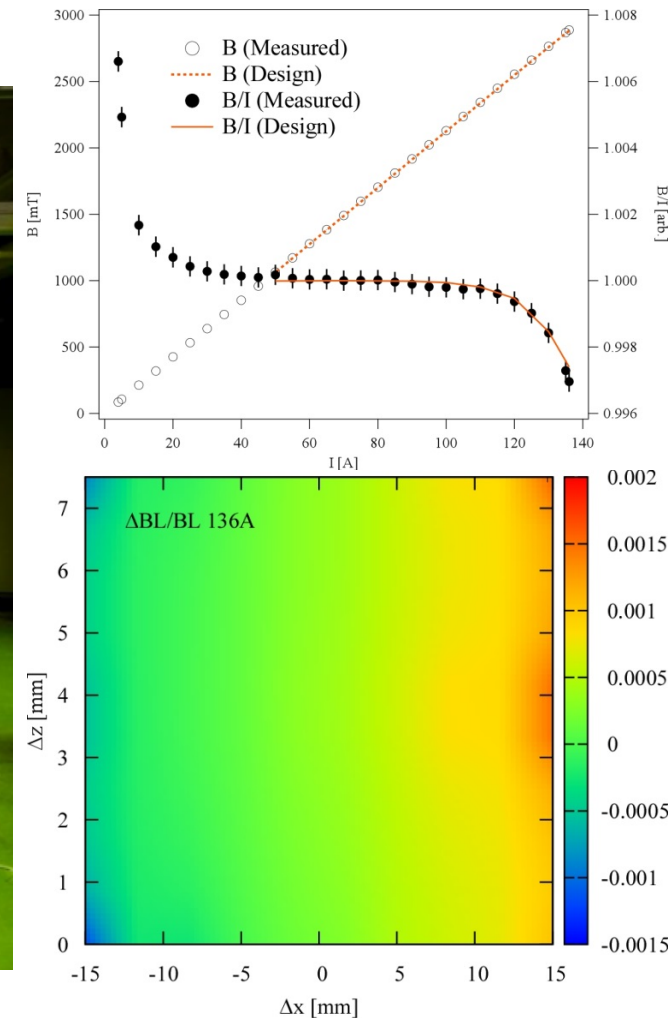
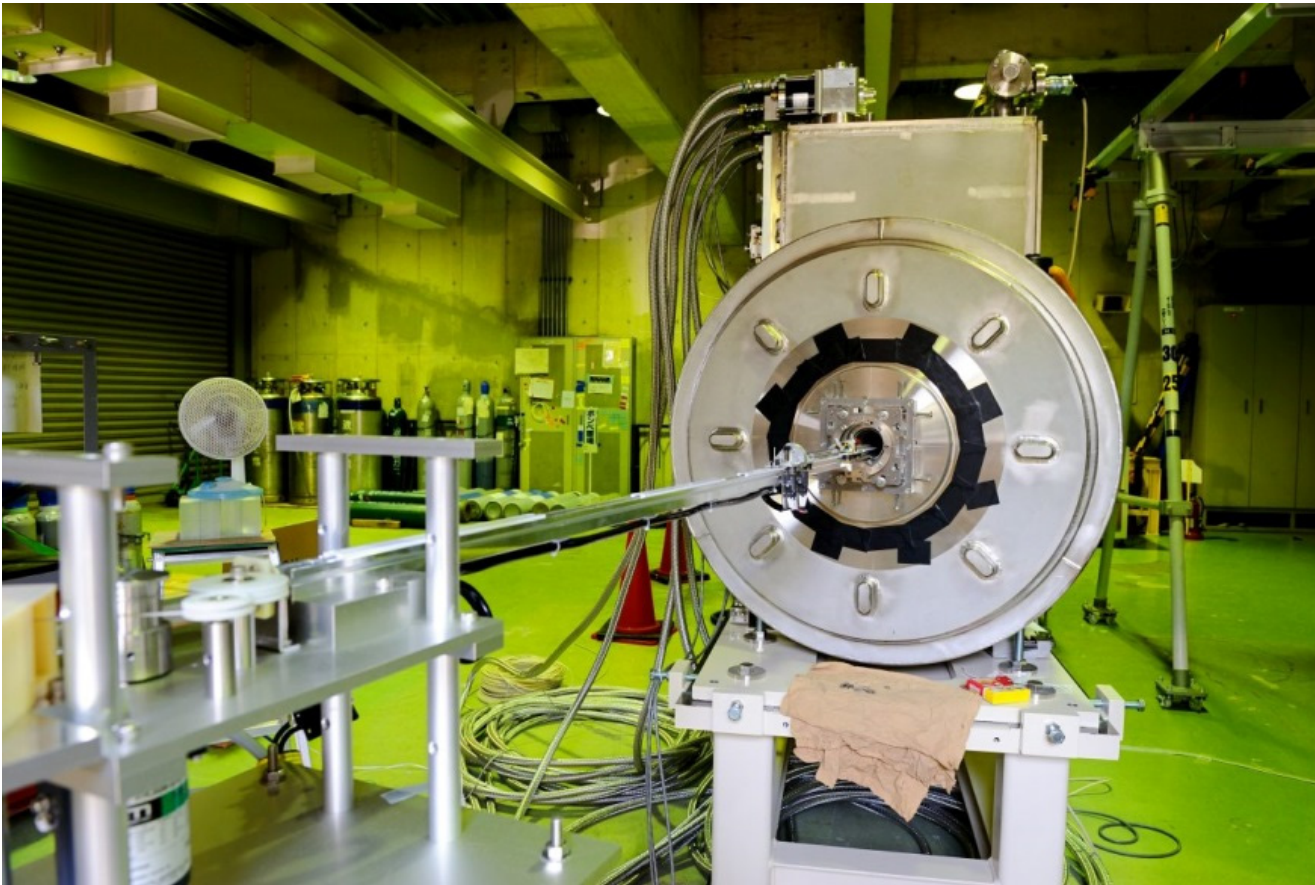
BM10 (22.5deg)

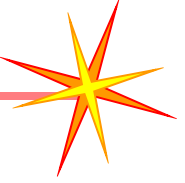


Field measurements



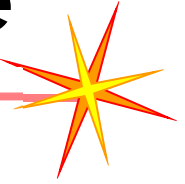
- Magnetic field measurements were performed
 - to verify the SC magnet design



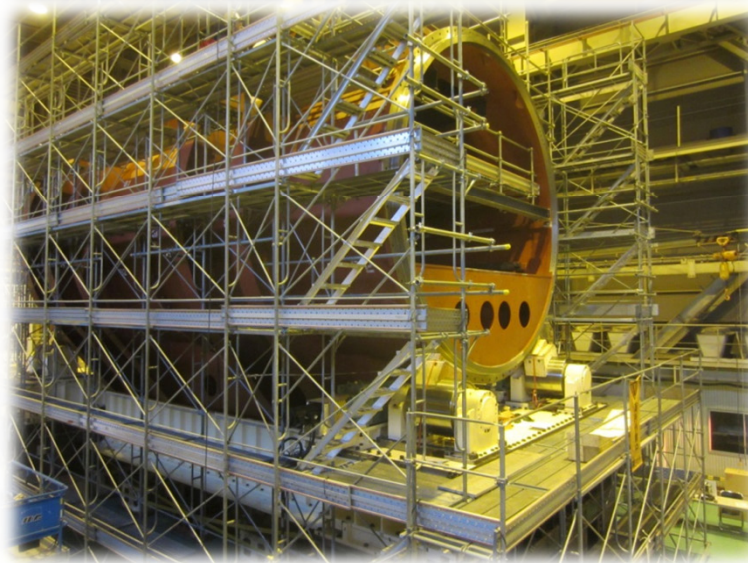
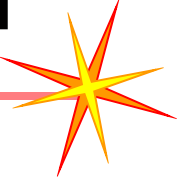


Construction of the gantry structure

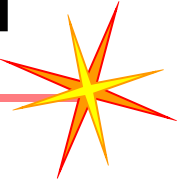
Construction of structure



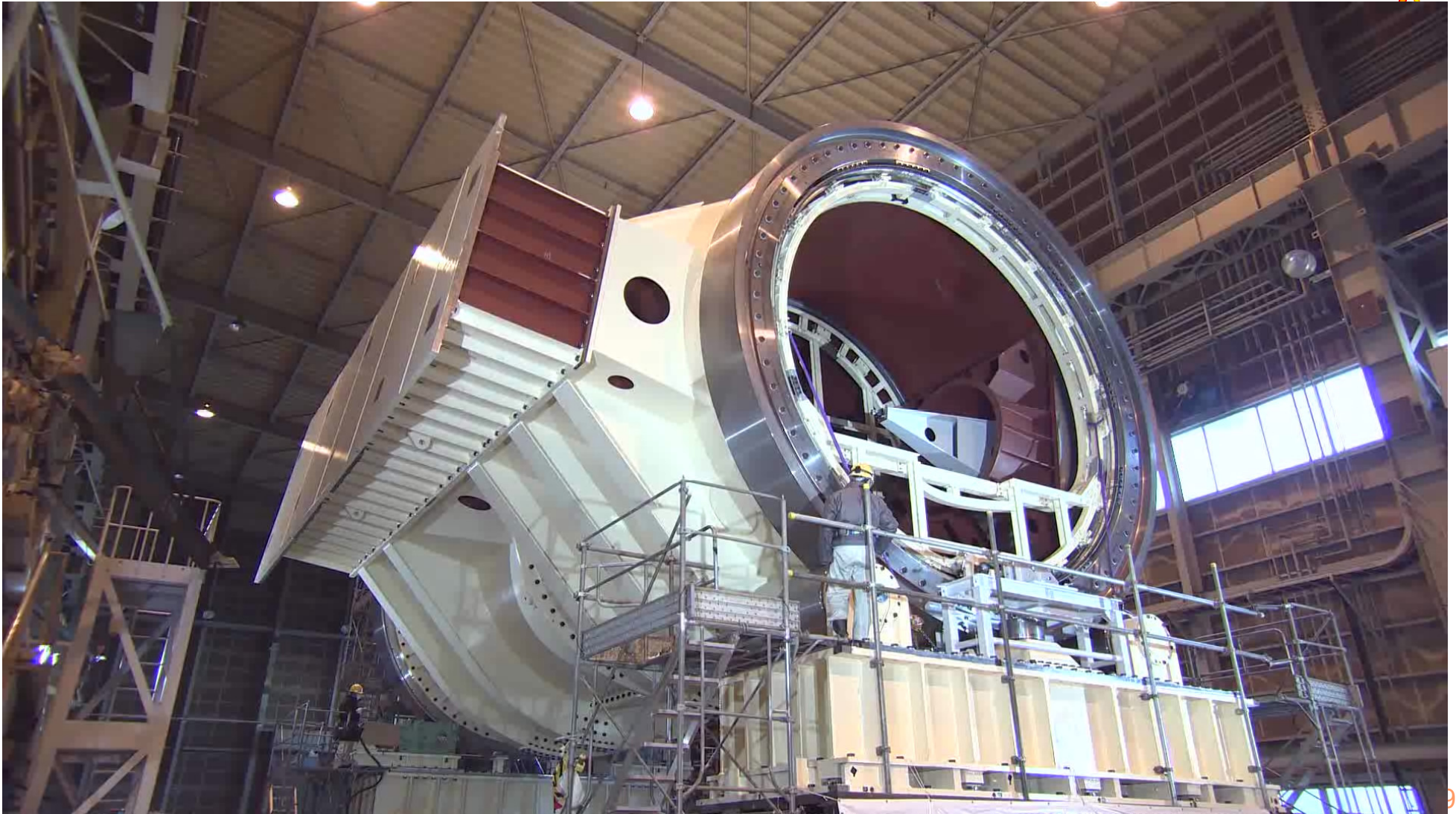
Assembling at Toshiba



Assembling at Toshiba



Rotation tests at Toshiba



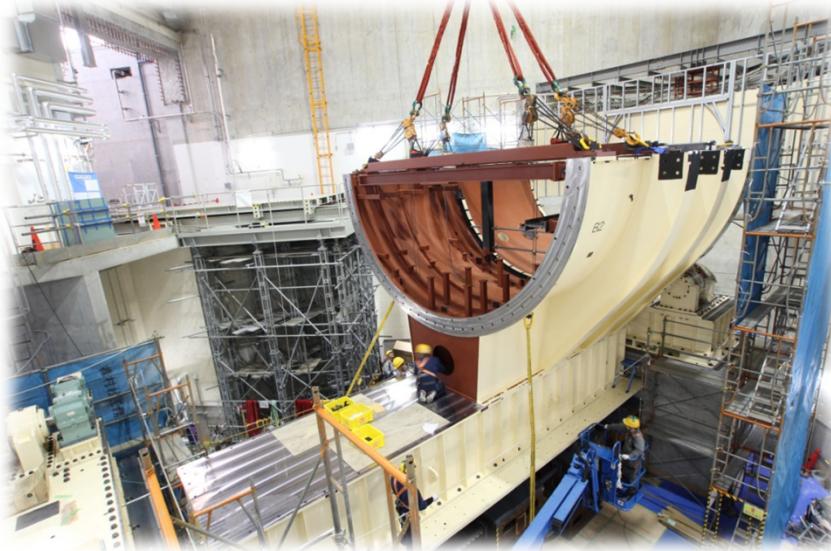
Transportation to NIRS



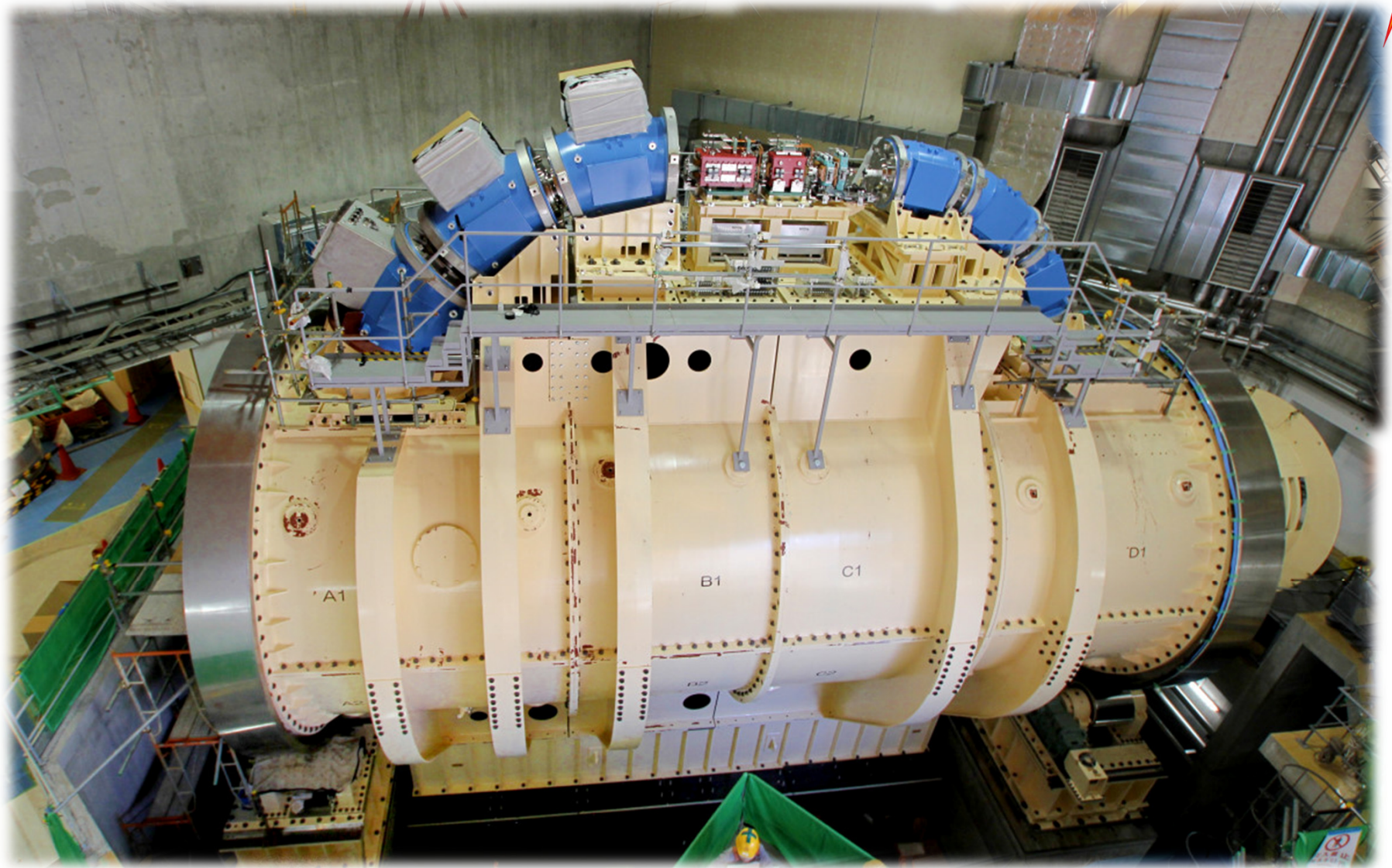
Installation to the gantry room



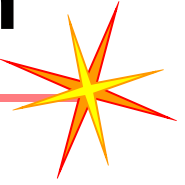
Reassembling at NIRS



Reassembling at NIRS



Treatment-room design

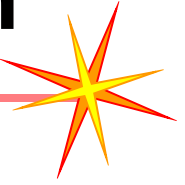


- The treatment room for the gantry is designed, based on the existing room E & F

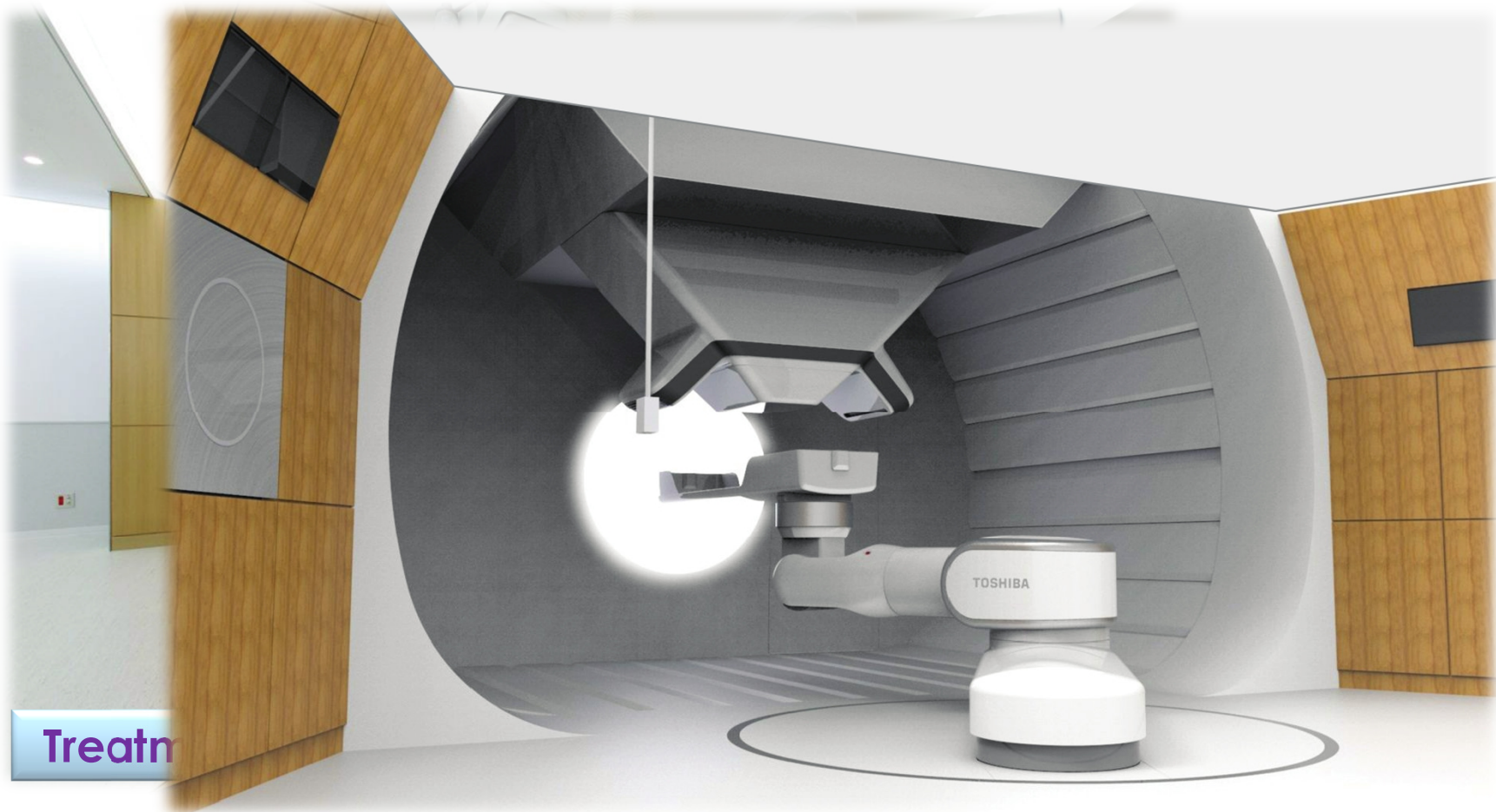


Treatment room E and F

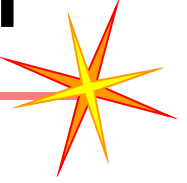
Treatment-room design



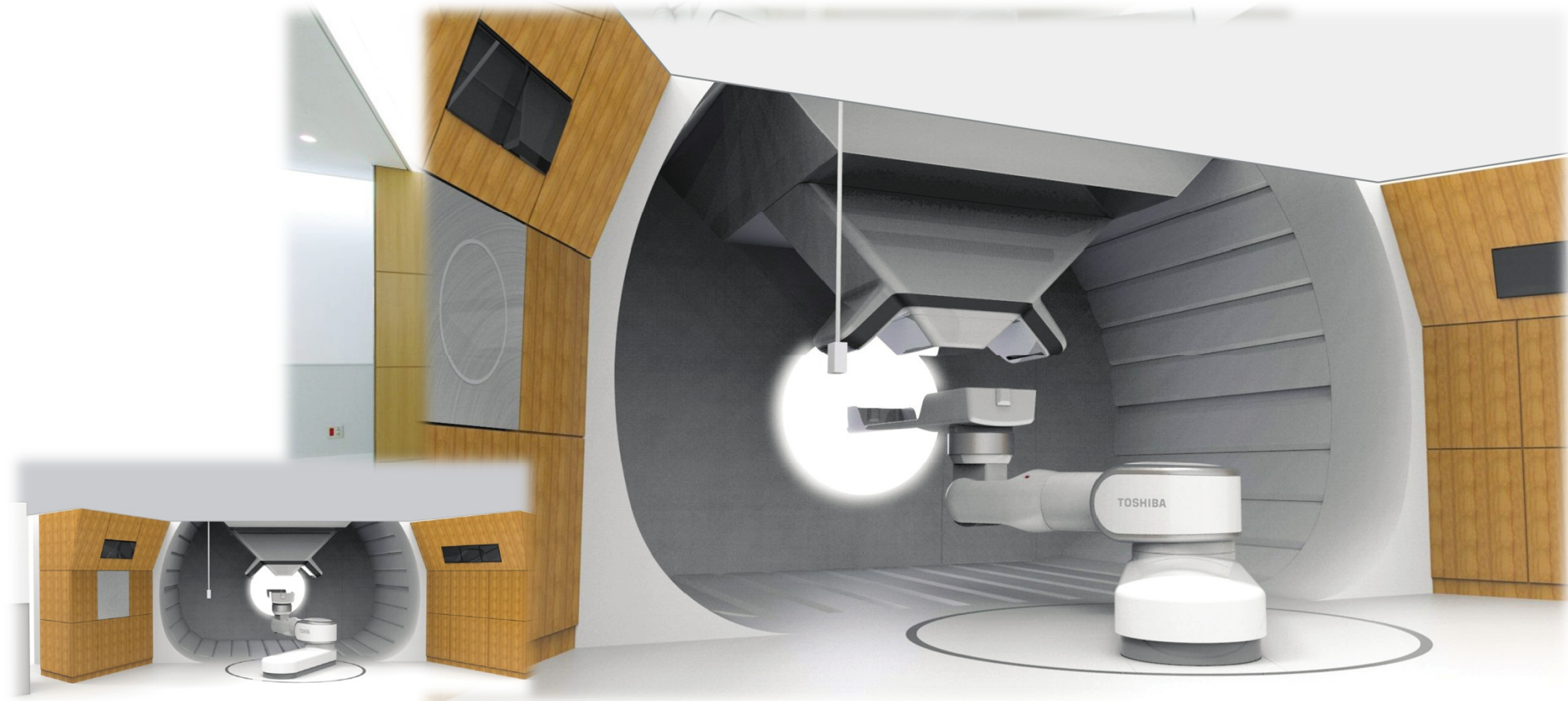
- The treatment room for the gantry is designed, based on the existing room E & F

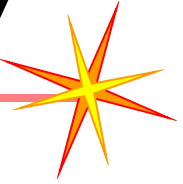


Treatment-room design



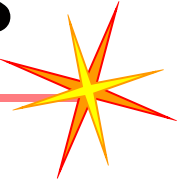
- The treatment room for the gantry is designed, based on the existing room E & F





- **Design of the superconducting rotating-gantry**
 - **Compact (~proton gantries)**
 - **Construction will be completed by the end of this month**
- **Future plan**
 - **Commissioning will be made from this October**
 - **Treatment will be made in 2016**





- K. Noda, T. Shirai, T. Fujita, T. Furukawa, K. Mizushima, Y. Hara, Y. Saraya, R. Tansho, S. Matsuba, S. Mori, S. Sato, K. Shoda (NIRS)
- T. Fujimoto, H. Arai (AEC)
- T. Ogitsu (KEK)
- N. Amemiya (Kyoto Univ.)
- Y. Nagamoto, T. Orikasa, S. Takayama, (Toshiba)

Specifications of SC magnets



Parameters	Symbol	Unit	BM01	BM02	BM03	BM04	BM05	BM06	BM07	BM08	BM09	BM10
Type	—	—	Superconducting sector magnet									
Coil	—	—	Dipole+Quard.						Dipole		Dipole+Quard.	
Bending angle	θ	deg	18	26				18	22.5			
Bending radius	ρ	m	2.3						2.8			
Maximum field	B _{dipole}	T	2.88						2.37			
Maximum field gradient	G _{max}	T/m	10						—		1.3	
Bore size	D _{bore}	mm	ϕ60						□122	□170	□206	
Effective radius or area	D _f or A _f	mm	ϕ40						□120	□160	□200	
Uniformity (dipole)	ΔBL/BL	—	±1×10 ⁻⁴									
Uniformity (quadrupole)	ΔGL/GL	—	±1×10 ⁻³									
Inductance (dipole)	L	H	6.2	9.1				6.2	5.2	8.9	12	
Stored Energy (dipole)	P	kJ	57	84				57	133	225	319	